

(19) World Intellectual Property
Organization
International Bureau



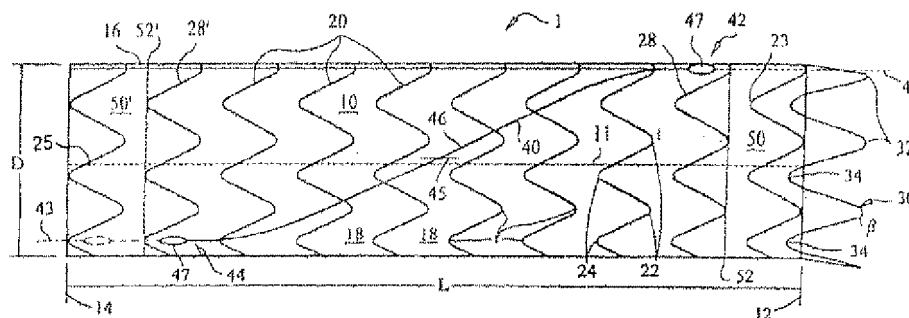
(43) International Publication Date
17 March 2005 (17.03.2005)

PCT

(10) International Publication Number
WO 2005/023149 A2

- (51) International Patent Classification⁷: A61F (74) Agent: MAYBACK, Gregory, L.; Lerner and Greenberg, P.A., P.O. Box 2480, Hollywood, FL 33022-2480 (US).
- (21) International Application Number: PCT/US2004/028530 (81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NA, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.
- (22) International Filing Date: 2 September 2004 (02.09.2004)
- (25) Filing Language: English
- (26) Publication Language: English
- (30) Priority Data:
60/499,652 3 September 2003 (03.09.2003) US
60/500,155 4 September 2003 (04.09.2003) US
10/784,462 23 February 2004 (23.02.2004) US
10/884,136 2 July 2004 (02.07.2004) US
- (71) Applicant (for all designated States except US): BOLTON MEDICAL, INC. [US/US]; 799 International Parkway, Sunrise, FL 33325 (US).
- (84) Designated States (unless otherwise indicated, for every kind of regional protection available): ARIPO (BW, GH, GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PL, PT, RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).
- (71) Applicants and
(72) Inventors: ARBEFEUILLE, Samuel [US/US]; 1410 Coolidge Street, Hollywood, FL 33020 (US). BERRA, Humberto [US/US]; 12100 Limestone Way, Cooper City, FL 33026 (US). OUELETTE, Gerry [US/US]; 10671 N.W. 17th Court, Coral Springs, FL 33071 (US).
- Published:
— without international search report and to be republished upon receipt of that report
- For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

(54) Title: STENT GRAFT, STENT GRAFT DELIVERY SYSTEM AND KIT AND METHOD FOR IMPLANTING THE STENT GRAFT



(57) Abstract: A vascular repair device includes a graft body and a framework having at least two stents connected to the body. The stents can each be respectively connected to graft body adjacent the proximal and distal ends and the support member is shorter than the separation distance therebetween to form a gimbal at least at one end. A first stent is connected along an entirety thereof and a second stent is connected at distal apices thereof. Distal apices of the second stent have radii of curvature smaller than proximal apices. A curved longitudinal member can be connected to the graft body, the member being substantially symmetrical with respect to the centerline. The member can be connected to the graft body independent of the framework. At least one of the member ends can have a curved extremity. A delivery system and kit and method for implanting the graft are also provided.

WO 2005/023149 A2

STENT GRAFT, STENT GRAFT DELIVERY SYSTEM AND KIT AND METHOD FOR IMPLANTING THE STENT GRAFT

BACKGROUND OF THE INVENTION

5 Field of the Invention:

The invention lies in the field of endoluminal blood vessel repairs. The invention specifically relates to a delivery system, a kit, and method for endoluminally repairing aneurysm and/or dissections of the thoracic transverse aortic arch, thoracic posterior aortic arch, and the descending thoracic portion of the aorta with a self-aligning stent graft.

10

Description of the Related Art:

A stent graft is an implantable device made of a tube-shaped surgical graft covering and an expanding or self-expanding frame. The stent graft is placed inside a blood vessel to bridge, for example, an aneurismal, dissected, or other diseased segment of the blood vessel, and, thereby, exclude the hemodynamic pressures of blood flow from the diseased segment of the blood vessel.

15 In selected patients, a stent graft advantageously eliminates the need to perform open thoracic or abdominal surgical procedures to treat diseases of the aorta and eliminates the need for total aortic reconstruction. Thus, the patient has less trauma and experiences a decrease in hospitalization and recovery times. The time needed to insert a stent graft is substantially less than the typical anesthesia time required for open aortic bypass surgical repair, for example.

20 Use of surgical and/or endovascular grafts have widespread use throughout the world in vascular surgery. There are many different kinds of vascular graft configurations. Some have supporting framework over their entirety, some have only two stents as a supporting framework, and others simply have the tube-shaped graft material with no additional supporting framework, an example that is not relevant to the present invention.

25 One of the most commonly known supporting stent graft frameworks is that disclosed in U.S. Patent Nos. 5,282,824 and 5,507,771 to Gianturco (hereinafter collectively referred to as "Gianturco"). Gianturco describes a zig-zag-shaped, self-expanding stent commonly referred to as a z-stent. The stents are, preferably, made of nitinol, but also have been made from stainless steel and other biocompatible materials.

There are various features characterizing a stent graft. The first significant feature is the tube of graft material. This tube is commonly referred to as the graft and forms the tubular shape that will, ultimately, take the place the diseased portion of the blood vessel. The graft is, preferably, made of a woven sheet (tube) of polyester or PTFE. The circumference of the graft tube is, typically, at least as large as the diameter and/or circumference of the vessel into which the graft will be inserted so that there is no possibility of blood flowing around the graft (also referred to as endoleak) to either displace the graft or to reapply hemodynamic pressure against the diseased portion of the blood vessel. Accordingly, to so hold the graft, self-expanding frameworks are attached typically to the graft material, whether on the interior or exterior thereof. Because blood flow within the lumen of the graft could be impaired if the framework was disposed on the interior wall of the graft, the framework is connected typically to the exterior wall of the graft. The ridges formed by such an exterior framework help to provide a better fit in the vessel by providing a sufficiently uneven outer surface that naturally grips the vessel where it contacts the vessel wall and also provides areas around which the vessel wall can endothelialize to further secure the stent graft in place.

One of the significant dangers in endovascular graft technology is the possibility of the graft migrating from the desired position in which it is installed. Therefore, various devices have been created to assist in anchoring the graft to the vessel wall.

One type of prior art prosthetic device is a stent graft made of a self-expanding metallic framework. For delivery, the stent graft is, first, radially compressed and loaded into an introducer system that will deliver the device to the target area. When the introducer system holding the stent graft positioned in an appropriate location in the vessel and allowed to open, the radial force imparted by the self-expanding framework is helpful, but, sometimes, not entirely sufficient, in endoluminally securing the stent graft within the vessel.

United States Patent No. 5,824,041 to Lenker et al. (hereinafter "Lenker") discloses an example of a stent graft delivery system. Lenker discloses various embodiments in which a sheath is retractable proximally over a prosthesis to be released. With regard to FIGS. 7 and 8, Lenker names components 72 and 76, respectively, as "sheath" and "prosthesis-containment sheath." However, the latter is merely the catheter in which the prosthesis 74 and the sheath 72 are held. With regard to FIGS. 9 and 10, the sheath 82 has inner and outer layers 91, 92 fluid-tightly connected to one another to form a ballooning structure around

the prosthesis P. This ballooning structure inflates when liquid is inflated with a non-compressible fluid medium and flares radially outward when inflated. With regard to FIGS. 13 to 15, Lenker discloses the "sheath" 120, which is merely the delivery catheter, and an eversible membrane 126 that "folds back over itself (everts) as the sheath 120 is retracted so that there are always two layers of the membrane between the distal end of the sheath [120] and the prosthesis P." Lenker at col. 9, lines 63 to 66. The eversion (peeling back) is caused by direct connection of the distal end 130 to the sheath 120. The Lenker delivery system shown in FIGS. 19A to 19D holds the prosthesis P at both ends 256, 258 while an outer catheter 254 is retracted over the prosthesis P and the inner sheath 260. The inner sheath 260 remains inside the outer catheter 254 before, during, and after retraction. Another structure for holding the prosthesis P at both ends is illustrated in FIGS. 23A and 23B. Therein, the proximal holder having resilient axial members 342 is connected to a proximal ring structure 346. FIGS. 24A to 24C also show an embodiment for holding the prosthesis at both ends inside thin-walled tube 362.

To augment radial forces of stents, some prior art devices have added proximal and/or distal stents that are not entirely covered by the graft material. By not covering with graft material a portion of the proximal/distal ends of the stent, these stents have the ability to expand further radially than those stents that are entirely covered by the graft material. By expanding further, the proximal/distal stent ends better secure to the interior wall of the vessel and, in doing so, press the extreme cross-sectional surface of the graft ends into the vessel wall to create a fixated blood-tight seal.

One example of such a prior art exposed stent can be found in United States Patent Publication US 2002/0198587 to Greenberg et al. The modular stent graft assembly therein has a three-part stent graft: a two-part graft having an aortic section 12 and an iliac section 14 (with four sizes for each) and a contralateral iliac occluder 80. FIGS. 1, 2, and 4 to 6 show the attachment stent 32. As illustrated in FIGS. 1, 2, and 4, the attachment stent 32, while rounded, is relatively sharp and, therefore, increases the probability of puncturing the vessel.

A second example of a prior art exposed stent can be found in U.S. Patent Publication 2003/0074049 to Hoganson et al. (hereinafter "Hoganson"), which discloses a covered stent 10 in which the elongated portions or sections 24 of the ends 20a and 20b extend beyond the marginal edges of the cover 22. See Hoganson at FIGS. 1, 3, 9, 11a, 11b, 12a, 12b, and 13. However, these extending exposed edges are triangular, with sharp apices pointing both

upstream and downstream with regard to a graft placement location. Such a configuration of the exposed stent 20a, 20b increases the possibility of puncturing the vessel. In various embodiments shown in FIGS. 6a, 6b, 6c, 10, 14a, Hoganson teaches completely covering the extended stent and, therefore, the absence of a stent extending from the cover 22. It is
5 noted that the Hoganson stent is implanted by inflation of a balloon catheter.

Another example of a prior art exposed stent can be found in U.S. Patent No. 6,565,596 to White et al. (hereinafter "White I"), which uses a proximally extending stent to prevent twisting or kinking and to maintain graft against longitudinal movement. The extending stent is expanded by a balloon and has a sinusoidal amplitude greater than the next adjacent
10 one or two sinusoidal wires. White I indicates that it is desirable to space wires adjacent upstream end of graft as close together as is possible. The stent wires of White I are actually woven into graft body by piercing the graft body at various locations. See White I at FIGS. 6 and 7. Thus, the rips in the graft body can lead to the possibility of the exposed stent moving with respect to the graft and of the graft body ripping further. Between the
15 portions of the extending stent 17, the graft body has apertures.

The stent configuration of U.S. Patent No. 5,716,393 to Lindenberg et al. is similar to White I in that the outermost portion of the one-piece stent -- made from a sheet that is cut/punched and then rolled into cylinder -- has a front end with a greater amplitude than the remaining body of the stent

20 A further example of a prior art exposed stent can be found in U.S. Patent No. 6,524,335 to Hartley et al. (hereinafter "Hartley"). FIGS. 1 and 2 of Hartley particularly disclose a proximal first stent 1 extending proximally from graft proximal end 4 with both the proximal and distal apices narrowing to pointed ends.

Yet another example of a prior art exposed stent can be found in U.S. Patent No. 6,355,056
25 to Pinheiro (hereinafter "Pinheiro I"). Like the Hartley exposed stent, Pinheiro discloses exposed stents having triangular, sharp proximal apices.

Still a further example of a prior art exposed stent can be found in U.S. Patent No. 6,099,558 to White et al. (hereinafter "White II"). The White II exposed stent is similar to the exposed stent of White I and also uses a balloon to expand the stent.

30 An added example of a prior art exposed stent can be found in U.S. Patent No. 5,871,536 to Lazarus, which discloses two support members 68 longitudinally extending from proximal end to a rounded point. Such points, however, create a very significant possibility of piercing the vessel.

An additional example of a prior art exposed stent can be found in U.S. Patent No. 5,851,228 to Pinheiro (hereinafter "Pinheiro II"). The Pinheiro II exposed stents are similar to the exposed stents of Pinheiro I and, as such, have triangular, sharp, proximal apices. Still another example of a prior art exposed stent can be found in Lenker (U.S. Patent No. 5,824,041), which shows a squared-off end of the proximal and distal exposed band members 14. A portion of the exposed members 14 that is attached to the graft material 18, 20 is longitudinally larger than a portion of the exposed members 14 that is exposed and extends away from the graft material 18, 20. Lenker et al. does not describe the members 14 in any detail.

Yet a further example of a prior art exposed stent can be found in U.S. Patent No. 5,824,036 to Lauterjung, which, of all of the prior art embodiments described herein, shows the most pointed of exposed stents. Specifically, the proximal ends of the exposed stent are apices pointed like a minaret. The minaret points are so shaped intentionally to allow forks 300 (see Lauterjung at FIG. 5) external to the stent 154 to pull the stent 154 from the sheath 302, as opposed to being pushed.

A final example of a prior art exposed stent can be found in U.S. Patent No. 5,755,778 to Kleshinski. The Kleshinski exposed stents each have two different shaped portions, a triangular base portion and a looped end portion. The totality of each exposed cycle resembles a castellation. Even though the end-most portion of the stent is curved, because it is relatively narrow, it still creates the possibility of piercing the vessel wall.

All of these prior art stents suffer from the disadvantageous characteristic that the relatively sharp proximal apices of the exposed stents have a shape that is likely to puncture the vessel wall.

Devices other than exposed stents have been used to inhibit graft migration. A second of such devices is the placement of a relatively stiff longitudinal support member longitudinally extending along the entirety of the graft.

The typical stent graft has a tubular body and a circumferential framework. This framework is not usually continuous. Rather, it typically takes the form of a series of rings along the tubular graft. Some stent grafts have only one or two of such rings at the proximal and/or distal ends and some have many stents tandemly placed along the entirety of the graft material. Thus, the overall stent graft has an "accordion" shape. During the systolic phase of each cardiac cycle, the hemodynamic pressure within the vessel is substantially parallel with the longitudinal plane of the stent graft. Therefore, a device

having unsecured stents, could behave like an accordion or concertina with each systolic pulsation, and may have a tendency to migrate downstream. (A downstream migration, to achieve forward motion, has a repetitive longitudinal compression and extension of its cylindrical body.) Such movement is entirely undesirable. Connecting the stents with
5 support along the longitudinal extent of the device thereof can prevent such movement. To provide such support, a second anti-migration device can be embodied as a relatively stiff longitudinal bar connected to the framework.

A clear example of a longitudinal support bar can be found in Pinheiro I (6,355,056) and Pinheiro II (5,851,228). Each of these references discloses a plurality of longitudinally
10 extending struts 40 extending between and directly interconnecting the proximal and distal exposed stents 20a, 20b. These struts 40 are designed to extend generally parallel with the inner lumen 15 of the graft 10, in other words, they are straight.

Another example of a longitudinal support bar can be found in United States Patent No. 6,464,719 to Jayaraman. The Jayaraman stent is formed from a graft tube 21 and a
15 supporting sheet 1 made of nitinol. This sheet is best shown in FIG. 3. The end pieces 11, 13 of the sheet are directly connected to one another by wavy longitudinal connecting pieces 15 formed by cutting the sheet 1. To form the stent graft, the sheet 1 is coiled with or around the cylindrical tube 21. See FIGS. 1 and 4. Alternatively, a plurality of connecting
20 pieces 53 with holes at each end thereof can be attached to a cylindrical fabric tube 51 by stitching or sutures 57, as shown in FIG. 8. Jayaraman requires more than one of these serpentine shaped connecting pieces 53 to provide longitudinal support.

United States Patent Publication 2002/0016627 and United States Patent No. 6,312,458 to Golds each disclose a variation of a coiled securing member 20.

A different kind of supporting member is disclosed in FIG. 8 of United States Patent No.
25 6,053,943 to Edwin et al.

Like Jayaraman, United States Patent No. 5,871,536 to Lazarus discloses a plurality of straight, longitudinal support structures 38 attached to the circumferential support structures 36, see FIGS. 1, 6, 7, 8, 10, 11, 12, 14. FIG. 8 of Lazarus illustrates the longitudinal support
30 structures 38 attached to a distal structure 36 and extending almost all of the way to the proximal structure 36. The longitudinal structures 38, 84, 94 can be directly connected to the body 22, 80 and can be telescopic 38, 64.

United States Patent Publication 2003/0088305 to Van Schie et al. (hereinafter "Van Schie") does not disclose a support bar. Rather, it discloses a curved stent graft using an

elastic material 8 connected to stents at a proximal end 2 and at a distal end 3 (see FIGS. 1, 2) thereof to create a curved stent graft. Because Van Schie needs to create a flexible curved graft, the elastic material 8 is made of silicone rubber or another similar material. Thus, the material 8 cannot provide support in the longitudinal extent of the stent graft.

5 Accordingly, an alternative to the elastic support material 8 is a suture material 25 shown in FIGS. 3 to 6.

SUMMARY OF THE INVENTION

The invention provides a stent graft, stent graft delivery system and kit and method for

10 implanting the stent graft that overcome the hereinafore-mentioned disadvantages of the heretofore-known devices and methods of this general type and that provides a vessel repair device that implants/conforms more efficiently within the natural or diseased course of the aorta by aligning with the natural curve of the aorta, decreases the likelihood of vessel puncture, increases the blood-tight vascular connection, retains the intraluminal wall of the

15 vessel position, is more resistant to migration, and delivers the stent graft into a curved vessel while minimizing intraluminal forces imparted during delivery and while minimizing the forces needed for a user to deliver the stent graft into a curved vessel.

Other features that are considered as characteristic for the invention are set forth in the appended claims.

20 Although the invention is illustrated and described herein as embodied in a stent graft, it is, nevertheless, not intended to be limited to the details shown because various modifications and structural changes may be made therein without departing from the spirit of the invention and within the scope and range of equivalents of the claims.

The construction and method of operation of the invention, however, together with

25 additional objects and advantages thereof, will be best understood from the following description of specific embodiments when read in connection with the accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

30 The features of the present invention, which are believed to be novel, are set forth with particularity in the appended claims. The invention, together with further objects and advantages thereof, may best be understood by reference to the following description, taken

in conjunction with the accompanying drawings, in the several figures of which like reference numerals identify like elements, and in which:

FIG. 1 is a side elevational view of a stent graft according to the invention;

FIG. 2 is a side elevational view of a stent of the stent graft of FIG. 1;

5 FIG. 3 is a cross-sectional view of the stent of FIG. 2 with different embodiments of protrusions;

FIG. 4 is a perspective view of a prior art round mandrel for forming prior art stents;

FIG. 5 is a fragmentary, side elevational view of a prior art stent in a portion of a vessel;

FIG. 6 is a perspective view of a dodecahedral-shaped mandrel for forming stents in FIGS.

10 1 to 3;

FIG. 7 is a fragmentary, side elevational view of the stent of FIGS. 1 to 3 in a portion of a vessel;

FIG. 8 is a fragmentary, enlarged side elevational view of the proximal end of the stent graft of FIG. 1 illustrating movement of a gimbaled end;

15 FIG. 9 is a side elevational view of a two-part stent graft according to the invention;

FIG. 10 is a fragmentary, side elevational view of a delivery system according to the invention with a locking ring in a neutral position;

FIG. 11 is a fragmentary, side elevational view of the delivery system of FIG. 10 with the locking ring in an advancement position and, as indicated by dashed lines, a distal handle

20 and sheath assembly in an advanced position;

FIG. 12 is a fragmentary, enlarged view of a sheath assembly of the delivery system of FIG. 10;

FIG. 13 is a fragmentary, enlarged view of an apex capture device of the delivery system of FIG. 10 in a captured position;

25 FIG. 14 is a fragmentary, enlarged view of the apex capture device of FIG. 13 in a released position;

FIG. 15 is a fragmentary, enlarged view of an apex release assembly of the delivery system of FIG. 10 in the captured position;

30 FIG. 16 is a fragmentary, enlarged view of the apex release assembly of FIG. 15 in the captured position with an intermediate part removed;

FIG. 17 is a fragmentary, enlarged view of the apex release assembly of FIG. 16 in the released position;

- FIG. 18 is a fragmentary, side elevational view of the delivery system of FIG. 11 showing how a user deploys the prosthesis;
- FIG. 19 is a fragmentary cross-sectional view of human arteries including the aorta with the assembly of the present invention in a first step of a method for inserting the prosthesis according to the invention;
- FIG. 20 is a fragmentary cross-sectional view of the arteries of FIG. 19 with the assembly in a subsequent step of the method for inserting the prosthesis;
- FIG. 21 is a fragmentary cross-sectional view of the arteries of FIG. 20 with the assembly in a subsequent step of the method for inserting the prosthesis;
- FIG. 22 is a fragmentary cross-sectional view of the arteries of FIG. 21 with the assembly in a subsequent step of the method for inserting the prosthesis;
- FIG. 23 is a fragmentary cross-sectional view of the arteries of FIG. 22 with the assembly in a subsequent step of the method for inserting the prosthesis;
- FIG. 24 is a fragmentary cross-sectional view of the arteries of FIG. 23 with the assembly in a subsequent step of the method for inserting the prosthesis;
- FIG. 25 is a fragmentary, diagrammatic, perspective view of the coaxial relationship of delivery system lumen according to the invention;
- FIG. 26 is a fragmentary, cross-sectional view of the apex release assembly according to the invention;
- FIG. 27 is a fragmentary, side elevational view of the stent graft of FIG. 1 with various orientations of radiopaque markers according to the invention;
- FIG. 28 is a fragmentary perspective view of the stent graft of FIG. 1 with various orientations of radiopaque markers according to the invention;
- FIG. 29 is a perspective view of a distal apex head of the apex capture device of FIG. 13;
- FIG. 30 is a fragmentary side elevational view of the distal apex head of FIG. 29 and a proximal apex body of the apex capture device of FIG. 13 with portions of a bare stent in the captured position;
- FIG. 31 is a fragmentary, side elevational view of the distal apex head and proximal apex body of FIG. 30 with a portion of the proximal apex body cut away to illustrate the bare stent in the captured position;
- FIG. 32 is a fragmentary side elevational view of the distal apex head and proximal apex body of FIG. 30 in the released position;

FIG. 33 is a fragmentary, cross-sectional view of an embodiment of handle assemblies according to the invention;

FIG. 34 is a cross-sectional view of a pusher clasp rotator of the handle assembly of FIG. 33;

5 FIG. 35 is a plan view of the pusher clasp rotator of FIG. 34 viewed along line C-C;

FIG. 36 is a plan and partially hidden view of the pusher clasp rotator of FIG. 34 with a helix groove for a first embodiment of the handle assembly of FIGS. 10, 11, and 18;

FIG. 37 is a cross-sectional view of the pusher clasp rotator of FIG. 36 along section line A-A;

10 FIG. 38 is a plan and partially hidden view of the pusher clasp rotator of FIG. 36;

FIG. 39 is a cross-sectional view of the pusher clasp rotator of FIG. 38 along section line B-B;

FIG. 40 is a perspective view of a rotator body of the handle assembly of FIG. 33;

FIG. 41 is an elevational and partially hidden side view of the rotator body of FIG. 40;

15 FIG. 42 is a cross-sectional view of the rotator body of FIG. 41 along section line A-A;

FIG. 43 is an elevational and partially hidden side view of the rotator body of FIG. 40;

FIG. 44 is an elevational and partially hidden side view of a pusher clasp body of the handle assembly of FIG. 33;

FIG. 45 is a cross-sectional view of the pusher clasp body of FIG. 44 along section line A-

20 A;

FIG. 46 is a cross-sectional view of the pusher clasp body of FIG. 44 along section line B-B;

FIG. 47 is a fragmentary, side elevational view of a portion of the handle assembly of FIG. 33 with a sheath assembly according to the invention;

25 FIG. 48 is an exploded side elevational view of a portion of the handle assembly of FIG. 47;

FIG. 49 is a fragmentary elevational and partially hidden side view of a handle body of the handle assembly of FIG. 33;

FIG. 50 is a fragmentary, exploded side elevational view of a portion of a second embodiment of the handle assembly according to the invention;

30 FIG. 51 is a fragmentary, side elevational view of the portion of FIG. 50 in a neutral position;

FIG. 52 is an exploded view of a first portion of the second embodiment of the handle assembly;

- FIG. 53 is a fragmentary, exploded view of a larger portion of the second embodiment of the handle assembly as compared to FIG. 52 with the first portion and the sheath assembly; FIG. 54 is perspective view of a clasp body of the second embodiment of the handle assembly;
- 5 FIG. 55 is an elevational side view of the clasp body of FIG. 54;
FIG. 56 is a cross-sectional view of the clasp body of FIG. 55 along section line A-A;
FIG. 57 is a plan view of the clasp body of FIG. 54;
FIG. 58 is a plan view of the clasp body of FIG. 57 viewed from section line B-B;
FIG. 59 is a fragmentary and partially hidden side elevational view of a clasp sleeve of the
- 10 second embodiment of the handle assembly;
FIG. 60 is a fragmentary, cross-sectional view of a portion the clasp sleeve of FIG. 59 along section line A;
FIG. 61 is a fragmentary, cross-sectional view of the clasp sleeve of FIG. 59 along section line C-C;
- 15 FIG. 62 is a fragmentary and partially hidden side elevational view of the clasp sleeve of FIG. 59 rotated with respect to FIG. 59;
FIG. 63 is a fragmentary, cross-sectional view of the nose cone and sheath assemblies of FIG. 10;
FIG. 64 is a fragmentary, perspective view of a portion of self-alignment configuration
- 20 according to the invention;
FIG. 65 is a diagrammatic, fragmentary, cross-sectional view of a distal portion of the delivery system with the self-alignment configuration according to the invention inside the descending thoracic aorta and with the self-alignment configuration in an orientation opposite a desired orientation;
- 25 FIG. 66 is a diagrammatic, fragmentary, cross-sectional view of the distal portion of the delivery system of FIG. 65 with the self-alignment configuration partially inside the descending thoracic aorta and partially inside the aortic arch and with the self-alignment configuration in an orientation closer to the desired orientation;
FIG. 67 is a diagrammatic, fragmentary, cross-sectional view of the distal portion of the
- 30 delivery system of FIG. 65 with the self-alignment configuration primarily inside the aortic arch and with the self-alignment configuration substantially in the desired orientation;
FIG. 68 is a fragmentary, enlarged, partially exploded perspective view of an alternative embodiment of a distal end of the graft push lumen of FIG. 25; and

FIG. 69 is a photograph of a user bending a stent graft assembly around a curving device to impart a curve to a guidewire lumen therein.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

5 While the specification concludes with claims defining the features of the invention that are regarded as novel, it is believed that the invention will be better understood from a consideration of the following description in conjunction with the drawing figures, in which like reference numerals are carried forward.

The present invention provides a stent graft and delivery system that treats, in particular,
10 thoracic aortic defects from the brachiocephalic level of the aortic arch distally to a level just superior to the celiac axis and provides an endovascular foundation for an anastomosis with the thoracic aorta, while providing an alternative method for partial/total thoracic aortic repair by excluding the vessel defect and making surgical repair of the aorta unnecessary. The stent graft of the present invention, however, is not limited to use in the aorta. It can be
15 endoluminally inserted in any accessible artery that could accommodate the stent graft's dimensions.

Stent Graft

The stent graft according to the present invention provides various features that, heretofore, have not been applied in the art and, thereby, provide a vessel repair device that
20 implants/conforms more efficiently within the natural or diseased course of the aorta, decreases the likelihood of vessel puncture, and increases the blood-tight vascular connection, and decreases the probability of graft mobility.

The stent graft is implanted endovascularly before or during or in place of an open repair of the vessel (i.e., an arch, in particular, the ascending and/or descending portion of the aorta)
25 through a delivery system described in detail below. The typical defects treated by the stent graft are aortic aneurysms, aortic dissections, and other diseases such as penetrating aortic ulcer, coarctation, and patent ductus arteriosus, related to the aorta. When endovascularly placed in the aorta, the stent graft forms a seal in the vessel and automatically affixes itself to the vessel with resultant effacement of the pathological lesion.

30 Referring now to the figures of the drawings in detail and first, particularly to FIG. 1 thereof, there is shown an improved stent graft 1 having a graft sleeve 10 and a number of stents 20. These stents 20 are, preferably, made of nitinol, an alloy having particularly special properties allowing it to rebound to a set configuration after compression, the

rebounding property being based upon the temperature at which the alloy exists. For a detailed explanation of nitinol and its application with regard to stents, see, e.g., United States Patent Nos. 4,665,906, 5,067,957, and 5,597,378 to Jervis and to Gianturco.

The graft sleeve 10 is cylindrical in shape and is made of a woven graft material along its entire length. The graft material is, preferably, polyester, in particular, polyester referred to under the name DACRON® or other material types like Expanded Polytetrafluoroethylene (“EPTFE”), or other polymeric based coverings. The tubular graft sleeve 10 has a framework of individual lumen-supporting wires each referred to in the art as a stent 20. Connection of each stent 20 is, preferably, performed by sewing a polymeric (nylon, polyester) thread around an entirety of the stent 20 and through the graft sleeve 10. The stitch spacings are sufficiently close to prevent any edge of the stent 20 from extending substantially further from the outer circumference of the graft sleeve 10 than the diameter of the wire itself. Preferably, the stitches have a 0.5 mm to 5 mm spacing.

The stents 20 are sewn either to the exterior or interior surfaces of the graft sleeve 10. FIG. 1 illustrates all stents 20, 30 on the exterior surface 16 of the graft sleeve 10. In a preferred non-illustrated embodiment, the most proximal 23 and distal stents and a bare stent 30 are connected to the interior surface of the graft sleeve 10 and the remainder of the stents 20 are connected to the exterior surface 16. Another possible non-illustrated embodiment alternates connection of the stents 20, 30 to the graft sleeve 10 from the graft exterior surface to the graft interior surface, the alternation having any periodic sequence.

A stent 20, when connected to the graft sleeve 10, radially forces the graft sleeve 10 open to a predetermined diameter D. The released radial force creates a seal with the vessel wall and affixes the graft to the vessel wall when the graft is implanted in the vessel and is allowed to expand.

Typically, the stents 20 are sized to fully expand to the diameter D of the fully expanded graft sleeve 10. However, a characteristic of the present invention is that each of the stents 20 and 30 has a diameter larger than the diameter D of the fully expanded graft sleeve 10. Thus, when the stent graft 1 is fully expanded and resting on the internal surface of the vessel where it has been placed, each stent 20 is imparting independently a radially directed force to the graft sleeve 10. Such pre-compression, as it is referred to herein, is applied (1) to ensure that the graft covering is fully extended, (2) to ensure sufficient stent radial force to make sure sealing occurs, (3) to affix the stent graft and prevent it from kinking, and (4) to affix the stent graft and prevent migration.

Preferably, each of the stents 20 is formed with a single nitinol wire. Of course other biocompatible materials can be used, for example, stainless steel, biopolymers, cobalt chrome, and titanium alloys.

The preferred shape of each stent 20 corresponds to what is referred in the art as a Z-stent, see, e.g., Gianturco (although the shape of the stents 20 can be in any form that satisfies the functions of a self-expanding stent). Thus, the wire forming the stent 20 is a ring having a wavy or sinusoidal shape. In particular, an elevational view orthogonal to the center axis 21 of the stent 20 reveals a shape somewhere between a triangular wave and a sinusoidal wave as shown in FIG. 2. In other words, the view of FIG. 2 shows that the stents 20 each have alternating proximal 22 and distal 24 apices. Preferably, the apices have a radius r that does not present too great of a point towards a vessel wall to prevent any possibility of puncturing the vessel, regardless of the complete circumferential connection to the graft sleeve 10. In particular, the radius r of curvature of the proximal 22 and distal 24 apices of the stent 20 are, preferably, equal. The radius of curvature r is between approximately 0.1 mm and approximately 3.0 mm, in particular, approximately 0.5 mm.

Another advantageous feature of a stent lies in extending the longitudinal profile along which the stent contacts the inner wall of a vessel. This longitudinal profile can be explained with reference to FIGS. 3 to 7.

Prior art stents and stents according to the present invention are formed on mandrels 29, 29' by winding the wire around the mandrel 29, 29' and forming the apexes 22, 24, 32, 34 by wrapping the wire over non-illustrated pins that protrude perpendicular from the axis of the mandrel. Such pins, if illustrated, would be located in the holes illustrated in the mandrels 29, 29' of FIGS. 4 and 6. Prior art stents are formed on a round mandrel 29 (also referred to as a bar). A stent 20' formed on a round mandrel 29 has a profile that is rounded (see FIG. 5). Because of the rounded profile, the stent 20' does not conform evenly against the inner wall of the vessel 2 in which it is inserted. This disadvantage is critical in the area of stent graft 1 seal zones -- areas where the ends of the graft 10 need to be laid against the inner wall of the vessel 2. Clinical experience reveals that stents 20' formed with the round mandrel 29 do not lie against the vessel 2; instead, only a mid-section of the stent 20' rests against the vessel 2, as shown in FIG. 5. Accordingly, when such a stent 20' is present at either of the proximal 12 or distal 14 ends of the stent graft 1, the graft material flares away from the wall of the vessel 2 into the lumen -- a condition that is to be avoided. An example of this flaring can be seen by comparing the upper and lower portions of the curved

longitudinal profile of the stent 20' in FIG. 5 with the linear longitudinal profile of the vessel 2.

To remedy this problem and ensure co-columnar apposition of the stent and vessel, stents 20 of the present invention are formed on a multiple-sided mandrel. In particular, the stents 20 are formed on a polygonal-shaped mandrel 29'. The mandrel 29' does not have sharp edges. Instead, it has flat sections and rounded edge portions between the respective flat sections. Thus, a stent formed on the mandrel 29' will have a cross-section that is somewhat round but polygonal, as shown in FIG. 3. The cross-sectional view orthogonal to the center axis 21 of such a stent 20 will have beveled or rounded edges 31 (corresponding to the rounded edge portions of the mandrel 29') disposed between flat sides or struts 33 (corresponding to the flat sections of the mandrel 29').

To manufacture the stent 20, apexes of the stents 20 are formed by winding the wire over non-illustrated pins located on the rounded portions of the mandrel 29'. Thus, the struts 33 lying between the apexes 22, 24, 32, 34 of the stents 20 lie flat against the flat sides of the mandrel 29'. When so formed on the inventive mandrel 29', the longitudinal profile is substantially less rounded than the profile of stent 20' and, in practice, is substantially linear.

For stents 20 having six proximal 22 and six distal 24 apices, the stents 20 are formed on a dodecahedron-shaped mandrel 29' (a mandrel having twelve sides), which mandrel 29' is shown in FIG. 6. A stent 20 formed on such a mandrel 29' will have the cross-section illustrated in FIG. 3.

The fourteen-apex stent 20 shown in FIG. 7 illustrates a stent 20 that has been formed on a fourteen-sided mandrel. The stent 20 in FIG. 7 is polygonal in cross-section (having fourteen sides) and, as shown in FIG. 7, has a substantially linear longitudinal profile. Clinically, the linear longitudinal profile improves the stent's 20 ability to conform to the vessel 2 and press the graft sleeve 10 outward in the sealing zones at the extremities of the individual stent 20.

Another way to improve the performance of the stent graft 1 is to provide the distal-most stent 25 on the graft 10 (i.e., downstream) with additional apices and to give it a longer longitudinal length (i.e., greater amplitude) and/or a longer circumferential length. When a stent 25 having a longer circumferential length is sewn to a graft, the stent graft 1 will perform better clinically. The improvement, in part, is due to a need for the distal portion of the graft material 10 to be pressed firmly against the wall of the vessel. The additional

apices result in additional points of contact between the stent graft 1 and vessel wall, thus ensuring better apposition to the wall of the vessel and better sealing of the graft material 10 to the vessel. The increased apposition and sealing substantially improves the axial alignment of the distal end 14 of the stent graft 1 to the vessel. As set forth above, each of
 5 the stents 20 and 30 has a diameter larger than the diameter D of the fully expanded graft sleeve 10. Thus, if the distal stent 25 also has a diameter larger than the diameter D, it will impart a greater radial bias on all 360 degrees of the corresponding section of the graft than stents not having such an oversized configuration.

A typical implanted stent graft 1 typically does not experience a lifting off at straight
 10 portions of a vessel because the radial bias of the stents acting upon the graft sleeve give adequate pressure to align the stent and graft sleeve with the vessel wall. However, when a typical stent graft is implanted in a curved vessel (such as the aorta), the distal end of the stent graft 1 does experience a lift off from the vessel wall. The increased apposition and sealing of the stent graft 1 according to the present invention substantially decreases the
 15 probability of lift off because the added height and additional apices enhance the alignment of the stent graft perpendicular to the vessel wall as compared to prior art stent grafts (no lift off occurs).

The number of total apices of a stent is dependent upon the diameter of the vessel in which the stent graft 1 is to be implanted. Vessels having a smaller diameter have a smaller total
 20 number of apices than a stent to be implanted in a vessel having a larger diameter. Table 1 below indicates preferred stent embodiments for vessels having different diameters. For example, if a vessel has a 26 or 27 mm diameter, then a preferred diameter of the graft sleeve 10 is 30 mm. For a 30 mm diameter graft sleeve, the intermediate stents 20 will have 5 apices on each side (proximal and distal) for a total of 10 apices. In other words, the stent
 25 defines 5 periodic "waves." The distal-most stent 25, in comparison, defines 6 periodic "waves" and, therefore, has 12 total apices. It is noted that the distal-most stent 25 in FIG. 1 does not have the additional apex. While Table 1 indicates preferred embodiments, these configurations can be adjusted or changed as needed.

Vessel Diameter (mm)	Graft Diameter (mm)	Stent Apices/Side (Distal-most Stent #)
19	22	5(5)
20-21	24	5(5)
22-23	26	5(5)

24-25	28	5(6)
26-27	30	5(6)
28-29	32	6(7)
30-31	34	6(7)
32-33	36	6(7)
34	38	6(7)
35-36	40	7(8)
37-38	42	7(8)
39-40	44	7(8)
41-42	46	7(8)

Table 1

To increase the security of the stent graft 1 in a vessel, an exposed or bare stent 30 is provided on the stent graft 1, preferably, only at the proximal end 12 of the graft sleeve 10 - proximal meaning that it is attached to the portion of the graft sleeve 10 from which the blood flows into the sleeve, i.e., blood flows from the bare stent 30 and through the sleeve 10 to the left of FIG. 1. The bare stent 30 is not limited to being attached at the proximal end 12. Another non-illustrated bare stent can be attached similarly to the distal end 14 of the graft sleeve 10.

Significantly, the bare stent 30 is only partially attached to the graft sleeve 10. Specifically, the bare stent 30 is fixed to the graft sleeve 10 only at the distal apices 34 of the bare stent 30. Thus, the bare stent 30 is partially free to extend the proximal apices 32 away from the proximal end of the graft sleeve 10.

The bare stent 30 has various properties, the primary one being to improve the apposition of the graft material to the contour of the vessel wall and to align the proximal portion of the graft covering in the lumen of the arch and provide a blood-tight closure of the proximal end 12 of the graft sleeve 10 so that blood does not pass between the vascular inside wall and outer surface 16 of the sleeve 10 (endoleak).

The preferred configuration for the radius of curvature α of the distal apices 34 is substantially equal to the radius r of the proximal 22 and distal 24 apices of the stent 20, in particular, it is equal at least to the radius of curvature r of the proximal apices of the stent 20 directly adjacent the bare stent 30. Thus, as shown in FIG. 8, a distance between the proximal apices 22 of the most proximal stent 23 and crossing points of the exposed

portions of the bare stent 30 are substantially at a same distance from one another all the way around the circumference of the proximal end 12 of the graft sleeve 10. Preferably, this distance varies based upon the graft diameter. Accordingly, the sinusoidal portion of the distal apices 34 connected to the graft sleeve 10 traverse substantially the same path as that of the stent 23 closest to the bare stent 30. Thus, the distance d between the stent 22 and all portions of the bare stent 30 connected to the graft sleeve 10 remain constant. Such a configuration is advantageous because it maintains the symmetry of radial force of the device about the circumference of the vessel and also aids in the synchronous, simultaneous expansion of the device, thus increasing apposition of the graft material to the vessel wall to induce a proximal seal -- and substantially improve the proximal seal -- due to increasing outward force members in contact with the vessel wall.

Inter-positioning the stents 23, 30 in phase with one another, creates an overlap, i.e., the apices 34 of the bare stent 30 are positioned within the troughs of the stent 23. A further advantage of such a configuration is that the overlap provides twice as many points of contact between the proximal opening of the graft 10 and the vessel in which the stent graft 1 is implanted. The additional apposition points keep the proximal opening of the graft sleeve 10 open against the vessel wall, which substantially reduces the potential for endoleaks. In addition, the overlap of the stents 23, 30 increases the radial load or resistance to compression, which functionally increases fixation and reduces the potential for device migration.

In contrast to the distal apices 34 of the bare stent 30, the radius of curvature β of the proximal apices 32 (those apices that are not sewn into the graft sleeve 10) is significantly larger than the radius of curvature α of the distal apices 34. A preferred configuration for the bare stent apices has a radius approximately equal to 1.5 mm for the proximal apices 32 and approximately equal to 0.5 mm for the distal apices 34. Such a configuration substantially prevents perforation of the blood vessel by the proximal apices 32, or, at a minimum, makes is much less likely for the bare stent 30 to perforate the vessel because of the less-sharp curvature of the proximal apices 32.

The bare stent 30 also has an amplitude greater than the other stents 20. Preferably, the peak-to-peak amplitude of the stents 20 is approximately 1.3 cm to 1.5 cm, whereas the peak-to-peak amplitude of the bare stent 30 is approximately 2.5 cm to 4.0 cm.

Accordingly, the force exerted by the bare stent 30 on the inner wall of the aorta (due to the bare stent 30 expanding to its native position) is spread over a larger surface area. Thus, the

bare stent 30 of the present invention presents a less traumatic radial stress to the interior of the vessel wall -- a characteristic that, while less per square mm than an individual one of the stents 20 would be, is sufficient, nonetheless, to retain the proximal end 12 in position. Simultaneously, the taller configuration of the bare stent 30 guides the proximal opening of the stent graft in a more "squared-off" manner. Thus, the proximal opening of the stent graft is more aligned with the natural curvature of the vessel in the area of the proximal opening.

As set forth above, because the vessel moves constantly, and due to the constantly changing pressure imparted by blood flow, any stent graft placed in the vessel has the natural tendency to migrate downstream. This is especially true when the stent graft 1 has graft sleeve segments 18 with lengths defined by the separation of the stents on either end of the segment 18, giving the stent graft 1 an accordion, concertina, or caterpillar-like shape. When such a shape is pulsating with the vessel and while hemodynamic pressure is imparted in a pulsating manner along the stent graft from the proximal end 12 to the downstream distal end 14, the stent graft 1 has a tendency to migrate downstream in the vessel. It is desired to have such motion be entirely prohibited.

Support along a longitudinal extent of the graft sleeve 10 assists in preventing such movement. Accordingly, as set forth above, prior art stent grafts have provided longitudinal rods extending in a straight line from one stent to another.

The present invention, however, provides a longitudinal, spiraling/helical support member 40 that, while extending relatively parallel to the longitudinal axis 11 of the graft sleeve 10, is not aligned substantially parallel to a longitudinal extent of the entirety of the stent graft 1 as done in the prior art. "Relatively parallel" is referred to herein as an extent that is more along the longitudinal axis 11 of the stent graft 1 than along an axis perpendicular thereto. Specifically, the longitudinal support member 40 has a somewhat S-turn shape, in that, a proximal portion 42 is relatively parallel to the axis 11 of the graft sleeve 10 at a first degree 41 (being defined as a degree of the 360 degrees of the circumference of the graft sleeve 10), and a distal portion 44 is, also, relatively parallel to the axis 11 of the tube graft, but at a different second degree 43 on the circumference of the graft sleeve 10. The difference between the first and second degrees 41, 43 is dependent upon the length L of the graft sleeve 10. For an approximately 20 cm (approx. 8") graft sleeve, for example, the second degree 43 is between 80 and 110 degrees away from the first degree 41, in particular, approximately 90 degrees away. In comparison, for an approximately 9 cm

(approx. 3.5") graft sleeve, the second degree 43 is between 30 and 60 degrees away from the first degree 41, in particular, approximately 45 degrees away. As set forth below, the distance between the first and second degrees 41, 43 is also dependent upon the curvature and the kind of curvature that the stent graft 1 will be exposed to when in vivo.

5 The longitudinal support member 40 has a curved intermediate portion 46 between the proximal and distal portions 42, 44. By using the word "portion" it is not intended to mean that the rod is in three separate parts (of course, in a particular configuration, a multi-part embodiment is possible). A preferred embodiment of the longitudinal support member 40 is a single, one-piece rod made of stainless steel, cobalt chrome, nitinol, or polymeric
10 material that is shaped as a fully curved helix 42, 44, 46 without any straight portion. In an alternative stent graft embodiment, the proximal and distal portions 42, 44 can be substantially parallel to the axis 11 of the stent graft 1 and the central portion 46 can be helically curved.

One way to describe the preferred curvature embodiment of the longitudinal support
15 member 40 can be using an analogy of asymptotes. If there are two asymptotes extending parallel to the longitudinal axis 11 of the graft sleeve 10 at the first and second degrees 41, 43 on the graft sleeve 10, then the proximal portion 42 can be on the first degree 41 or extend approximately asymptotically to the first degree 41 and the distal portion 44 can be on the second degree 43 or extend approximately asymptotically to the second degree 43.
20 Because the longitudinal support member 40 is one piece in a preferred embodiment, the curved portion 46 follows the natural curve formed by placing the proximal and distal portions 42, 44 as set forth herein.

In such a position, the curved longitudinal support member 40 has a centerline 45 (parallel to the longitudinal axis 11 of the graft sleeve 10 halfway between the first and second
25 degrees 41, 43 on the graft sleeve 10). In this embodiment, therefore, the curved portion intersects the centerline 45 at approximately 20 to 40 degrees in magnitude, preferably at approximately 30 to 35 degrees.

Another way to describe the curvature of the longitudinal support member can be with respect to the centerline 45. The portion of the longitudinal support member 40 between
30 the first degree 41 and the centerline 45 is approximately a mirror image of the portion of the longitudinal support member 40 between the second degree 43 and the centerline 45, but rotated one-hundred eighty degrees (180°) around an axis orthogonal to the centerline 45. Such symmetry can be referred to herein as "reverse-mirror symmetrical."

The longitudinal support member 40 is, preferably, sewn to the graft sleeve 10 in the same way as the stents 20. However, the longitudinal support member 40 is not sewn directly to any of the stents 20 in the proximal portions of the graft. In other words, the longitudinal support member 40 is independent of the proximal skeleton formed by the stents 20. Such a configuration is advantageous because an independent proximal end creates a gimbal that endows the stent graft with additional flexibility. Specifically, the gimballed proximal end allows the proximal end to align better to the proximal point of apposition, thus reducing the chance for endoleak. The additional independence from the longitudinal support member allows the proximal fixation point to be independent from the distal section that is undergoing related motion due to the physiological motion of pulsatile flow of blood. Also in a preferred embodiment, the longitudinal support member 40 is pre-formed in the desired spiral/helical shape (counter-clockwise from proximal to distal), before being attached to the graft sleeve 10.

Because vessels receiving the stent graft 1 are not typically straight (especially the aortic arch), the final implanted position of the stent graft 1 will, most likely, be curved in some way. In prior art stent grafts (which only provide longitudinally parallel support rods), there exist, inherently, a force that urges the rod, and, thereby, the entire stent graft, to the straightened, natural shape of the rod. This force is disadvantageous for stent grafts that are to be installed in an at least partly curved manner.

The curved shape of the longitudinal support member 40 according to the present invention eliminates at least a majority, or substantially all, of this disadvantage because the longitudinal support member's 40 natural shape is curved. Therefore, the support member 40 imparts less of a force, or none at all, to straighten the longitudinal support member 40, and, thereby, move the implanted stent graft in an undesirable way. At the same time, the curved longitudinal support member 40 negates the effect of the latent kinetic force residing in the aortic wall that is generated by the propagation of the pulse wave and systolic blood pressure in the cardiac cycle, which is, then, released during diastole. As set forth in more detail below, the delivery system of the present invention automatically aligns the stent graft 1 to the most optimal position while traversing the curved vessel in which it is to be implanted, specifically, the longitudinal support member 40 is placed substantially at the superior longitudinal surface line of the curved aorta (with respect to anatomical position). In a preferred embodiment, the longitudinal support member 40 can be curved in a patient-customized way to accommodate the anticipated curve of the actual vessel in which the

graft will be implanted. Thus, the distance between the first and second degrees 41, 43 will be dependent upon the curvature and the kind of curvature that the stent graft 1 will be exposed to when in vivo. As such, when implanted, the curved longitudinal support member 40 will, actually, exhibit an opposite force against any environment that would
5 alter its conformance to the shape of its resident vessel's existing course(es).

Preferably, the support member 40 is sewn, in a similar manner as the stents 20, on the outside surface 16 of the graft sleeve 10.

In prior art support rods, the ends thereof are merely a terminating end of a steel or nitinol rod and are, therefore, sharp. Even though these ends are sewn to the tube graft in the prior
10 art, the possibility of tearing the vessel wall still exists. It is, therefore, desirable to not provide the support rod with sharp ends that could puncture the vessel in which the stent graft is placed.

The two ends of the longitudinal support member 40 of the present invention do not end abruptly. Instead, each end of the longitudinal support member loops 47 back upon itself
15 such that the end of the longitudinal support member along the axis of the stent graft is not sharp and, instead, presents an exterior of a circular or oval shape when viewed from the ends 12, 14 of the graft sleeve 10. Such a configuration substantially prevents the possibility of tearing the vessel wall and also provides additional longitudinal support at the oval shape by having two longitudinally extending sides of the oval 47.

20 In addition, in another embodiment, the end of the longitudinal support member may be connected to the second proximal stent 28 and to the most distal stent. This configuration would allow the longitudinal support member to be affixed to stent 28 (see FIG. 1) and the most distal stent for support while still allowing for the gimbaled feature of the proximal end of the stent graft to be maintained.

25 A significant feature of the longitudinal support member 40 is that the ends of the longitudinal support member 40 may not extend all the way to the two ends 12, 14 of the graft sleeve 10. Instead, the longitudinal support member 40 terminates at or prior to the second-to-last stent 28 at the proximal end 12, and, if desired, prior to the second-to-last stent 28' at the distal end 14 of the graft sleeve 10. Such an ending configuration (whether
30 proximal only or both proximal and distal) is chosen for a particular reason -- when the longitudinal support member 40 ends before either of the planes defined by cross-sectional lines 52, 52', the sleeve 10 and the stents 20 connected thereto respectively form gimbaled portions 50, 50'. In other words, when a grasping force acting upon the gimbaled ends 50,

50' moves or pivots the cross-sectional plane defining each end opening of the graft sleeve 10 about the longitudinal axis 11 starting from the planes defined by the cross-sectional lines 52, 52', then the moving portions 50, 50' can be oriented at any angle γ about the center of the circular opening in all directions (360 degrees), as shown in FIG. 8. The
5 natural gimbal, thus, allows the ends 50, 50' to be inclined in any radial direction away from the longitudinal axis 11.

Among other things, the gimbaleed ends 50, 50' allow each end opening to dynamically align naturally to the curve of the vessel in which it is implanted. A significant advantage of the gimbaleed ends 50, 50' is that they limit propagation of the forces acting upon the
10 separate parts. Specifically, a force that, previously, would act upon the entirety of the stent graft 1, in other words, both the end portions 50, 50' and the middle portion of the stent graft 1 (i.e., between planes 52, 52'), now principally acts upon the portion in which the force occurs. For example, a force that acts only upon one of the end portions 50, 50' substantially does not propagate into the middle portion of the stent graft 1 (i.e., between
15 planes 52, 52'). More significantly, however, when a force acts upon the middle portion of the stent graft 1 (whether moving longitudinally, axially (dilation), or in a torqued manner), the ends 50, 50', because they are gimbaleed, remain relatively completely aligned with the natural contours of the vessel surrounding the respective end 50, 50' and have virtually none of the force transferred thereto, which force could potentially cause the ends to grate,
20 rub, or shift from their desired fixed position in the vessel. Accordingly, the stent graft ends 50, 50' remain fixed in the implanted position and extend the seating life of the stent graft 1.

Another advantage of the longitudinal support member 40 is that it increases the columnar strength of the graft stent 1. Specifically, the material of the graft sleeve can be compressed
25 easily along the longitudinal axis 11, a property that remains true even with the presence of the stents 20 so long as the stents 20 are attached to the graft sleeve 10 with a spacing between the distal apices 24 of one stent 20 and the proximal apices 22 of the next adjacent stent 20. This is especially true for the amount of force imparted by the flow of blood along the extent of the longitudinal axis 11. However, with the longitudinal support member 40
30 attached according to the present invention, longitudinal strength of the stent graft 1 increases to overcome the longitudinal forces imparted by blood flow.

Another benefit imparted by having such increased longitudinal strength is that the stent graft 1 is further prevented from migrating in the vessel because the tube graft is not

compressing and expanding in an accordion-like manner -- movement that would, inherently, cause graft migration.

A further measure for preventing migration of the stent graft 1 is to equip at least one of any of the individual stents 20, 30 or the longitudinal support member 40 with protuberances 60, such as barbs or hooks (FIG. 3). See, e.g., United States Patent Publication 2002/0052660 to Greenhalgh. In the preferred embodiment of the present invention, the stents 20, 30 are secured to the outer circumferential surface 16 of the graft sleeve 10. Accordingly, if the stents 20 (or connected portions of stent 30) have protuberances 60 protruding outwardly, then such features would catch the interior wall of the vessel and add to the prevention of stent graft 1 migration. Such an embodiment can be preferred for aneurysms but is not preferred for the fragile characteristics of dissections because such protuberances 60 can excoriate the inner layer(s) of the vessel and cause leaks between layers, for example.

As shown in FIG. 9, the stent graft 1 is not limited to a single graft sleeve 10. Instead, the entire stent graft can be a first stent graft 100 having all of the features of the stent graft 1 described above and a second stent graft 200 that, instead of having a circular extreme proximal end 12, as set forth above, has a proximal end 212 with a shape following the contour of the most proximal stent 220 and is slightly larger in circumference than the distal circumference of the first stent graft 100. Therefore, an insertion of the proximal end 212 of the second stent graft 200 into the distal end 114 of the first stent graft 100 results, in total, in a two-part stent graft. Because blood flows from the proximal end 112 of the first stent graft 100 to the distal end 214 of the second stent graft 200, it is preferable to have the first stent graft 100 fit inside the second stent graft 200 to prevent blood from leaking out therebetween. This configuration can be achieved by implanting the devices in reverse order (first implant graft 200 and, then, implant graft 100. Each of the stent grafts 100, 200 can have its own longitudinal support member 40 as needed.

It is not significant if the stent apices of the distal-most stent of the first stent graft 100 are not aligned with the stent apices of the proximal-most stent 220 of the second stent graft 200. What is important is the amount of junctional overlap between the two grafts 100, 200.

30 Delivery System

As set forth above, the prior art includes many different systems for endoluminally delivering a prosthesis, in particular, a stent graft, to a vessel. Many of the delivery systems have similar parts and most are guided along a guidewire that is inserted, typically, through

an insertion into the femoral artery near a patient's groin prior to use of the delivery system. To prevent puncture of the arteries leading to and including the aorta, the delivery system is coaxially connected to the guidewire and tracks the course of the guidewire up to the aorta. The parts of the delivery system that will track over the wire are, therefore, sized to have an

5 outside diameter smaller than the inside diameter of the femoral artery of the patient. The delivery system components that track over the guidewire include the stent graft and are made of a series of coaxial lumens referred to as catheters and sheaths. The stent graft is constrained, typically, by an outer catheter, requiring the stent graft to be compressed to fit inside the outer catheter. Doing so makes the portion of the delivery system that constrains

10 the stent graft very stiff, which, therefore, reduces that portion's flexibility and makes it difficult for the delivery system to track over the guidewire, especially along curved vessels such as the aortic arch. In addition, because the stent graft exerts very high radial forces on the constraining catheter due to the amount that it must be compressed to fit inside the catheter, the process of deploying the stent graft by sliding the constraining catheter off of

15 the stent graft requires a very high amount of force, typically referred to as a deployment force. Also, the catheter has to be strong enough to constrain the graft, requiring it to be made of a rigid material. If the rigid material is bent, such as when tracking into the aortic arch, the rigid material tends to kink, making it difficult if not impossible to deploy the stent graft.

20 Common features of vascular prosthesis delivery systems include a tapered nose cone fixedly connected to a guidewire lumen, which has an inner diameter substantially corresponding to an outer diameter of the guidewire such that the guidewire lumen slides easily over and along the guidewire. A removable, hollow catheter covers and holds a compressed prosthesis in its hollow and the catheter is fixedly connected to the guidewire

25 lumen. Thus, when the prosthesis is in a correct position for implantation, the physician withdraws the hollow catheter to gradually expose the self-expanding prosthesis from its proximal end towards its distal end. When the catheter has withdrawn a sufficient distance from each portion of the expanding framework of the prosthesis, the framework can expand to its native position, preferably, a position that has a diameter at least as great as the inner

30 diameter of the vessel wall to, thereby, tightly affix the prosthesis in the vessel. When the catheter is entirely withdrawn from the prosthesis and, thereby, allows the prosthesis to expand to the diameter of the vessel, the prosthesis is fully expanded and connected endoluminally to the vessel along the entire extent of the prosthesis, e.g., to treat a

dissection. When treating an aneurysm, for example, the prosthesis is in contact with the vessel's proximal and distal landing zones when completely released from the catheter. At such a point in the delivery, the delivery system can be withdrawn from the patient. The prosthesis, however, cannot be reloaded in the catheter if implantation is not optimal.

5 The aorta usually has a relatively straight portion in the abdominal region and in a lower part of the thoracic region. However, in the upper part of the thoracic region, the aorta is curved substantially, traversing an upside-down U-shape from the back of the heart over to the front of the heart. As explained above, prior art delivery systems are relatively hard and inflexible (the guidewire/catheter portion of the prior art delivery systems). Therefore, if
10 the guidewire/catheter must traverse the curved portion of the aorta, it will kink as it is curved or it will press against the top portion of the aortic curve, possibly puncturing the aorta if the diseased portion is located where the guidewire/catheter is exerting its force. Such a situation must be avoided at all costs because the likelihood of patient mortality is high. The prior art does not provide any way for substantially reducing the stress on the
15 curved portion of the aorta or for making the guidewire/catheter sufficiently flexible to traverse the curved portion without causing damage to the vessel.

The present invention, however, provides significant features not found in the prior art that assist in placing a stent graft in a curved portion of the aorta in a way that substantially reduces the stress on the curved portion of the aorta and substantially reduces the insertion
20 forces needed to have the compressed graft traverse the curved portion of the aorta. As set forth above, the longitudinal support member 40 is pre-formed in a desired spiral/helical shape before being attached to the graft sleeve 10 and, in a preferred embodiment, is curved in a patient-customized way to accommodate the anticipated curve of the actual vessel in which the graft will be implanted. As such, optimal positioning of the stent graft 1 occurs
25 when the longitudinal support member 40 is placed substantially at the superior longitudinal surface line of the curved aorta (with respect to anatomical position). Such placement can be effected in two ways. First, the stent graft 1, the support member 40, or any portion of the delivery system that is near the target site can be provided with radiopaque markers that are monitored by the physician and used to manually align the support member 40 in what
30 is perceived as an optimal position. The success of this alignment technique, however, is dependent upon the skill of the physician. Second, the delivery system can be made to automatically align the support member 40 at the optimal position. No such system existed in the prior art. However, the delivery system of the present invention provides such an

alignment device, thereby, eliminating the need for physician guesswork as to the three-dimensional rotational position of the implanted stent graft 1. This alignment device is explained in further detail below with respect to FIGS. 64 to 67.

The delivery system of the present invention also has a very simple to use handle assembly.

- 5 The handle assembly takes advantage of the fact that the inside diameter of the aorta is substantially larger than the inside diameter of the femoral arteries. The present invention, accordingly, uses a two-stage approach in which, after the device is inserted in through the femoral artery and tracks up into the abdominal area of the aorta (having a larger diameter (see FIG. 19) than the femoral artery), a second stage is deployed (see FIG. 20) allowing a
- 10 small amount of expansion of the stent graft while still constrained in a sheath; but this sheath, made of fabric/woven polymer or similar flexible material, is very flexible. Such a configuration gives the delivery system greater flexibility for tracking, reduces deployment forces because of the larger sheath diameter, and easily overcome kinks because the sheath is made of fabric.
- 15 To describe the delivery system of the present invention, the method for operating the delivery assembly 600 will be described first in association with FIGS. 10, 11, and 12. Thereafter, the individual components will be described to allow a better understanding of how each step in the process is effected for delivering the stent graft 1 to any portion of the aorta 700 (see FIGS. 19 to 24), in particular, the curved portion 710 of the aorta.
- 20 Initially, the distal end 14 of the stent graft 1 is compressed and placed into a hollow, cup-shaped, or tubular-shaped graft holding device, in particular, the distal sleeve 644 (see, e.g., FIG. 25). At this point, it is noted that the convention for indicating direction with respect to delivery systems is opposite that of the convention for indicating direction with respect to stent grafts. Therefore, the proximal direction of the delivery system is that portion closest
- 25 to the user/physician employing the system and the distal direction corresponds to the portion farthest away from the user/physician, i.e., towards the distal-most nose cone 632. The distal sleeve 644 is fixedly connected to the distal end of the graft push lumen 642, which lumen 642 provides an end face for the distal end 14 of the stent graft 1.
- Alternatively, the distal sleeve 644 can be removed entirely. In such a configuration, as
- 30 shown in FIG. 12, for example, the proximal taper of the inner sheath 652 can provide the measures for longitudinally holding the compressed distal end of the graft 1. If the sleeve 644 is removed, it is important to prevent the distal end 14 of the stent graft 1 from entering the space between the interior surface of the hollow sheath lumen 654 and the exterior

surface of the graft push lumen 642 slidably disposed in the sheath lumen 654. Selecting a radial thickness of the space to be less than the diameter of the wire making up the stent 20, 30 (in particular, no greater than half a diameter thereof) insures reliable movement of the distal end 14 of the stent graft 1. In another alternative configuration shown in FIG. 68, the

5 distal sleeve 644 can be a disk-shaped buttress 644 present at the distal end of the graft push lumen 642. An example configuration can provide the buttress 644 with a hollow proximal insertion peg 6442, a hollow distal stiffening tube 6444, and an intermediate buttress wall 6446. The buttress 644 is concentric to the center axis of the delivery system 600 and allows the co-axial guidewire lumen 620 and apex release lumen 640 to pass therethrough.

10 The peg 6442 allows for easy connection to the graft push lumen 643. The stiffening tube 64 creates a transition in stiffness from the graft push lumen 642 to the apex release lumen 620 and guidewire lumen 640 and provides support to the lumen 620, 640 located therein. Such a transition in stiffness reduces any possibility of kinking at the distal end of the graft push lumen 642 and aids in transferring force from the graft push lumen 642 to the lumen

15 therein 620, 640 when all are in a curved orientation. The buttress wall 6446 provides a flat surface that will contact the distal-end-facing side of the stent graft 1 and can be used to push the stent graft distally when the graft push lumen 642 is moved distally. The alternative configuration of the buttress 644 insures that the stent graft 1 does not become impinged within the graft push lumen 642 and the lumen therein 620, 640 when these

20 components are moved relative to each other.

As set forth in more detail below, each apex 32 of the bare stent 30 is, then, loaded into the apex capture device 634 so that the stent graft 1 is held at both its proximal and distal ends. The loaded distal end 14, along with the distal sleeve 644 and the graft push lumen 642, are, in turn, loaded into the inner sheath 652, thus, further compressing the entirety of the stent

25 graft 1. The captured bare stent 30, along with the nose cone assembly 630 (including the apex capture device 634), is loaded until the proximal end of the nose cone 632 rests on the distal end of the inner sheath 652. The entire nose cone assembly 630 and sheath assembly 650 is, then, loaded proximally into the rigid outer catheter 660, further compressing the stent graft 1 (resting inside the inner sheath 652) to its fully compressed position for later

30 insertion into a patient. See FIG. 63.

The stent graft 1 is, therefore, held both at its proximal and distal ends and, thereby, is both pushed and pulled when moving from a first position (shown in FIG. 19 and described below) to a second position (shown in FIG. 21 and described below). Specifically, pushing

is accomplished by the non-illustrated interior end face of the hollow distal sleeve 644 (or the taper 653 of the inner sheath 652) and pulling is accomplished by the hold that the apex capture device 634 has on the apices 32 of the bare stent 30.

The assembly 600 according to the present invention tracks along a guidewire 610 already
5 inserted in the patient and extending through the aorta and up to, but not into, the left ventricle of the heart 720. Therefore, a guidewire 610 is inserted through the guidewire lumen 620 starting from the nose cone assembly 630, through the sheath assembly 650, through the handle assembly 670, and through the apex release assembly 690. The guidewire 610 extends out the proximal-most end of the assembly 600. The guidewire
10 lumen 620 is coaxial with the nose cone assembly 630, the sheath assembly 650, the handle assembly 670, and the apex release assembly 690 and is the innermost lumen of the assembly 600 immediately surrounding the guidewire 610.

Before using the delivery system assembly 600, all air must be purged from inside the assembly 600. Therefore, a liquid, such as sterile U.S.P. saline, is injected through a non-
15 illustrated tapered luer fitting to flush the guidewire lumen at a non-illustrated purge port located near a proximal end of the guidewire lumen. Second, saline is also injected through the luer fitting 612 of the lateral purge-port (see FIG. 11), which liquid fills the entire internal co-axial space of the delivery system assembly 600. It may be necessary to
20 manipulate the system to facilitate movement of the air to be purged to the highest point of the system.

After purging all air, the system can be threaded onto the guidewire and inserted into the patient. Because the outer catheter 660 has a predetermined length, the fixed front handle 672 can be disposed relatively close to the entry port of the femoral artery. It is noted, however, that the length of the outer catheter 660 is sized such that it will not have the fixed
25 proximal handle 672 directly contact the entry port of the femoral artery in a patient who has the longest distance between the entry port and the thoracic/abdominal junction 742, 732 of the aorta expected in a patient (this distance is predetermined). Thus, the delivery assembly 600 of the present invention can be used with typical anatomy of the patient. Of course, the assembly 600 can be sized to any usable length.

30 The nose cone assembly 630 is inserted into a patient's femoral artery and follows the guidewire 610 until the nose cone 632 reaches the first position at a level of the celiac axis. The first position is shown in FIG. 19. The nose cone assembly 630 is radiopaque, whether wholly or partially, to enable the physician to determine fluoroscopically, for example, that

the nose cone assembly 630 is in the first position. For example, the nose cone 632 can have a radiopaque marker 631 anywhere thereon or the nose cone 632 can be entirely radiopaque.

After the nose cone assembly 630 is in the first position shown in FIG. 19, the locking ring
5 676 is placed from its neutral position N, shown in FIG. 10, into its advancement position A, shown in FIG. 11. As will be described below, placing the locking ring 676 into its advancement position A allows both the nose cone assembly 630 and the internal sheath assembly 650 to move as one when the proximal handle 678 is moved in either the proximal or distal directions because the locking ring 676 radially locks the graft push lumen 642 to
10 the lumens of the apex release assembly 690 (including the guidewire lumen 620 and an apex release lumen 640). The locking ring 676 is fixedly connected to a sheath lumen 654. Before describing how various embodiments of the handle assembly 670 function, a summary of the multi-lumen connectivity relationships, throughout the neutral N, advancement A, and deployment D positions, is described.

15 When the locking ring is in the neutral position N shown in FIG. 10, the pusher clasp spring 298 shown in FIG. 48 and the proximal spring 606 shown in FIG. 52 are both disengaged. This allows free movement of the graft push lumen 642 with the guidewire lumen 620 and the apex release lumen 640 within the handle body 674.

When the locking ring 676 is moved into the advancement position A, shown in FIG. 11,
20 the pusher clasp spring 298 shown in FIG. 48 is engaged and the proximal spring 606 shown in FIG. 52 is disengaged. The sheath lumen 654 (fixedly attached to the inner sheath 652) is, thereby, locked to the graft push lumen 642 (fixedly attached to the distal sleeve 644) so that, when the proximal handle 678 is moved toward the distal handle 672, both the sheath lumen 654 and the graft push lumen 642 move as one. At this point, the graft push
25 lumen 642 is also locked to both the guidewire lumen 620 and the apex release lumen 640 (which are locked to one another through the apex release assembly 690 as set forth in more detail below). Accordingly, as the proximal handle 678 is moved to the second position, shown with dashed lines in FIG. 11, the sheath assembly 650 and the nose cone assembly 630 progress distally out of the outer catheter 660 as shown in FIGS. 20 and 21 and with
30 dashed lines in FIG. 11.

At this point, the sheath lumen 654 needs to be withdrawn from the stent graft 1 to, thereby, expose the stent graft 1 from its proximal end 12 to its distal end 14 and, ultimately, entirely off of its distal end 14. Therefore, movement of the locking ring 676 into the deployment

position D will engage the proximal spring 606 shown in FIG. 52 and disengage the pusher clasp spring 298 shown in FIG. 48. Accordingly, the graft push lumen 642 along with the guidewire lumen 620 and the apex release lumen 640 are locked to the handle body 674 so as not to move with respect to the handle body 674. The sheath lumen 654 is unlocked from the graft push lumen 642. Movement of the distal handle 678 back to the third position (proximally), therefore, pulls the sheath lumen 654 proximally, thus, proximally withdrawing the inner sheath 652 from the stent graft 1.

At this point, the delivery assembly 600 only holds the bare stent 30 of the stent graft 1. Therefore, final release of the stent graft 1 occurs by releasing the bare stent 30 from the nose cone assembly 630, which is accomplished using the apex release assembly 690 as set forth below.

In order to explain how the locking and releasing of the lumen occur as set forth above, reference is made to FIGS. 33 to 62.

FIG. 33 is a cross-sectional view of the proximal handle 678 and the locking ring 676. A pusher clasp rotator 292 is disposed between a clasp sleeve 614 and the graft push lumen 642. A specific embodiment of the pusher clasp rotator 292 is illustrated in FIGS. 34 through 39. Also disposed between the clasp rotator 292 and the graft push lumen 642 is a rotator body 294, which is directly adjacent the graft push lumen 642. A specific embodiment of the rotator body 294 is illustrated in FIGS. 40 through 43. Disposed between the rotator body 294 and the sheath lumen 654 is a pusher clasp body 296, which is fixedly connected to the rotator body 294 and to the locking ring 676. A specific embodiment of the pusher clasp body 296 is illustrated in FIGS. 44 through 46. A pusher clasp spring 298 operatively connects the pusher clasp rotator 292 to the rotator body 294 (and, thereby, the pusher clasp body 296).

An exploded view of these components is presented in FIG. 48, where an O-ring 293 is disposed between the rotator body 294 and the pusher clasp body 296. As shown in the plan view of FIG. 47, a crimp ring 295 connects the sheath lumen 654 to the distal projection 297 of the pusher clasp body 296. A hollow handle body 674 (see FIGS. 10, 11, and 33), on which the proximal handle 678 and the locking ring 676 are slidably mounted, holds the pusher clasp rotator 292, the rotator body 294, the pusher clasp body 296, and the pusher clasp spring 298 therein. This entire assembly is rotationally mounted to the distal handle 672 for rotating the stent graft 1 into position (see FIGS. 23 and 24 and the

explanations thereof below). A specific embodiment of the handle body 674 is illustrated in FIG. 49.

A setscrew 679 extends from the proximal handle 678 to contact a longitudinally helixed groove in the pusher clasp rotator 292 (shown in FIGS. 36 and 38). Thus, when moving the proximal handle 678 proximally or distally, the pusher clasp rotator 292 rotates clockwise or counter-clockwise.

An alternative embodiment of the locking ring 676 is shown in FIGS. 50 et seq., which is the preferred embodiment because, instead of applying a longitudinal movement to rotate the pusher clasp spring 298 through the cam/follower feature of the proximal handle 678 and pusher clasp rotator 292, a rotating locking knob 582 is located at the proximal end of the handle body 674. The knob 582 has three positions that are clearly shown in FIG. 51: a neutral position N, an advancement position A, and a deployment position D. The functions of these positions N, A, D correspond to the positions N, A, D of the locking ring 676 and the proximal handle 678 as set forth above.

In the alternative embodiment, a setscrew 584 is threaded into the clasp sleeve 614 through a slot 675 in the handle body 674 and through a slot 583 in the knob 582 to engage the locking knob 582. Because of the x-axis orientation of the slot 583 in the knob 582 and the y-axis orientation of the slot 675 in the handle body 674, when the knob 582 is slid over the end of the handle body 674 and the setscrew 584 is screwed into the clasp sleeve 614, the knob 582 is connected fixedly to the handle body 674. When the locking knob 582 is, thereafter, rotated between the neutral N, advancement A, and deployment D positions, the clasp sleeve 614 rotates to actuate the spring lock (see FIGS. 48 and 52).

A setscrew 586, shown in FIG. 53, engages a groove 605 in the proximal clasp assembly 604 to connect the proximal clasp assembly 604 to the clasp sleeve 614 but allows the clasp sleeve 614 to rotate around the clasp body 602. The clasp sleeve 614 is shown in FIGS. 50 and 53 and, in particular, in FIGS. 59 to 62. The proximal clasp assembly 604 of FIG. 53 is more clearly shown in the exploded view of FIG. 52. The proximal clasp assembly 604 is made of the components including a proximal spring 606, a locking washer 608, a fastener 603 (in particular, a screw fitting into internal threads of the proximal clasp body 602), and a proximal clasp body 602. The proximal clasp body 602 is shown, in particular, in FIGS. 54 through 58. The proximal clasp assembly 604 is connected fixedly to the handle body 674, preferably, with a screw 585 shown in FIG. 50 and hidden from view in FIG. 51 under knob 582.

The handle body 674 has a position pin 592 for engaging in position openings at the distal end of the locking knob 582. The position pin 592 can be a setscrew that only engages the handle body 674. When the locking knob 582 is pulled slightly proximally, therefore, the knob can be rotated clockwise or counter-clockwise to place the pin 592 into the position openings corresponding to the advancement A, neutral N, and deployment D positions. As shown in FIG. 18, to begin deployment of the stent graft 1, the user/physician grasps both the distal handle 672 and the proximal handle 678 and slides the proximal handle 678 towards the distal handle 672 in the direction indicated by arrow A. This movement, as shown in FIGS. 19 to 21, causes the flexible inner sheath 652, holding the compressed stent graft 1 therein, to emerge progressively from inside the outer catheter 660. Such a process allows the stent graft 1, while constrained by the inner sheath 652, to expand to a larger diameter shown in FIG. 12, this diameter being substantially larger than the inner diameter of the outer catheter 660 but smaller than the inner diameter of the vessel in which it is to be inserted. Preferably, the outer catheter 660 is made of a polymer (co-extrusions or teflons) and the inner sheath 652 is made of a material, such as a fabric/woven polymer or other similar material. Therefore, the inner sheath 652 is substantially more flexible than the outer catheter 660.

It is noted, at this point, that the inner sheath 652 contains a taper 653 at its proximal end, distal to the sheath's 652 connection to the sheath lumen 654 (at which connection the inner sheath 652 has a similar diameter to the distal sleeve 644 and works in conjunction with the distal sleeve 644 to capture the distal end 14 of the stent graft 1. The taper 653 provides a transition that substantially prevents any kinking of the outer catheter 660 when the stent graft 1 is loaded into the delivery assembly 600 (as in the position illustrated in FIGS. 10 and 11) and, also, when the outer catheter 660 is navigating through the femoral and iliac vessels. One specific embodiment of the sheath lumen 654 has a length between approximately 30 and approximately 40 inches, in particular, 36 inches, an outer diameter of between approximately 0.20 and approximately 0.25 inches, in particular 0.238 inches, and an inner diameter between approximately 0.18 and approximately 0.22 inches, in particular, 0.206 inches.

When the proximal handle 678 is moved towards its distal position, shown by the dashed lines in FIG. 11, the nose cone assembly 630 and the sheath assembly 650 move towards a second position where the sheath assembly 650 is entirely out of the outer catheter 660 as shown in FIGS. 20 and 21. As can be seen most particularly in FIGS. 20 and 21, as the

nose cone assembly 630 and the sheath assembly 650 are emerging out of the outer catheter 660, they are traversing the curved portion 710 of the descending aorta. The tracking is accomplished visually by viewing radiopaque markers on various portions of the delivery system and/or the stent graft 1 with fluoroscopic measures. Such markers will be described in further detail below. The delivery system can be made visible, for example, by the nose cone 630 being radiopaque or containing radiopaque materials.

It is noted that if the harder outer catheter 660 was to have been moved through the curved portion 710 of the aorta 700, there is a great risk of puncturing the aorta 700, and, particularly, a diseased portion 744 of the proximal descending aorta 710 because the outer catheter 660 is not as flexible as the inner sheath 652. But, because the inner sheath 652 is so flexible, the nose cone assembly 630 and the sheath assembly 650 can be extended easily into the curved portion 710 of the aorta 700 with much less force on the handle than previously needed with prior art systems while, at the same time, imparting harmless forces to the intraluminal surface of the curved aorta 710 due to the flexibility of the inner sheath 652.

At the second position shown in FIG. 21, the user/physician, using fluoroscopic tracking of radiopaque markers (e.g., marker 631) on any portion of the nose cone or on the stent graft 1 and/or sheath assemblies 630, 650, for example, makes sure that the proximal end 112 of the stent graft 1 is in the correct longitudinal position proximal to the diseased portion 744 of the aorta 700. Because the entire inserted assembly 630, 650 in the aorta 700 is still rotationally connected to the portion of the handle assembly 670 except for the distal handle 672 (distal handle 672 is connected with the outer sheath 660 and rotates independently of the remainder of the handle assembly 670), the physician can rotate the entire inserted assembly 630, 650 clockwise or counterclockwise (indicated in FIG. 20 by arrow B) merely by rotating the proximal handle 678 in the desired direction. Such a feature is extremely advantageous because the non-rotation of the outer catheter 660 while the inner sheath 652 is rotating eliminates stress on the femoral and iliac arteries when the rotation of the inner sheath 652 is needed and performed.

Accordingly, the stent graft 1 can be pre-aligned by the physician to place the stent graft 1 in the optimal circumferential position. FIG. 23 illustrates the longitudinal support member 40 not in the correct superior position and FIG. 24 illustrates the longitudinal support member 40 in the correct superior position. The optimal superior surface position is, preferably, near the longest superior longitudinal line along the circumference of the curved

portion of the aorta as shown in FIGS. 23 and 24. As set forth above, when the longitudinal support member 40 extends along the superior longitudinal line of the curved aorta, the longitudinal support member 40 substantially eliminates any possibility of forming a kink in the inferior radial curve of the stent graft 1 during use and also allows transmission of

5 longitudinal forces exerted along the inside lumen of the stent graft 1 to the entire longitudinal extent of the stent graft 1, thereby allowing the entire outer surface of the stent graft 1 to resist longitudinal migration. Because of the predefined curvature of the support member 40, the support member 40 cannot align exactly and entirely along the superior longitudinal line of the curved aorta. Accordingly, an optimal superior surface position of

10 the support member 40 places as much of the central portion of the support member 40 (between the two ends 47 thereof) as possible close to the superior longitudinal line of the curved aorta. A particularly desirable implantation position has the superior longitudinal line of the curved aorta intersecting the proximal half of the support member 40 -- the proximal half being defined as that portion of the support member 40 located between the

15 centerline 45 and the proximal support member loop 47. However, for adequate implantation purposes, the centerline 45 of the support member 40 can be as much as seventy circumferential degrees away from either side of the superior longitudinal line of the curved aorta. Adequate implantation can mean that the stent graft 1 is at least approximately aligned. When implantation occurs with the stent graft 1 being less than

20 seventy degrees, for example, less than forty degrees, away from either side of the superior longitudinal line of the curved aorta, then it is substantially aligned.

In prior art stent grafts and stent graft delivery systems, the stent graft is, typically, provided with symmetrically-shaped radiopaque markers along one longitudinal line and at least one other symmetrically-shaped radiopaque marker disposed along another longitudinal line on

25 the opposite side (one-hundred eighty degrees (180°)) of the stent graft. Thus, using two-dimensional fluoroscopic techniques, the only way to determine if the stent graft is in the correct rotational position is by having the user/physician rotate the stent graft in both directions until it is determined that the first longitudinal line is superior and the other longitudinal line is anterior. Such a procedure requires more work by the physician and is,

30 therefore, undesirable.

According to a preferred embodiment of the invention illustrated in FIGS. 27 and 28, unique radiopaque markers 232, 234 are positioned on the stent graft 1 to assist the user/physician in correctly positioning the longitudinal support member 40 in the correct

aortic superior surface position with only one directional rotation, which corresponds to the minimal rotation needed to place the stent graft 1 in the rotationally correct position.

Specifically, the stent graft 1 is provided with a pair of symmetrically shaped but diametrically opposed markers 232, 234 indicating to the user/physician which direction the stent graft 1 needs to be rotated to align the longitudinal support member 40 to the superior longitudinal line of the curved aorta (with respect to anatomical position). Preferably, the markers 232, 234 are placed at the proximate end 12 of the graft sleeve 10 on opposite sides (one-hundred eighty degrees (180°)) of the graft sleeve 10.

The angular position of the markers 232, 234 on the graft sleeve 10 is determined by the position of the longitudinal support member 40. In a preferred embodiment, the support member 40 is between the two markers 232, 234. To explain such a position, if the marker 232 is at a 0 degree position on the graft sleeve 10 and the marker 234 is at a one-hundred eighty degree (180°) position, then the centerline 45 of the support member 40 is at a ninety degree position. However, an alternative position of the markers can place the marker 234 ninety degrees away from the first degree 41 (see FIG. 1). Such a positioning is dependent somewhat upon the way in which the implantation is to be viewed by the user/physician and can be varied based on other factors. Thus, the position can be rotated in any beneficial way.

Preferred ancillary equipment in endovascular placement of the stent graft 1 is a fluoroscope with a high-resolution image intensifier mounted on a freely angled C-arm. The C-arm can be portable, ceiling, or pedestal mounted. It is important that the C-arm have a complete range of motion to achieve AP to lateral projections without moving the patient or contaminating the sterile field. Capabilities of the C-arm should include: Digital Subtraction Angiography, High-resolution Angiography, and Roadmapping.

For introduction of the delivery system into the groin access arteries, the patient is, first, placed in a sterile field in a supine position. To determine the exact target area for placement of the stent graft 1, the C-arm is rotated to project the patient image into a left anterior oblique projection, which opens the radial curve of the thoracic aortic arch for optimal visualization without superimposition of structures. The degree of patient rotation will vary, but is usually 40 to 50 degrees. At this point, the C-arm is placed over the patient with the central ray of the fluoroscopic beam exactly perpendicular to the target area. Such placement allows for the markers 232, 234 to be positioned for correct placement of the stent graft 1. Failure to have the central ray of the fluoroscopic beam perpendicular to the

target area can result in parallax, leading to visual distortion to the patient anatomy due to the divergence of the fluoroscopic x-ray beam, with a resultant misplacement of the stent graft 1. An angiogram is performed and the proposed stent graft landing zones are marked on the visual monitor. Once marked, neither the patient, the patient table, nor the
5 fluoroscopic C-arm can be moved, otherwise, the reference markers become invalid. The stent graft 1 is, then, placed at the marked landing zones.

In a preferred embodiment, the markers 232, 234 are hemispherical, in other words, they have the approximate shape of a "D". This shape is chosen because it provides special, easy-to-read indicators that instantly direct the user/physician to the correct placement
10 position for the longitudinal support member 40. FIG. 27, for example, illustrates a plan view of the markers 232, 234 when they are placed in the upper-most superior longitudinal line of the curved aorta. The correct position is indicated clearly because the two hemispheres have the flat diameters aligned on top of or immediately adjacent to one another such that a substantially complete circle is formed by the two hemispherically
15 rounded portions of the markers 232, 234. This position is also indicated in the perspective view of FIG. 28.

Each of FIGS. 27 and 28 have been provided with examples where the markers 232, 234 are not aligned and, therefore, the stent graft 1 is not in the correct insertion position. For example, in FIG. 27, two markers 232', 234' indicate a misaligned counter-clockwise-rotated stent graft 1 when viewed from the plane 236 at the right end of the stent graft 1 of
20 FIG. 23 looking toward the left end thereof and down the axis 11. Thus, to align the markers 232', 234' in the most efficient way possible (the shortest rotation), the user/physician sees that the distance between the two flat diameters is closer than the distance between the highest points of the hemispherical curves. Therefore, it is known that
25 the two flat diameters must be joined together by rotating the stent graft 1 clockwise.

FIG. 28 has also been provided with two markers 232'', 234'' indicating a misaligned clockwise-rotated stent graft 1 when viewed from the plane 236 at the right end of the stent graft 1 of FIG. 27 looking toward the left end thereof and down the axis 11. Thus, to align the markers 232'', 234'' in the most efficient way possible (the shortest rotation), the
30 user/physician sees that the distance between the highest points of the hemispherical curves is smaller than the distance between the two flat diameters. Therefore, it is known that the two flat diameters must be joined together by rotating the stent graft 1 in the direction that

the highest points of the hemispherical curves point; in other words, the stent graft 1 must be rotated counter-clockwise.

A significant advantage provided by the diametrically opposed symmetric markers 232, 234 is that they can be used for migration diagnosis throughout the remaining life of a patient after the stent graft 1 has been placed inside the patient's body. If fluoroscopic or radiographic techniques are used any time after the stent graft 1 is inserted in the patient's body, and if the stent graft 1 is viewed from the same angle as it was viewed when placed therein, then the markers' 232, 234 relative positions observed should give the examining individual a very clear and instantaneous determination as to whether or not the stent graft 1 has migrated in a rotational manner.

The hemispherical shape of the markers 232, 234 are only provided as an example shape. The markers 232, 234 can be any shape that allows a user/physician to distinguish alignment and direction of rotation for alignment. For example, the markers 232, 234 can be triangular, in particular, an isosceles triangle having the single side be visibly longer or shorter than the two equal sides.

As set forth above, alignment to the optimal implantation position is dependent upon the skill of the physician(s) performing the implantation. The present invention improves upon the embodiments having longitudinal and rotational radiopaque markers 232, 234 and substantially eliminates the need for rotational markers. Specifically, it is noted that the guidewire 610 travels through a curve through the aortic arch towards the heart 720. It is, therefore, desirable to pre-shape the delivery system to match the aorta of the patient.

The guidewire lumen 620 is formed from a metal, preferably, stainless steel. Thus, the guidewire lumen 620 can be deformed plastically into any given shape. In contrast, the apex release lumen 640 is formed from a polymer, which tends to retain its original shape and cannot plastically deform without an external force, e.g., the use of heat. Therefore, to effect the pre-shaping of the delivery assembly 600, the guidewire lumen 620, as shown in FIG. 64, is pre-shaped with a curve at a distal-most area 622 of the lumen 620. The pre-shape can be determined, for example, using the fluoroscopic pre-operative techniques described above, in which the guidewire lumen 620 can be customized to the individual patient's aortic shape. Alternatively, the guidewire lumen 620 can be pre-shaped in a standard manner that is intended to fit an average patient. Another alternative is to provide a kit that can be used to pre-shape the guidewire lumen 620 in a way that is somewhat

tailored to the patient, for example, by providing a set of delivery systems 600 or a set of different guidewire lumens 620 that have different radii of curvature.

With the pre-curved guidewire lumen 620, when the nose cone 632 and inner sheath 652 exit the outer catheter 660 and begin to travel along the curved guidewire 610, the natural
5 tendency of the pre-curved guidewire lumen 620 will be to move in a way that will best align the two curves to one another (see FIGS. 20 and 21). The primary factor preventing the guidewire lumen 620 from rotating itself to cause such an alignment is the torque generated by rotating the guidewire lumen 620 around the guidewire 610. The friction between the aorta and the device also resists rotational motion. The delivery system 600,
10 however, is configured naturally to minimize such torque. As set forth above with respect to FIGS. 15 to 17, the guidewire lumen 620 freely rotates within the apex release lumen 640 and is only connected to the apex release lumen 640 at the proximal-most area of both lumen 620, 640. While the inner sheath 652 advances through the aortic arch, the two lumen 620, 640 are rotationally connected only at the apex release assembly 690. This
15 means that rotation of the guidewire lumen 620 about the guidewire 610 and within the apex release lumen 640 occurs along the entire length of the guidewire lumen 620. Because the metallic guidewire lumen 620 is relatively rotationally elastic along its length, rotation of the distal-most portion (near the nose cone assembly 630) with respect to the proximal-most portion (near the apex release assembly 690) requires very little force. In other words, the
20 torque resisting rotation of the distal-most portion to conform to the curve of the guidewire 610 is negligible. Specifically, the torque is so low that the force resisting the alignment of the guidewire lumen 620 to the guidewire 610 causes little, negligible, or no damage to the inside of the aorta, especially to a dissecting inner wall of a diseased aorta.

Due to the configuration of the delivery system 600 of the present invention, when the
25 guidewire lumen 620 is extended from the outer catheter 660 (along with the apex release lumen 640, the stent graft 1, the inner sheath 652 as shown in FIGS. 20 and 21, for example), the pre-shape of the guidewire lumen 620 causes automatic and natural rotation of the entire distal assembly – including the stent graft 1 -- along its longitudinal axis. This means that the length and connectivity of the guidewire lumen 620, and the material from of
30 which the guidewire lumen 620 is made, allow the entire distal assembly (1, 620, 630, 640, 650) to naturally rotate and align the pre-curved guidewire lumen 620 with the curve of the guidewire 610 – this is true even if the guidewire lumen 620 is inserted into the aorta entirely opposite the curve of the aorta (one-hundred eighty degrees (180°)). In all

circumstances, the curved guidewire lumen 620 will cause rotation of the stent graft 1 into an optimal implantation position, that is, aligning the desired portion of the support member 40 within ± 70 degrees of the superior longitudinal line of the curved aorta. Further, the torque forces acting against rotation of the guidewire lumen 620 will not be too high to
5 cause damage to the aorta while carrying out the rotation.

The self-aligning feature of the invention begins with a strategic loading of the stent graft 1 in the inner sleeve 652. To describe the placement of the supporting member 40 of the stent graft 1 relative to the curve 622 of the guidewire lumen 620, an X-Y coordinate curve plane is defined and shown in FIG. 64. In particular, the guidewire lumen 620 is curved and that
10 curve 622 defines the curve plane 624.

To insure optimal implantation, when loading the stent graft 1 into the inner sheath 652, a desired point on the supporting member 40 between the centerline 45 of the stent graft 1 and the proximal support member loop 47 is aligned to intersect the curve plane 624. The preferred, but not required, location of the desired point on the supporting member 40 is
15 located forty-five (45) degrees around the circumference of the stent graft 1 shown in FIG. 1 beginning from the first degree 41 in line with the proximal support member loop 47. When the stent graft 1 is loaded in the preferred orientation, it is ready for insertion into the inner sleeve 652. During the loading process, the stent graft 1 and the guidewire lumen 620 are held constant rotationally. After such loading, the inner sleeve 652 is retracted into the
20 outer catheter 660 and the delivery system 600 is ready for purging with saline and use with a patient.

FIGS. 65 to 67 illustrate self-alignment of the distal assembly 620, 630, 640, 650 after it is pushed out from the distal end of the outer catheter 660 (see FIGS. 20 and 21). FIG. 65 shows an aorta 700 and the distal assembly after it has traversed the iliac arteries 802 and enters the descending thoracic portion 804 of the aorta. The nose cone assembly 630 is
25 positioned just before the aortic arch 806 and the stent graft 1 is contained within the inner sheath 652. A reference line 820 is placed on the stent graft 1 at a longitudinal line of the stent graft 1 that is intended to align with the superior longitudinal line 808 (indicated with dashes) of the aortic arch 806. In FIG. 65, the reference line 820 also lies on the curved
30 plane 624 defined by the pre-curved guidewire lumen 620. As can be clearly seen from FIG. 65, the reference line 820 is positioned almost on or on the inferior longitudinal line of the curved aorta – thus, the stent graft 1 is one-hundred eighty degrees (180°) out of alignment. FIG. 66 shows the nose cone assembly 630 fully in the aortic arch 806 and the

inner sleeve 652 at the entrance of the aortic arch 806. With the self-aligning configuration of the pre-curved guidewire lumen 620, movement of the distal assembly from the position shown in FIG. 65 to the position shown in FIG. 66 causes a rotation of the reference line 820 almost ninety degrees (90°) clockwise (with respect to a view looking upward within the descending aorta) towards the superior longitudinal line 808. In FIG. 67, the nose cone assembly 630 has reached, approximately, the left subclavian artery 810. Rotational movement of the distal assembly is, now, complete, with the reference line 820 almost aligned with the superior longitudinal line 808 of the aortic arch 806. From the views of FIGS. 65 to 67, also shown is the fact that the pre-curved guidewire lumen 620 has not caused any portion of the inner sleeve 652 to push against the inner surface of the aortic arch 806 with force -- force that might exacerbate an aortic dissection.

It is noted that the guidewire lumen 620 need not be rotationally fixedly connected to the apex release lumen 640 when the apex release assembly 690 is in the locked position shown in FIGS. 15 and 16. Instead, a non-illustrated, freely rotatable coupling can be interposed anywhere along the guidewire lumen 620 (but, preferably, closer to the apex release assembly 690). This coupling would have a proximal portion rotationally fixedly connected to the to the apex release lumen 640 when the apex release assembly 690 is in the locked position shown in FIGS. 15 and 16 and a freely-rotatable distal portion that is fixedly connected to all of the guidewire lumen 620 disposed distal thereto. Thus, the guidewire lumen 620 near the sheath assembly 650 will always be freely rotatable and, thereby, allow easy and torque-free rotation of the guidewire lumen 620 about the guidewire 610.

It is also noted that the pre-curved section 622 of the guidewire lumen need not be made at the manufacturer. As shown in FIG. 69, a curving device can be provided with the delivery system 600 to allow the physician performing the implantation procedure to tailor-fit the curve 622 to the actual curve of the vessel in which the stent graft 1 is to be implanted.

Because different patients can have different aortic arch curves, a plurality of these curving devices can be provided with the delivery system 600, each of the curving devices having a different curved shape. Each device can also have two sides with each side having a different curved shape, thus, reducing the number of devices if a large number of curves are required. Further, the curving devices can all be rotationally connected on a common axle or spindle for each of transport, storage, and use.

For tailoring the curve to the patient's curved vessel, the physician can, for example, fluoroscopically view the vessel (e.g., aortic arch) and determine therefrom the needed curve

by, for example, holding up the curving device to the display. Any kind of curving device can be used to impart a bend to the guidewire lumen 620 when the guidewire lumen 620 is bent around the circumference.

Because of the predefined curvature of the support member 40, the support member 40
5 cannot align exactly and entirely along the superior longitudinal line of the curved aorta. Accordingly, an optimal superior surface position of the support member 40 places as much of the central portion of the support member 40 (between the two ends 47 thereof) as possible close to the superior longitudinal line 808 of the curved aorta. A particularly
10 desirable implantation position has the superior longitudinal line 808 of the curved aorta intersecting the proximal half of the support member 40 – the proximal half being defined as that portion of the support member 40 located between the centerline 45 and the proximal support member loop 47. However, for adequate implantation purposes, the centerline 45 of the support member 40 can be as much as seventy circumferential degrees away from either side of the superior longitudinal line of the curved aorta.

15 When the stent graft 1 is in place both longitudinally and circumferentially (FIG. 21), the stent graft 1 is ready to be removed from the inner sheath 652 and implanted in the vessel 700. Because relative movement of the stent graft 1 with respect to the vessel is no longer desired, the inner sheath 652 needs to be retracted while the stent graft 1 remains in place, i.e., no longitudinal or circumferential movement. Such immovability of the stent graft 1 is
20 insured by, first, the apex capture device 634 of the nose cone assembly 630 holding the front of the stent graft 1 by its bare stent 30 (see FIGS. 13, 22, and 23) and, second, by unlocking the locking ring 676/placing the locking ring/knob in the D position -- which allows the sheath lumen 654 to move independently from the guidewire lumen 620, apex release lumen 640, and graft push lumen 642. The apex capture device 634, as shown in
25 FIGS. 13, 14, 30 and 311 (and as will be described in more detail below), is holding each individual distal apex 32 of the bare stent 30 in a secure manner -- both rotationally and longitudinally.

The nose cone assembly 630, along with the apex capture device 634, is securely attached to the guidewire lumen 620 (and the apex release lumen 640 at least until apex release occurs).

30 The inner sheath 652 is securely attached to a sheath lumen 654, which is coaxially disposed around the guidewire lumen 620 and fixedly attached to the proximal handle 678. The stent graft 1 is also supported at its distal end by the graft push lumen 642 and the distal sleeve 644 or the taper 653 of the inner sheath 652. (The entire coaxial relationship of the

various lumen 610, 620, 640, 642, 654, and 660 is illustrated for exemplary purposes only in FIG. 25, and a portion of which can also be seen in the exploded view of the handle assembly in FIG. 50) Therefore, when the proximal handle 678 is moved proximally with the locking ring 676 in the deployment position D, the sheath lumen 654 moves proximally as shown in FIGS. 13, 22, and 23, taking the sheath 652 proximally along with it while the guidewire lumen 620, the apex release lumen 640, the graft push lumen 642, and the distal sleeve 644 remain substantially motionless and, therefore, the stent graft 1 remains both rotationally and longitudinally steady.

The stent graft 1 is, now, ready to be finally affixed to the aorta 700. To perform the implantation, the bare stent 30 must be released from the apex capture device 634. As will be described in more detail below, the apex capture device 634 shown in FIGS. 13, 14, and 29 to 32, holds the proximal apices 32 of the bare stent 30 between the distal apex head 636 and the proximal apex body 638. The distal apex head 636 is fixedly connected to the guidewire lumen 620. The proximal apex body 638, however, is fixedly connected to the apex release lumen 640, which is coaxial with both the guidewire lumen 620 and the sheath lumen 654 and disposed therebetween, as illustrated diagrammatically in FIG. 25. (As will be described in more detail below, the graft push lumen 642 is also fixedly connected to the apex release lumen 640.) Therefore, relative movement of the apex release lumen 640 and the guidewire lumen 620 separates the distal apex head 636 and a proximal apex body 638 from one another.

To cause such relative movement, the apex release assembly 690 has, in a preferred embodiment, three parts, a distal release part 692, a proximal release part 694, and an intermediate part 696 (which is shown in the form of a clip in FIGS. 16 and 26). To insure that the distal apex head 636 and the proximal apex body 638 always remain fixed with respect to one another until the bare stent 30 is ready to be released, the proximal release part 694 is formed with a distal surface 695, the distal release part 692 is formed with a proximal surface 693, and the intermediate part 696 has proximal and distal surfaces corresponding to the surfaces 695, 693 such that, when the intermediate part 696 is inserted removably between the distal surface 695 and the proximal surface 693, the intermediate part 696 fastens the distal release part 692 and the proximal release part 694 with respect to one another in a form-locking connection. A form-locking connection is one that connects two elements together due to the shape of the elements themselves, as opposed to a force-locking connection, which locks the elements together by force external to the elements.

Specifically, as shown in FIG. 26, the clip 696 surrounds a distal plunger 699 of the proximal release part 694 that is inserted slidably within a hollow 698 of the distal release part 692. The plunger 699 of the proximal release part 694 can slide within the hollow 698, but a stop 697 inside the hollow 698 prevents the distal plunger 699 from withdrawing from the hollow 698 more than the longitudinal span of the clip 696.

To allow relative movement between the distal apex head 636 and the proximal apex body 638, the intermediate part 696 is removed easily with one hand and, as shown from the position in FIG. 16 to the position in FIG. 17, the distal release part 692 and the proximal release part 694 are moved axially towards one another (preferably, the former is moved towards the latter). Such movement separates the distal apex head 636 and the proximal apex body 638 as shown in FIG. 14. Accordingly, the distal apices 32 of the bare stent 30 are free to expand to their natural position in which the bare stent 30 is released against the vessel 700.

Of course, the apex release assembly 690 can be formed with any kind of connector that moves the apex release lumen 640 and the guidewire lumen 620 relative to one another. In a preferred alternative embodiment, for example, the intermediate part 696 can be a selectable lever that is fixedly connected to either one of the distal release part 692 or the proximal release part 694 and has a length equal to the width of the clip 696 shown in FIG. 26. Thus, when engaged by pivoting the lever between the distal release part 692 and the proximal release part 694, for example, the parts 692, 694 cannot move with respect to one another and, when disengaged by pivoting the lever out from between the parts 692, 694, the distal release part 692 and the proximal release part 694 are free to move towards one another.

The apex capture device 634 is unique to the present invention in that it incorporates features that allow the longitudinal forces subjected on the stent graft 1 to be fully supported, through the bare stent 30, by both the guidewire lumen 620 and apex release lumen 640. Support occurs by providing the distal apex head 636 with a distal surface 639 - which surface 639 supports the proximal apices 32 of the bare stent 30 (shown in the enlarged perspective view of the distal apex head 636 in FIG. 29). When captured, each proximal apex 32 of the bare stent 30 separately rests on a distal surface 639, as more clearly shown in FIGS. 30 and 31. The proximal spokes of the distal apex head 636 slide within the fingers of the proximal apex body 638 as these parts moves towards one another. A slight space, therefore, exists between the fingers and the outer circumferential surfaces

of the spokes. To insure that the bare stent 30 does not enter this space (which would prevent a proper release of the bare stent 30 from the apex capture device 634, a radial thickness of the space must be less than the diameter of the wire making up the bare stent 30. Preferably, the space is no greater than half a diameter of the wire.

- 5 Having the distal surface 639 be the load-bearing surface of the proximal apices 32 ensures expansion of each and every one of the distal apices 32 from the apex release assembly 690. The proximal surface 641 of the distal apex head 636 (see FIG. 30) meets with the interior surfaces of the proximal apex body 638 to help carry the apex load because the apices of the bare stent 30 are captured therebetween when the apex capture device 634 is closed.
- 10 Complete capture of the bare stent 30, therefore, fully transmits any longitudinal forces acting on the bare stent 30 to both the guidewire lumen 620 and apex release lumen 640, making the assembly much stronger. Such capture can be clearly seen in the cut-away view of the proximal apex body 638 in FIG. 31. For release of the apices 32 of the bare stent 30, the proximal apex body 638 moves leftward with respect to FIGS. 30 to 33 (compare FIGS.
- 15 30 and 31 with FIG. 32). Because friction exists between the apices 32 and the "teeth" of the proximal apex body 638 when the apices 32 are captured, the apices 32 will also try to move to the left along with the proximal apex body 638 and, if allowed to do so, possibly would never clear the "teeth" to allow each apex 32 to expand. However, as the proximal apex body 638 disengages (moves in the direction of arrow C in FIG. 31), direct contact
- 20 with the distal surface 639 entirely prevents the apices 32 from sliding in the direction of arrow C along with the proximal apex body 638 to ensure automatic release of every captured apex 32 of the bare stent 30. Because the proximal apex body 638 continues to move in the direction of arrow C, eventually the "teeth" will clear their respective capture of the apices 32 and the bare stent 30 will expand entirely. The release position of the distal apex head 636 and the proximal apex body 638 is shown in FIGS. 14 and 32, and
- 25 corresponds to the position of the apex release assembly 690 in FIG. 17. As can be seen, tapers on the distal outer surfaces of the proximal apex body 638 further assist in the prevention of catching the proximal apices 32 of the bare stent 30 on any part of the apex capture device 634. In this configuration, the distal surfaces 639 bear all the load upon the bare stent 30 and the fingers of the proximal apex body 638.

Simply put, the apex capture device 634 provides support for load placed on the stent graft 1 during advancement A of the inner sheath 652 and during withdrawal of the inner sheath 652 (i.e., during deployment D). Such a configuration benefits the apposition of the bare

stent 30 by releasing the bare stent 30 after the entire graft sleeve 10 has been deployed, thus reducing the potential for vessel perforation at the point of initial deployment.

When the stent graft 1 is entirely free from the inner sheath 652 as shown in FIG. 24, the proximal handle 678 is, then, substantially at or near the third position (deployment

5 position) shown in FIG. 10.

The stent graft 1 is, now, securely placed within the vessel 700 and the entire portion 630, 650, 660 of the assembly 600 may be removed from the patient.

While the preferred embodiments of the invention have been illustrated and described, it will be clear that the invention is not so limited. Numerous modifications, changes,

10 variations, substitutions, and equivalents will occur to those skilled in the art without departing from the spirit and scope of the present invention as defined by the appended claims.

CLAIMS

1. A vascular repair device, comprising:
- a tubular graft body;
- 5 a structural framework having at least two stents connected to said graft body; and
- a curved longitudinal support member connected to said graft body and having a centerline, said support member being substantially symmetrical with respect to said centerline.
- 10 2. The vascular repair device according to claim 1, wherein said longitudinal support member is of a material selected from the group consisting of nitinol, stainless steel, biopolymers, Cobalt Chrome, and titanium alloys.
- 15 3. The vascular repair device according to claim 1, wherein said longitudinal support member has a flattened S-shape.
4. The vascular repair device according to claim 1, wherein said longitudinal support member has a partial helix shape.
- 20 5. The vascular repair device according to claim 1, wherein said longitudinal support member is curved with substantially asymptotic ends.
6. The vascular repair device according to claim 1, wherein said longitudinal support member is connected to said graft body independent of said structural framework.
- 25 7. The vascular repair device according to claim 1, wherein said longitudinal support member is connected to one of said stents of said structural framework.
- 30 8. The vascular repair device according to claim 7, wherein said longitudinal support member has an end connected to said one stent.

9. The vascular repair device according to claim 7, wherein said longitudinal support member has two ends each connected to respective ones of said stents of said structural framework.
- 5 10. The vascular repair device according to claim 1, wherein said longitudinal support member is pre-formed in said curved shape.
11. The vascular repair device according to claim 1, wherein said longitudinal support member has rounded ends.
- 10 12. The vascular repair device according to claim 1, wherein said longitudinal support member has a looped end with a curved longitudinal extremity.
13. The vascular repair device according to claim 1, wherein said longitudinal support member has two looped ends each with curved longitudinal extremities.
- 15 14. The vascular repair device according to claim 1, wherein said longitudinal support member is shorter than said structural framework.
- 20 15. A vascular repair device, comprising:
- a tubular graft body;
- a structural framework having at least two stents connected to said tubular graft body; and
- 25 a curved longitudinal support member connected to said graft body independent of said structural framework.
16. A vascular repair device, comprising:
- 30 a tubular graft body;
- a structural framework having at least two stents connected to said tubular graft body; and

a longitudinal support member having two ends, at least one of said ends having a curved longitudinal extremity.

- 5 17. The vascular repair device according to claim 16, wherein said support member is curved.

18. A vascular repair device, comprising:

- 10 a tubular graft body having a proximal end and a distal end;

a structural framework having at least two stents each respectively connected to said tubular graft body adjacent said proximal end and said distal end and defining a separation distance therebetween; and

- 15 a longitudinal support member shorter than said separation distance and being connected to said graft body between said at least two stents to form a gimbal at at least one of said proximal and distal ends of said graft body.

- 20 19. The vascular repair device according to claim 18, wherein said support member is curved.

20. A vascular repair device, comprising:

- 25 a tubular graft body having a proximal end and a distal end;

a structural framework having at least two pairs of stents each respectively connected to said graft body adjacent said proximal end and said distal end, said stents of each of said pairs of stents being separated from one another at said graft body to define a respective
30 outer stent and a respective inner stent; and

a longitudinal support member connected to said graft body and extending between:

at least said inner stent of a first of said two pairs of stents; and

at least said outer stent of a second of said two pairs of stents.

5 21. The vascular repair device according to claim 20, wherein said support member is connected to said graft body between both of said inner stents of said two pairs of stents.

22. The vascular repair device according to claim 20, wherein said support member has ends each connected to said inner stent of each of said two pairs of stents.

10

23. The vascular repair device according to claim 20, wherein:

said support member has ends; and

15 at least one of said ends is connected to said inner stent of one of said two pairs of stents.

24. The vascular repair device according to claim 20, wherein said support member is curved.

20 25. A vascular repair device, comprising:

a tubular graft body having a proximal end and a distal end;

25 a structural framework having at least two pairs of stents each respectively connected to said graft body adjacent said proximal end and said distal end, said stents of each of said pairs of stents being separated from one another at said graft body to define a respective outer stent and a respective inner stent; and

30 a curved longitudinal support member having two ends and being connected to said graft body between both of said inner stents of said two pairs of stents.

26. The vascular repair device according to claim 25, wherein said support member is connected to said graft body without touching said inner stents.

27. The vascular repair device according to claim 25, wherein said support member is connected to said graft body to touch at least one of said inner stents.

5 28. A vascular repair device, comprising:

a tubular graft body having first and second ends;

10 a structural framework having at least three stents, two of said stents being connected to said tubular graft body adjacent said first end, said two stents being separated from one another on said graft body to define an outer stent and an inner stent, a third of said stents being connected to said tubular graft body adjacent said second end; and

15 a longitudinal support member having two ends and being connected to said graft body between said inner stent and said third stent without touching said inner stent and said third stent.

29. The vascular repair device according to claim 28, wherein said support member is curved.

20

30. A vascular repair device, comprising:

a tubular graft body;

25 a structural framework having at least two stents;

a first of said stents being connected to said tubular graft body along an entirety of said first stent;

30 a second of said stents having a periodically changing shape to define proximal apices having given radii of curvature and distal apices having radii of curvature smaller than said given radii of curvature; and

said second stent being connected to said tubular body at said distal apices.

31. The vascular repair device according to claim 30, wherein said second stent is connected to said tubular body only at said distal apices.

5

32. The vascular repair device according to claim 30, wherein said first stent has alternating proximal and distal apices with substantially equal radii of curvature.

33. The vascular repair device according to claim 32, wherein said radii of curvature is
10 between approximately 0.1 mm and approximately 3.0 mm.

34. The vascular repair device according to claim 32, wherein said radii of curvature is approximately 0.5 mm.

15 35. The vascular repair device according to claim 30, wherein:

said graft body has a proximal end;

said second stent is connected at said proximal end; and

20

said proximal apices extend away from said proximal end.

36. The vascular repair device according to claim 35, wherein:

25 said first stent has alternating proximal and distal apices with substantially equal radii of curvature; and

said distal apices of said second stent have radii of curvature substantially equal to said radii of curvature of said proximal and distal apices of said first stent.

30

37. The vascular repair device according to claim 36, wherein said proximal apices of said second stent have radii of curvature approximately equal to 1.5 mm and said distal apices of said second stent have radii of curvature approximately equal to 0.5 mm.

38. The vascular repair device according to claim 30, wherein:

said first stent has a given amplitude; and

5

said second stent has an amplitude greater than said given amplitude.

39. A vascular repair device, comprising:

10 a tubular graft body;

a structural framework having at least two stents;

a first of said stents:

15

having a periodically changing shape to define first proximal apices having first radii of curvature and first distal apices having radii of curvature substantially equal to said first radii of curvature; and

20 being connected to said tubular graft body along an entirety of said first stent; and

a second of said stents:

25

having a periodically changing shape to define second proximal apices having second radii of curvature larger than said first radii of curvature and second distal apices having radii of curvature substantially equal to said first radii of curvature; and

being connected to said tubular body only at said second distal apices.

30

40. The vascular repair device according to claim 1, wherein said support member is substantially reverse-mirror symmetrical with respect to said centerline.

41. The vascular repair device according to claim 1, wherein said graft body has a diameter at least as large as a diameter of a vessel into which said graft body is to be placed.

42. The vascular repair device according to claim 1, wherein:

5

said at least two stents each have apices;

said structural framework has a distal-most stent; and

10 said distal-most stent has at least one more apex than another of said at least two stents.

43. The vascular repair device according to claim 16, wherein said graft body has a diameter at least as large as a diameter of a vessel into which said graft body is to be placed.

15 44. The vascular repair device according to claim 16, wherein:

said at least two stents each have apices;

said structural framework has a distal-most stent; and

20

said distal-most stent has at least one more apex than another of said at least two stents.

45. The vascular repair device according to claim 39, wherein said first stent has at least one more apex than said second stent.

25

46. The vascular repair device according to claim 1, wherein:

said graft body has a longitudinal extent defining a longitudinal direction; and

said stents have a substantially linear profile in said longitudinal direction.

30 47. The vascular repair device according to claim 46, wherein said stents have a linear longitudinal profile.

48. The vascular repair device according to claim 46, wherein said stents have a circular cross-sectional shape.

49. The vascular repair device according to claim 46, wherein said stents have a non-
5 circular cross-sectional shape.

50. The vascular repair device according to claim 49, wherein said non-circular cross-sectional shape is selected from the group consisting of a ten-sided shape through a twenty-sided shape.

10

51. A vascular repair device, comprising:

a tubular graft body (10);

15 a structural framework connected to said graft body (10); and

a pair of radiopaque markers (232, 234) connected to said graft body, said markers (232,234) each having a contact diameter and being symmetrical about said contact diameter on opposing sides of said contact diameter.

20

52. The vascular repair device according to claim 51, wherein said markers (232, 234) are connected at opposing sides of said graft body (10).

53. The vascular repair device according to claim 51, wherein said tubular graft body (10)
25 has a proximate end and said markers (232, 234) are disposed at said proximate end (12) on opposite sides thereof (10).

54. The vascular repair device according to claim 51, wherein said markers (232, 234) are each hemispherical.

30

55. The vascular repair device according to claim 54, wherein:

said markers (232, 234) are on opposite sides of said graft body (10) along respective longitudinal axes of said graft body (10); and

an opposition of said hemispherical markers (232, 234) forms a complete circular shape
5 when said markers (232, 234) are viewed from an orientation aligning said axes with one another.

56. The vascular repair device according to claim 51, wherein said markers (232, 234) are each D-shaped.

10

57. The vascular repair device according to claim 56, wherein:

said markers (232, 234) are on opposite sides of said graft body (10) along respective longitudinal axes of said graft body (10); and

15

an opposition of said D-shaped markers (232, 234) forms a complete ovular shape with said markers (232, 234) when said markers (232, 234) are viewed from an orientation aligning said axes with one another.

20 58. The vascular repair device according to claim 51, wherein said structural framework has at least two stents each connected to said graft body (10).

59. A vascular repair device, comprising:

25 a tubular graft body (10);

a structural framework connected to said graft body (10); and

a pair of radiopaque markers (232, 234) each having a first shape and being connected to
30 opposing sides of said graft body, each of said first shapes including an alignment segment, and, in a plan view of one of said markers, said alignment segments aligning with one another to, together, define a second shape different from said first shape.

60. The vascular repair device according to claim 59, wherein said second shape is symmetrical about said alignment segment.

61. The vascular repair device according to claim 59, wherein said tubular graft body (10) has a proximate end and said markers (232, 234) are disposed at said proximate end (12) on opposite sides thereof (10).

62. The vascular repair device according to claim 59, wherein said markers (232, 234) are each hemispherical.

10

63. The vascular repair device according to claim 62, wherein:

said markers (232, 234) are on opposite sides of said graft body (10) along respective longitudinal axes of said graft body (10); and

15

an opposition of said hemispherical markers (232, 234) forms a complete circular shape when said markers (232, 234) are viewed from an orientation aligning said axes with one another.

64. The vascular repair device according to claim 59, wherein said markers (232, 234) are each D-shaped.

65. The vascular repair device according to claim 64, wherein:

25 said markers (232, 234) are on opposite sides of said graft body (10) along respective longitudinal axes of said graft body (10); and

an opposition of said D-shaped markers (232, 234) forms a complete ovular shape with said markers (232, 234) when said markers (232, 234) are viewed from an orientation aligning said axes with one another.

30

66. The vascular repair device according to claim 59, wherein said structural framework has at least two stents each connected to said graft body (10).

67. A vascular repair device, comprising:

a tubular graft body (10);

5

a structural framework connected to said graft body (10); and

a pair of symmetrically shaped and diametrically opposed radiopaque markers (232, 234) connected to said graft body (10).

10

68. A method for implanting a vascular repair device, which comprises:

providing a pair of radiopaque markers (232, 234) on opposing sides of a longitudinal axis of a vascular repair device (1) such that, when viewed from a side of the vascular repair device (1), the markers (232, 234) together form a given shape;

15

implanting the vascular repair device (1) in a blood vessel while viewing the side of the vascular repair device (1); and

aligning the vascular repair device (1) in a given orientation by rotating the vascular repair device (1) along the longitudinal axis until the viewed markers (232, 234) substantially form the given shape.

20

69. The method according to claim 68, which further comprises forming the markers (232,234) each with a shape having a contact segment, the shape being symmetrical, when the two contact segments are aligned with one another, about the aligned contact segments.

25

70. The method according to claim 68, which further comprises:

shaping each of the markers (232,234) with an alignment segment; and

30

aligning the alignment segments with one another to form the given shape when viewed in a plan view of one of the markers (232,234).

71. The method according to claim 68, which further comprises communicating a direction in which the vascular repair device (1) needs to rotate minimally to align the markers (232, 234) in the given shape by selecting a form of the given shape.

5

72. The method according to claim 71, which further comprises:

providing each of the markers with a shape selected from the group consisting of a hemispherical shape and a D-shape; and

10

indicating the direction for minimal rotation with two flat diameters of the shape and two highest points of opposing curves of the shape.

73. The method according to claim 68, which further comprises selecting the given shape to communicate a direction in which the vascular repair device (1) needs to rotate minimally to align the markers (232, 234) in the given shape.

15

74. The method according to claim 73, which further comprises:

20 providing each of the markers with a shape selected from the group consisting of a hemispherical shape and a D-shape; and

indicating the direction for minimal rotation with two flat diameters of the shape and two highest points of opposing curves of the shape.

25

75. The method according to claim 68, wherein the given shape is one of a circle, a diamond, and an oval.

76. The method according to claim 68, which further comprises providing each of the markers (232, 234) as one of the group consisting of hemispherical markers (232,234), D-shaped markers (232,234), triangular markers (232,234), and isosceles triangular-shaped markers (232,234).

30

77. The method according to claim 68, which further comprises providing the pair of markers (232,234) as symmetrically shaped and diametrically opposed radiopaque markers (232, 234).

5 78. The method according to claim 68, which further comprises carrying out the implanting and viewing step by viewing the markers (232, 234) with a fluoroscope and a high-resolution image intensifier mounted on a freely, angled C-arm.

79. The method according to claim 78, which further comprises rotating the C-arm to
10 project a patient image into a left anterior oblique projection and open a radial curve of a thoracic aortic arch for visualization without superimposition of structures to determine a target area for placement of the vascular repair device (1).

80. The method according to claim 79, which further comprises:

15 placing the C-arm over the patient with a central ray of a fluoroscopic beam substantially perpendicular to the target area;

performing an angiogram and marking the proposed landing zones of the vascular repair
20 device (1) on a visual monitor;

keeping the patient, a patient table, and the C-arm stable during implantation of the vascular repair device (1); and

25 placing the vascular repair device (1) in the patient aligned with the marked landing zones.

81. The method according to claim 68, wherein the given orientatation aligns a segment of the vascular repair device (1) within approximately seventy degrees of a superior surface position in a curved aorta.

30

82. The method according to claim 68, wherein the given orientatation aligns a segment of the vascular repair device (1) within approximately seventy degrees of an upper-most superior longitudinal line of a curved aorta.

83. The method according to claim 68, which further comprises diagnosing a vascular migration of the vascular repair device (1) by viewing the markers (232, 234) after the vascular repair device (1) has been placed inside a patient's body.

5

84. The method according to claim 83, which further comprises carrying out the diagnosing step by:

recording a position of the markers (232, 234) from a given angle when the vascular repair
10 device (1) is implanted in the patient;

viewing the markers (232, 234) after a given amount of time has lapsed after the original implantation; and

15 comparing a relative position of the later-viewed markers (232, 234) with the recorded position of the originally implanted markers (232, 234).

85. The method according to claim 68, which further comprises:

20 providing a repair device delivery assembly (600) with a proximal handle assembly (670) and a distal implantation assembly (630, 650), the delivery assembly (600) having a central axis;

carrying out the vascular repair device (1) implanting step utilizing the delivery assembly
25 (670); and

carrying out the aligning step by rotating at least a portion of the delivery assembly (670) about the central axis.

30 86. The method according to claim 85, which further comprises minimizing rotation in the aligning step by pre-aligning the vascular repair device (1) in a given orientation in the implantation assembly (630, 650) before the delivery assembly (600) is used in the patient.

87. A delivery system for endovascularly delivering a prosthesis along a guidewire to an implantation site having a curved shape, the delivery system comprising:

a proximal control handle having:

5

a handle body; and

a prosthesis movement control assembly movably disposed at said handle body;

10 a hollow catheter having a proximal end connected to said control handle and a distal end, said catheter defining an interior cavity therein; and

a hollow prosthesis delivery assembly movably disposed in said interior cavity, said prosthesis delivery assembly having at least one hollow guidewire lumen for slidably
15 receiving therein the guidewire, said guidewire lumen having a curved distal end for orienting said prosthesis delivery assembly when passing through a curved portion of a vessel.

88. The system according to claim 87, wherein said curved distal end of said guidewire
20 lumen has a curved shaped substantially corresponding to the curved shape of the implantation site.

89. The system according to claim 87, wherein said catheter is rotatably mounted on said
25 control handle.

90. The system according to claim 87, wherein:

the implantation site having the curved shape is a curved portion of an aorta; and

30 said curved distal end has a curved shape substantially corresponding to a curve of the aorta of the patient in which the prosthesis is to be implanted.

91. The system according to claim 87, wherein said guidewire lumen is of metal.

92. The system according to claim 91, wherein said metal is stainless steel.

93. The system according to claim 89, wherein said catheter is rotatably connected to said
5 control handle and said control assembly is connected to said delivery assembly to permit
rotation of said handle body and, thereby, said delivery assembly in the implantation site
while said catheter remains substantially rotationally stable.

94. The system according to claim 87, wherein said guidewire lumen is rotatably mounted
10 to said prosthesis delivery assembly.

96. The system according to claim 87, wherein said prosthesis delivery assembly has a
rotating coupling rotatably mounting said guidewire lumen to said prosthesis delivery
assembly.

15

97. A delivery system for endovascularly delivering a prosthesis along a guidewire to an
implantation site having a curved shape, the delivery system comprising:

a proximal control handle having:

20

a handle body; and

a prosthesis movement control assembly movably disposed at said handle body;

25 a hollow catheter having a proximal end connected to said control handle and a distal end,
said catheter defining an interior cavity therein;

a hollow prosthesis delivery assembly movably disposed in said interior cavity;

30 said delivery assembly having at least one hollow guidewire lumen for slidably receiving
therein the guidewire;

said guidewire lumen having a pre-curved distal end with a curved shape for orienting said prosthesis delivery assembly when passing through a curved portion of a vessel; and

said pre-curved distal end having:

5

when disposed entirely in said catheter, a shape substantially corresponding to a shape of a surrounding portion of said catheter;

10

when disposed partly in said catheter and partly out of said catheter, a shape substantially corresponding to:

a first shape of a surrounding portion of said catheter for a first portion of said pre-curved distal end disposed in said catheter; and

15

a second curved shape for a second portion of said pre-curved distal end disposed outside said catheter; and

when said pre-curved distal end is disposed entirely out of said catheter, one of:

20

said curved shape; and

a shape substantially corresponding to the curved shape of the implantation site.

25 98. The delivery system according to claim 97, wherein a curve of said pre-curved distal end substantially corresponds to the curved shape of the implantation site.

99. The delivery system according to claim 97, wherein:

30 said catheter is substantially linear; and

when disposed entirely in said catheter, said pre-curved distal end has a substantially linear shape substantially corresponding to said surrounding portion of said catheter.

100. The system according to claim 97, wherein said catheter is rotatably mounted on said control handle.

5 101. The system according to claim 97, wherein:

the implantation site having the curved shape is a curved portion of an aorta; and

10 said curved distal end has a curved shape substantially corresponding to a curve of the aorta of the patient in which the prosthesis is to be implanted.

102. The system according to claim 97, wherein said guidewire lumen is of metal.

15 103. The system according to claim 102, wherein said metal is stainless steel.

104. The system according to claim 100, wherein said catheter is rotatably connected to said control handle and said control assembly is connected to said delivery assembly to permit rotation of said handle body and, thereby, said delivery assembly in the implantation site while said catheter remains substantially rotationally stable.

20 105. The system according to claim 97, wherein said prosthesis delivery assembly has a rotating coupling rotatably mounting said guidewire lumen to said prosthesis delivery assembly.

25 106. In combination with a delivery system for endovascularly delivering a prosthesis loaded in a prosthesis delivery assembly along a guidewire to an implantation site having a curved shape, a self-aligning prosthesis control assembly comprising:

30 a hollow guidewire lumen for slidably receiving therein the guidewire;

said guidewire lumen having a pre-curved distal end with a curved shape for orienting the prosthesis delivery assembly when passing through a curved portion of a vessel; and

said pre-curved distal end having:

5 when disposed entirely in the delivery system, a shape substantially corresponding to a shape of a surrounding portion of the delivery system;

when disposed partly in the delivery system and partly out of the delivery system, a shape substantially corresponding to:

10 a first shape of a surrounding portion of the delivery system for a first portion of said pre-curved distal end disposed in the delivery system; and

a second curved shape for a second portion of said pre-curved distal end outside the delivery system; and

15 when said pre-curved distal end is disposed entirely out of the delivery system, one of:

said curved shape; and

20 a shape substantially corresponding to the curved shape of the implantation site.

25 107. The delivery system according to claim 106, wherein a curve of said pre-curved distal end substantially corresponds to the curved shape of the implantation site.

30 108. The delivery system according to claim 106, wherein, when disposed entirely in the delivery system, said surrounding portion of the delivery system is linear and said pre-curved distal end has a substantially linear shape substantially corresponding to said linear surrounding portion.

109. The delivery system according to claim 106, wherein:

a portion of the delivery system surrounding said pre-curved distal end is substantially linear; and

5 said pre-curved distal end has a substantially linear shape substantially corresponding to said surrounding portion of the delivery system when disposed entirely in the delivery system.

110. The system according to claim 106, wherein:

10 the implantation site having the curved shape is a curved portion of an aorta; and

said pre-curved distal end has a curved shape substantially corresponding to the curved portion of the aorta of the patient in which the prosthesis is to be implanted.

15 111. The system according to claim 106, wherein said guidewire lumen is of metal.

112. The system according to claim 111, wherein said metal is stainless steel.

20 113. The system according to claim 106, further comprising a rotating coupling rotatably mounting said guidewire lumen to said prosthesis delivery assembly.

25 114. An endovascular prosthesis delivery kit for endovascularly delivering a prosthesis along a guidewire to an implantation site having a curved shape, the delivery kit comprising:

a proximal control handle having:

a handle body; and

30 a prosthesis movement control assembly movably disposed at said handle body;

a hollow catheter having a proximal end connected to said control handle and a distal end, said catheter defining an interior cavity therein;

a hollow prosthesis delivery assembly movably disposed in said interior cavity, said prosthesis delivery assembly having at least one hollow guidewire lumen for slidably receiving therein the guidewire, said guidewire lumen having a curved distal end for
5 orienting said prosthesis delivery assembly when passing through a curved portion of a vessel; and

a curving device forming a curved shape of said curved distal portion.

10 115. The kit according to claim 114, wherein said curving device is a set of curving devices having differently curved shapes and at least one of said curving devices forming said curved shape of said curved distal portion to at least approximately correspond said curved shape to the curved shape of the vessel in which the prosthesis is to be implanted.

15 116. The kit according to claim 114, wherein said curving device is a set of curving devices having differently curved shapes and at least one of said curving devices forming said curved shape of said curved distal portion to substantially correspond said curved shape to the curved shape of the vessel in which the prosthesis is to be implanted.

20 117. The system according to claim 114, wherein said catheter is rotatably mounted on said control handle.

118. The system according to claim 114, wherein:

25 the implantation site having the curved shape is a curved portion of an aorta; and

said curved distal end has a curved shape at least approximately corresponding to a curve of the aorta of the patient in which the prosthesis is to be implanted.

30 119. The system according to claim 117, wherein said catheter is rotatably connected to said control handle and said control assembly is connected to said delivery assembly to permit rotation of said handle body and, thereby, said delivery assembly in the implantation site while said catheter remains substantially rotationally stable.

120. The system according to claim 114, wherein said guidewire lumen is rotatably mounted to said prosthesis delivery assembly.
- 5 121. The system according to claim 114, wherein said prosthesis delivery assembly has a rotating coupling rotatably mounting said guidewire lumen to said prosthesis delivery assembly.
122. The kit according to claim 114, wherein said pre-curved distal end has:
- 10 when disposed entirely in said catheter, a shape substantially corresponding to a shape of a surrounding portion of said catheter;
- when disposed partly in said catheter and partly out of said catheter, a shape
- 15 substantially corresponding to:
- a first shape of a surrounding portion of said catheter for a first portion of said pre-curved distal end disposed in said catheter; and
- 20 a second curved shape for a second portion of said pre-curved distal end disposed outside said catheter; and
- when said pre-curved distal end is disposed entirely out of said catheter, one of:
- 25 said curved shape; and
- a shape substantially corresponding to the curved shape of the implantation site.
- 30 123. A self-aligning delivery system for endovascularly delivering at least one of a prosthesis and a prosthesis delivery assembly loaded with a prosthesis along a guidewire to a vessel implantation site having a curved shape, the delivery system comprising:

a hollow guidewire lumen for slidably receiving therein the guidewire, said guidewire lumen having a pre-curved distal end orienting at least one of the prosthesis and the prosthesis delivery assembly when said pre-curved distal end passes through a curved portion of a vessel.

5

124. A method for automatic endovascular alignment of a prosthesis, loaded in a delivery assembly, in a curved implantation site of a vessel having positioned therein a guidewire extending at least into the implantation site, which comprises:

10 providing a prosthesis delivery system with a longitudinally movable guidewire lumen having a curved distal portion;

threading the guidewire lumen over the guidewire along with the loaded distal delivery assembly to advance the guidewire lumen and the loaded distal delivery assembly towards
15 the implantation site; and

advancing the curved distal portion and the loaded distal delivery assembly into the curved implantation site to at least approximately align the curved distal portion to a curve of the curved implantation site and, thereby, orient the prosthesis.

20

125. A method for automatic endovascular alignment of a prosthesis in a curved implantation site of a vessel, which comprises:

providing a prosthesis delivery system with a longitudinally movable distal delivery
25 assembly and a longitudinally movable guidewire lumen having a curved distal portion;

loading the prosthesis in the distal delivery assembly;

positioning a guidewire at least into the curved implantation site of the vessel;

30

threading the guidewire lumen over the guidewire along with the loaded distal delivery assembly to advance the guidewire lumen and the loaded distal delivery assembly along the guidewire towards the curved implantation site; and

further advancing the guidewire lumen with the curved distal portion and the loaded distal delivery assembly along the guidewire and into the curved implantation site to at least approximately align the curved distal portion to a curve of the curved implantation site and,
5 thereby, orient the prosthesis.

126. The method according to claim 125, wherein the curved distal portion defines a distal portion plane and the curved implantation site of the vessel is a curved portion of an aorta, and which further comprises carrying out the loading step by substantially aligning a given
10 longitudinal line of the prosthesis in the distal portion plane.

127. The method according to claim 126, which further comprises:

positioning the guidewire into the curved portion of the aorta; and
15 carrying out the further advancing step by orienting the prosthesis to at least approximately align the given longitudinal line with a superior longitudinal surface line of the curved portion of the aorta.

20 128. The method according to claim 126, which further comprises:

positioning the guidewire into the curved portion of the aorta; and

carrying out the further advancing step by orienting the prosthesis to substantially align the
25 given longitudinal line with a superior longitudinal surface line of the curved portion of the aorta.

129. The method according to claim 126, which further comprises:

30 providing the prosthesis with a curved longitudinal support member disposed at least in part on the given longitudinal line; and

carrying out the further advancing step by orienting the prosthesis to at least approximately align the part of the support member with a superior longitudinal surface line of the curved portion of the aorta.

- 5 130. The method according to claim 129, which further comprises carrying out the loading step by aligning at least a part of the curved longitudinal support member in the distal portion plane.

- 10 131. The method according to claim 126, which further comprises:
providing the prosthesis with a curved longitudinal support member disposed at least in part on the given longitudinal line; and

- 15 carrying out the further advancing step by orienting the prosthesis to substantially align the part of the support member with a superior longitudinal surface line of the curved portion of the aorta.

- 20 132. The method according to claim 131, which further comprises carrying out the loading step by aligning at least a substantial part of the curved longitudinal support member in the distal portion plane.

- 25 133. The method according to claim 125, which further comprises carrying out the further advancing step by substantially aligning the curved distal portion with the curve of the curved implantation site.

- 30 134. The method according to claim 125, which further comprises carrying out the further advancing step by at least approximately aligning the curved distal portion with the curve of the curved implantation site by rotating the distal delivery assembly and the prosthesis loaded therein.

135. The method according to claim 125, which further comprises carrying out the further advancing step by orienting the prosthesis in an optimal superior surface position.

136. The method according to claim 125, which further comprises carrying out the further advancing step by automatically aligning the prosthesis in an optimal superior surface position while traversing a curve of the vessel in which the prosthesis is to be implanted.
- 5 137. The method according to claim 129, which further comprises automatically aligning the prosthesis to place at least a portion of the longitudinal support member at least approximately at the superior longitudinal surface line of the curved aorta while traversing the curved portion of the aorta.
- 10 138. The method according to claim 125, which further comprises pre-curving the prosthesis in a shape at least approximately corresponding to the curved shape of the curved implantation site.
139. The method according to claim 129, which further comprises pre-forming the
15 longitudinal support member in a curved shape and attaching the curved longitudinal support member to the prosthesis.
140. The method according to claim 129, which further comprises pre-forming the
20 longitudinal support member in a curved shape substantially corresponding to the curved portion of the aorta.
141. The method according to claim 129, which further comprises pre-forming the
25 longitudinal support member in a curved shape substantially corresponding to the curved portion of the aorta in which the prosthesis is to be implanted.
142. The method according to claim 125, which further comprises:
- viewing the curve of the vessel in which the prosthesis is to be implanted; and
- 30 subsequently forming the curved shape of the curved distal portion to correspond to the curve of the vessel viewed.

143. The method according to claim 142, which further comprises providing a curving device and forming the curved shape of the curved distal portion with the curving device to correspond to the curve of the vessel viewed.
- 5 144. The method according to claim 142, which further comprises providing a set of curving devices having differently curved shapes and forming the curved shape of the curved distal portion with at least one of the curving devices to at least approximately correspond to the curve of the vessel viewed.
- 10 145. The method according to claim 125, which further comprises connecting the guidewire lumen to the prosthesis delivery system to minimize a restoring force when the guidewire lumen is rotated along its longitudinal axis.
146. The method according to claim 125, which further comprises freely rotatably
15 connecting the guidewire lumen to the prosthesis delivery system to minimize a restoring force when the guidewire lumen is rotated along its longitudinal axis.
147. The method according to claim 125, which further comprises connecting the
20 guidewire lumen to the prosthesis delivery system at a proximal-most area of the guidewire lumen to minimize a restoring force when the guidewire lumen is rotated along its longitudinal axis.
148. The method according to claim 125, which further comprises rotationally fixedly
25 connecting the guidewire lumen to the distal delivery assembly as the guidewire lumen and the distal delivery assembly advance to the implantation site.
149. The method according to claim 125, which further comprises forming the guidewire
30 lumen from a material permitting ends thereof to be twisted with respect to one another into an at least one-hundred eighty degree axially rotated orientation without deforming the guidewire lumen.
150. The method according to claim 125, which further comprises forming the guidewire lumen from a material permitting ends thereof to be twisted with respect to one another into

an at least one-hundred eighty degree axially rotated orientation without producing a restoring force sufficient to harm a vessel wall.

151. The method according to claim 125, which further comprises forming the guidewire
5 lumen from a metal.

152. The method according to claim 125, which further comprises forming the guidewire lumen from stainless steel.

10 153. The method according to claim 125, wherein the curved distal portion defines a distal portion plane and which further comprises carrying out the further advancing step by further advancing the guidewire lumen with the curved distal portion and the loaded distal delivery assembly into the curved implantation site to at least approximately align the curved distal plane to a superior longitudinal surface line of the curved portion of the vessel.

15 154. The method according to claim 125, wherein the curved distal portion defines a distal portion plane and which further comprises carrying out the further advancing step by further advancing the guidewire lumen with the curved distal portion and the loaded distal delivery assembly into the curved implantation site to orient the curved distal portion such that the
20 curved distal plane intersects within seventy circumferential degrees of a plane passing through a superior longitudinal surface line of the curved portion of the vessel.

155. The method according to claim 125, which further comprises carrying out the further advancing step by further advancing the guidewire lumen with the curved distal portion and
25 the loaded distal delivery assembly into the curved implantation site to at least approximately orient the prosthesis in an optimal implantation position.

156. The method according to claim 129, wherein the curved distal portion defines a distal portion plane and which further comprises carrying out the loading step by substantially
30 aligning a plane passing through a proximal end of the curved longitudinal support member between thirty-five and fifty-five degrees around the circumference of the prosthesis to the distal portion plane.

157. The method according to claim 129, wherein the curved distal portion defines a distal portion plane and which further comprises carrying out the loading step by substantially aligning a plane passing through a proximal end of the curved longitudinal support member at approximately forty-five degrees around the circumference of the prosthesis to the distal
5 portion plane.

158. The method according to claim 129, wherein a superior longitudinal surface line of the curved portion of the vessel in which the prosthesis is to be implanted defines a superior plane and which further comprises carrying out the further advancing step by further
10 advancing the guidewire lumen with the curved distal portion and the loaded distal delivery assembly into the curved implantation site to at least approximately intersect the superior plane with a proximal half of the curved longitudinal support member.

159. A method for automatic endovascular alignment of a prosthesis in a curved
15 implantation site of a vessel, which comprises:

advancing a guidewire lumen having a curved distal portion along a guidewire and into the curved implantation site to at least approximately align the curved distal portion to a curve of the curved implantation site.
20

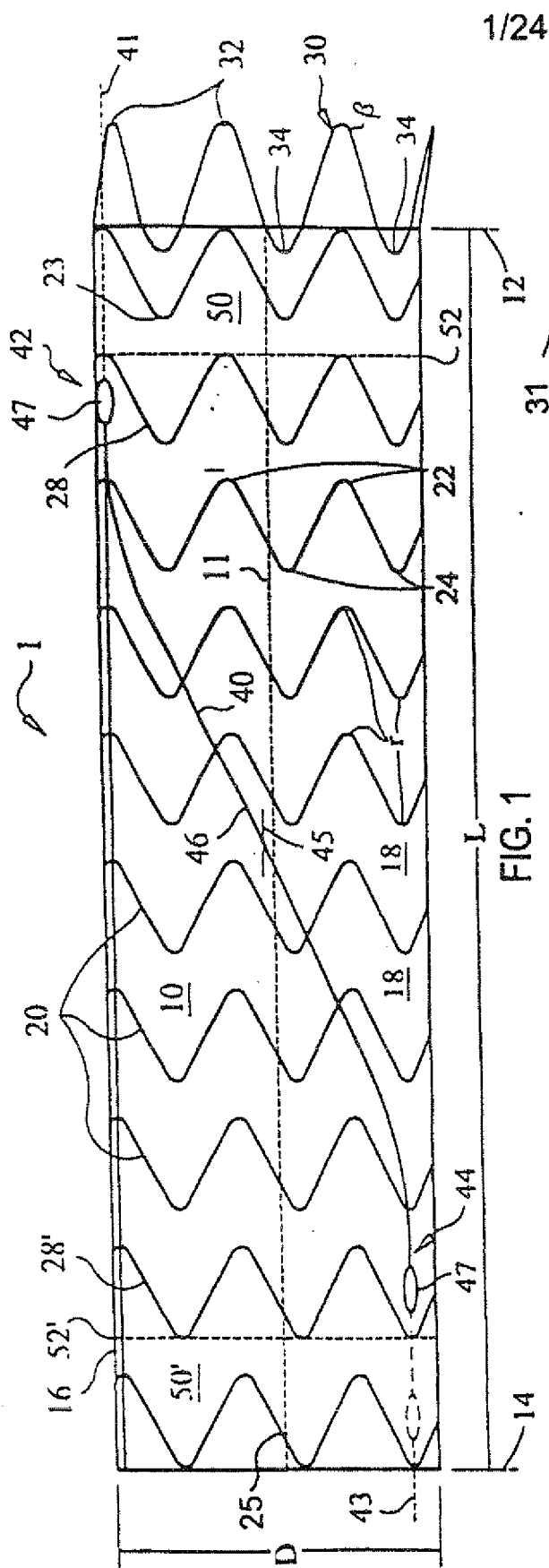


FIG. 1

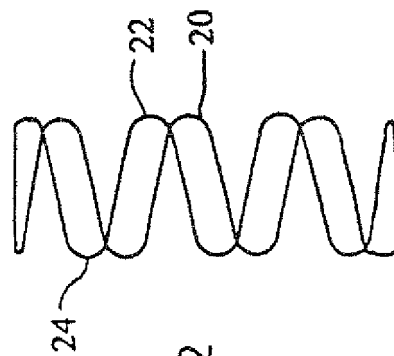


FIG. 2

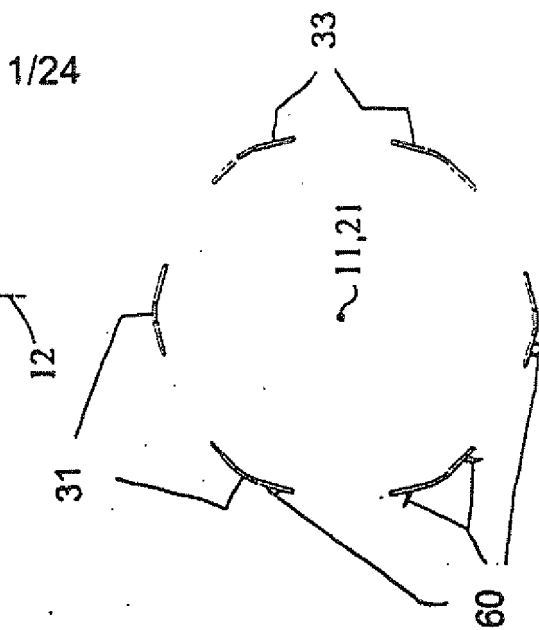
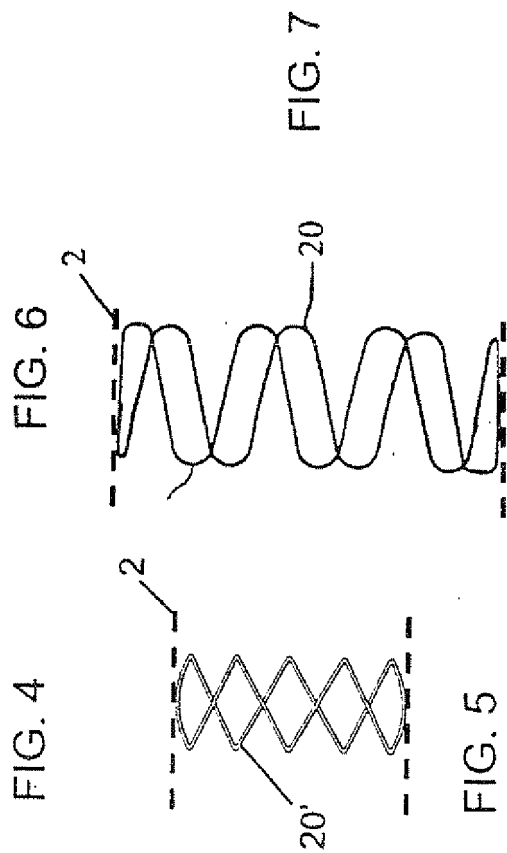
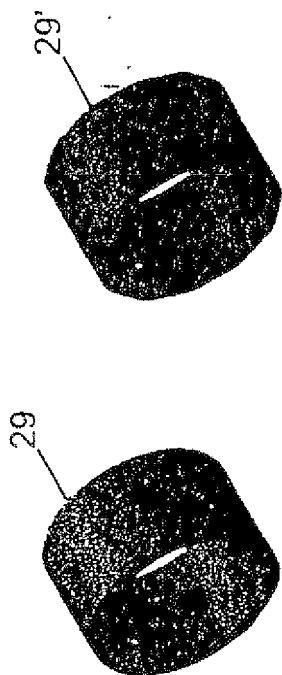
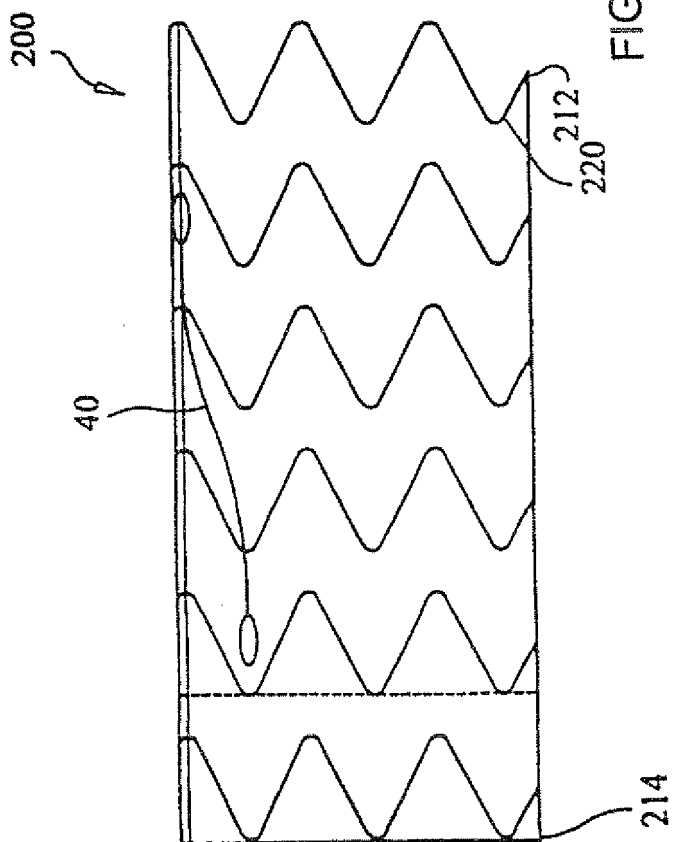
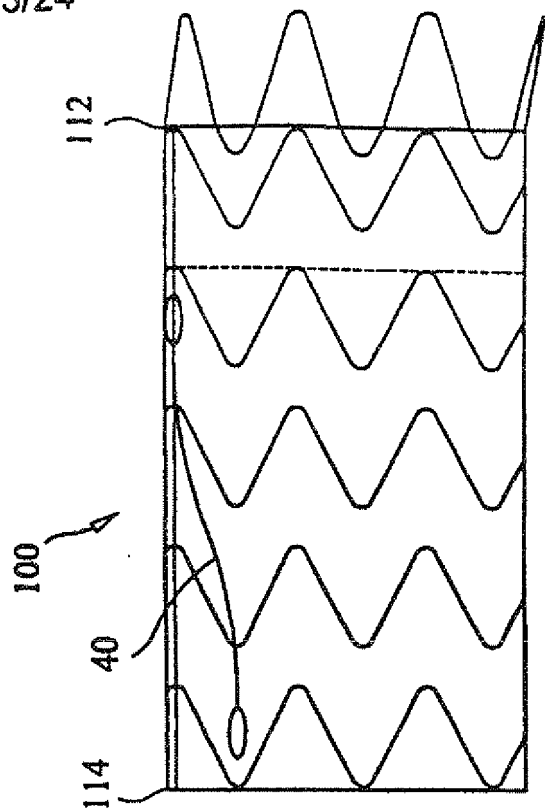
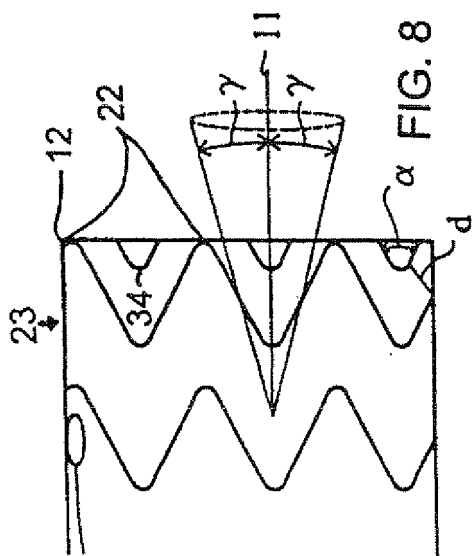


FIG. 3

2/24



3/24



4/24

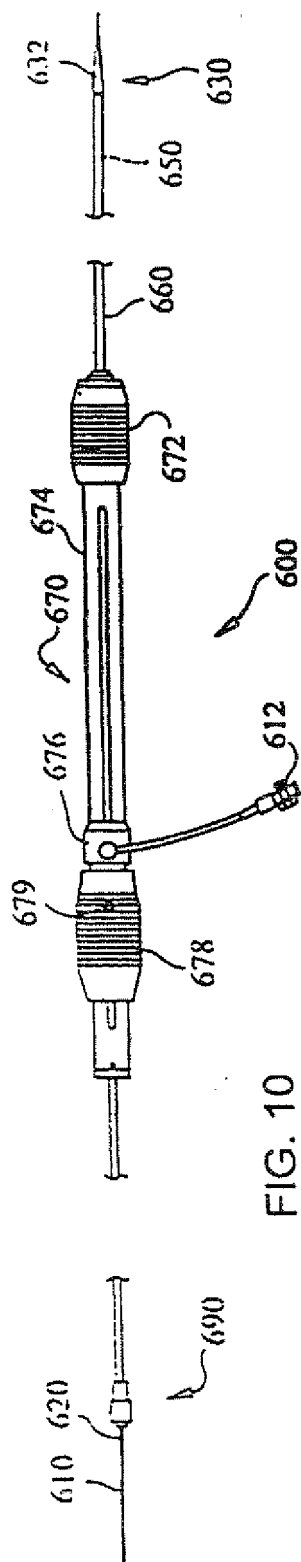


FIG. 10

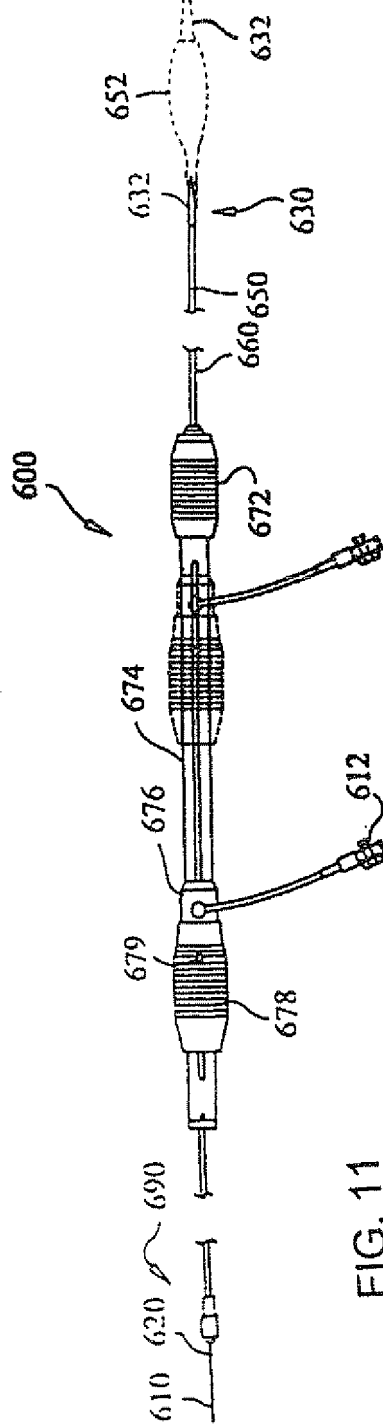


FIG. 11

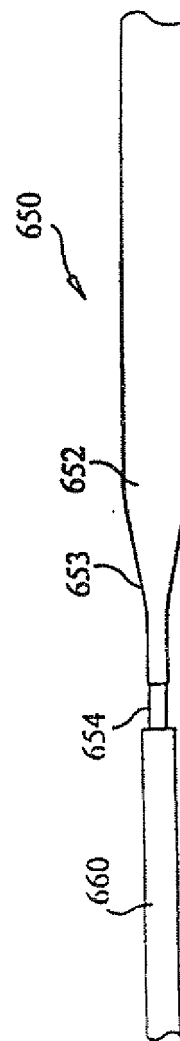


FIG. 12

5/24

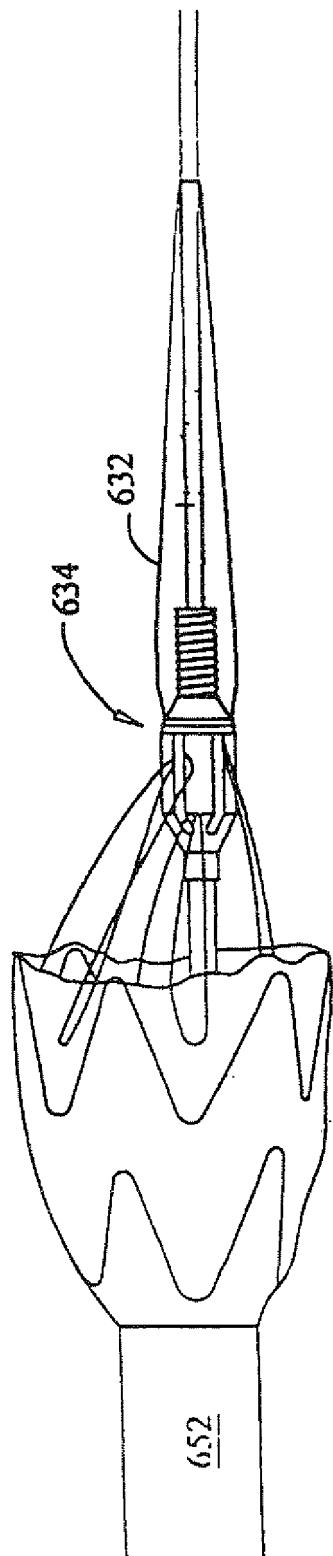


FIG. 13

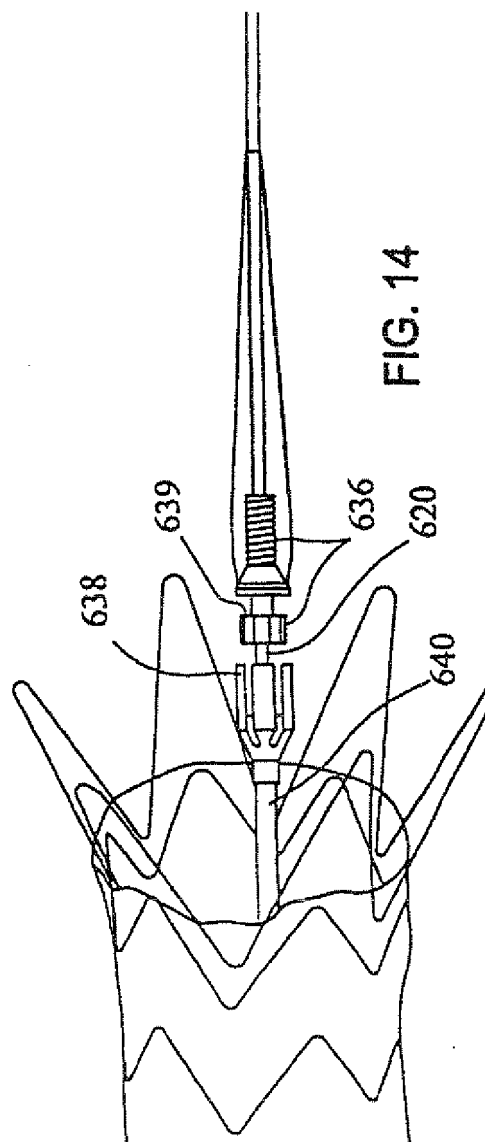


FIG. 14

6/24

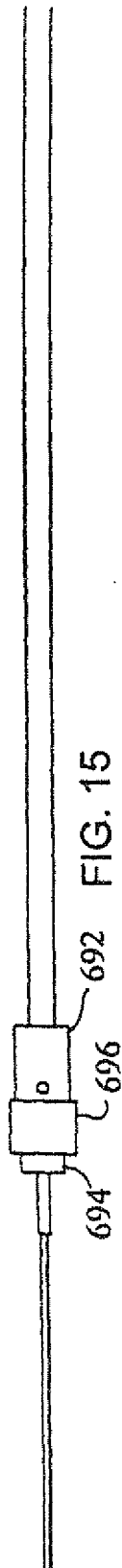


FIG. 15

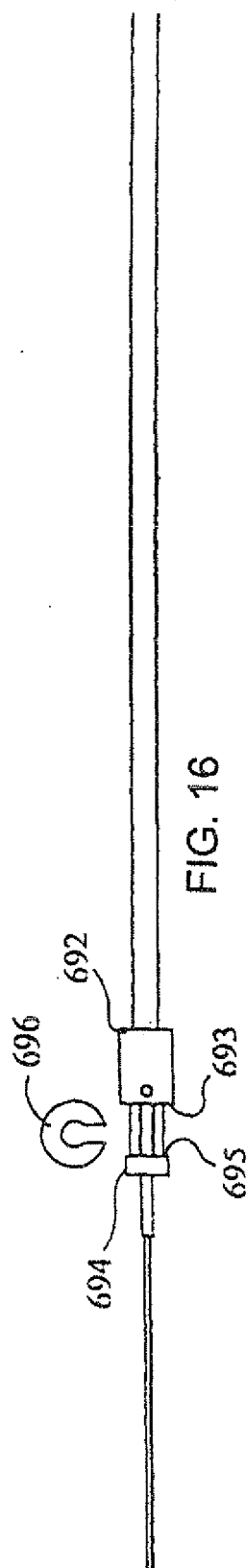


FIG. 16



FIG. 17

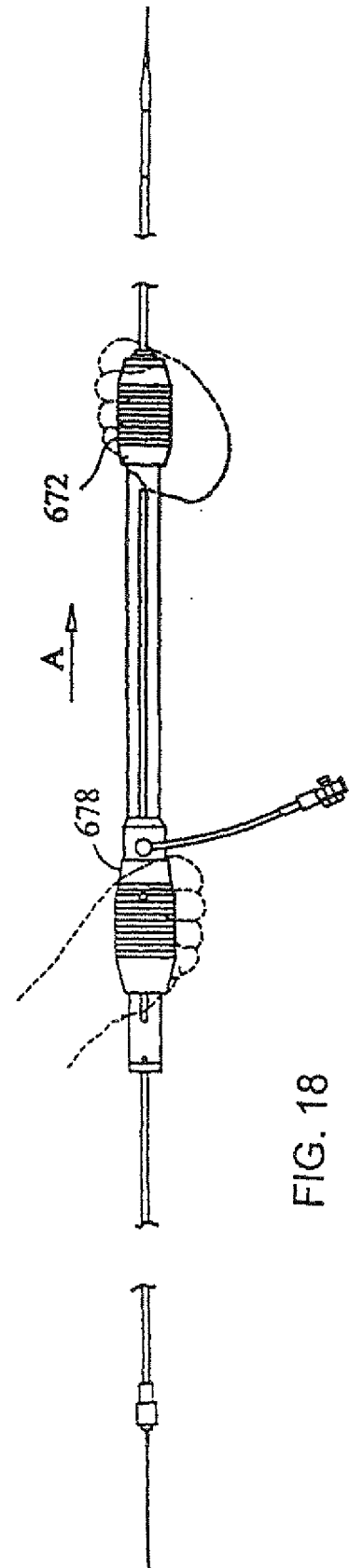


FIG. 18

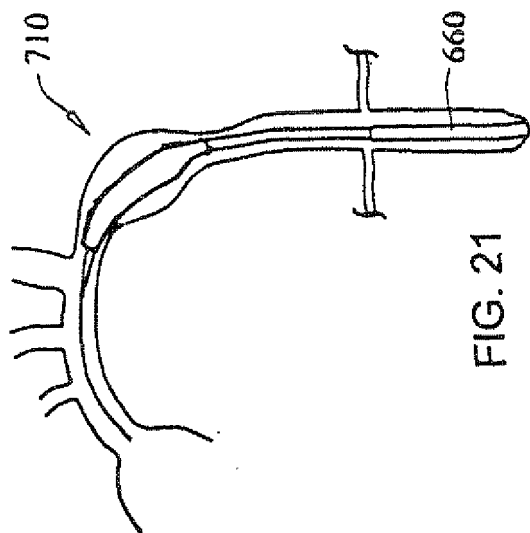


FIG. 21

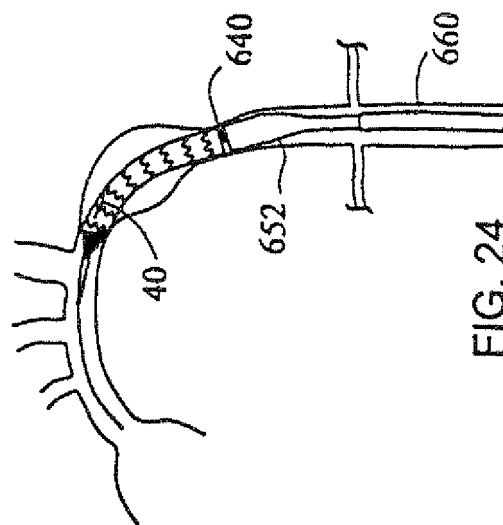


FIG. 24

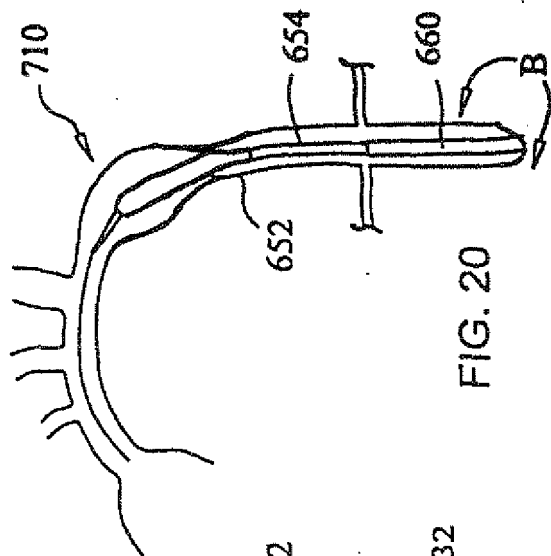


FIG. 20

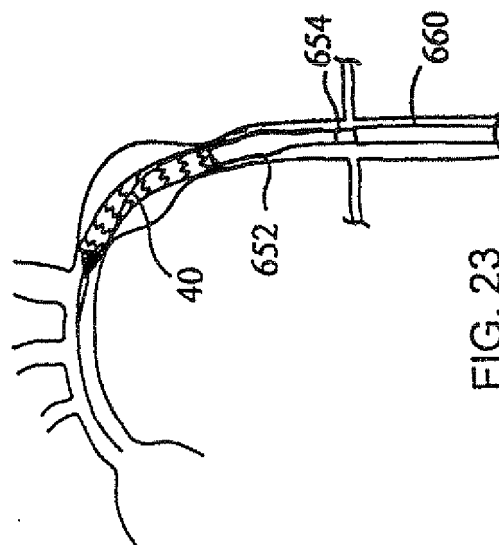


FIG. 23

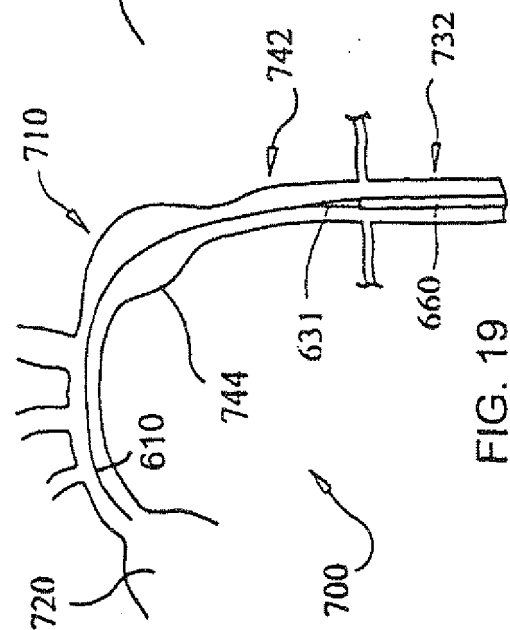


FIG. 19

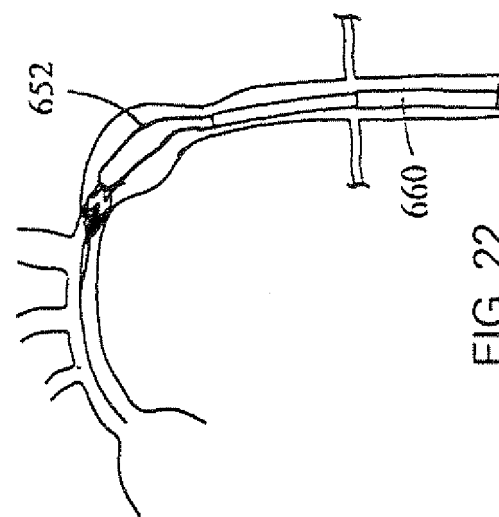


FIG. 22

8/24

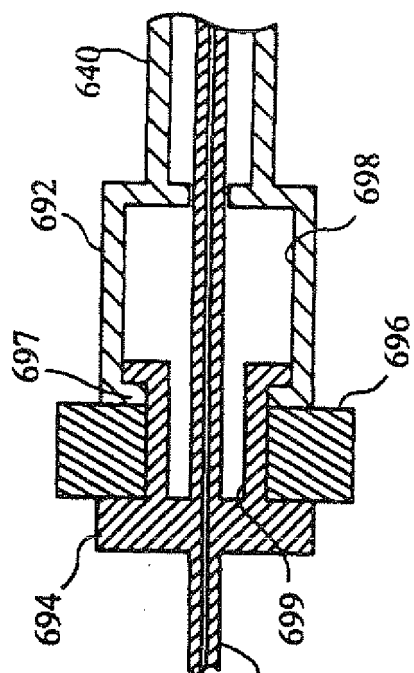


FIG. 26

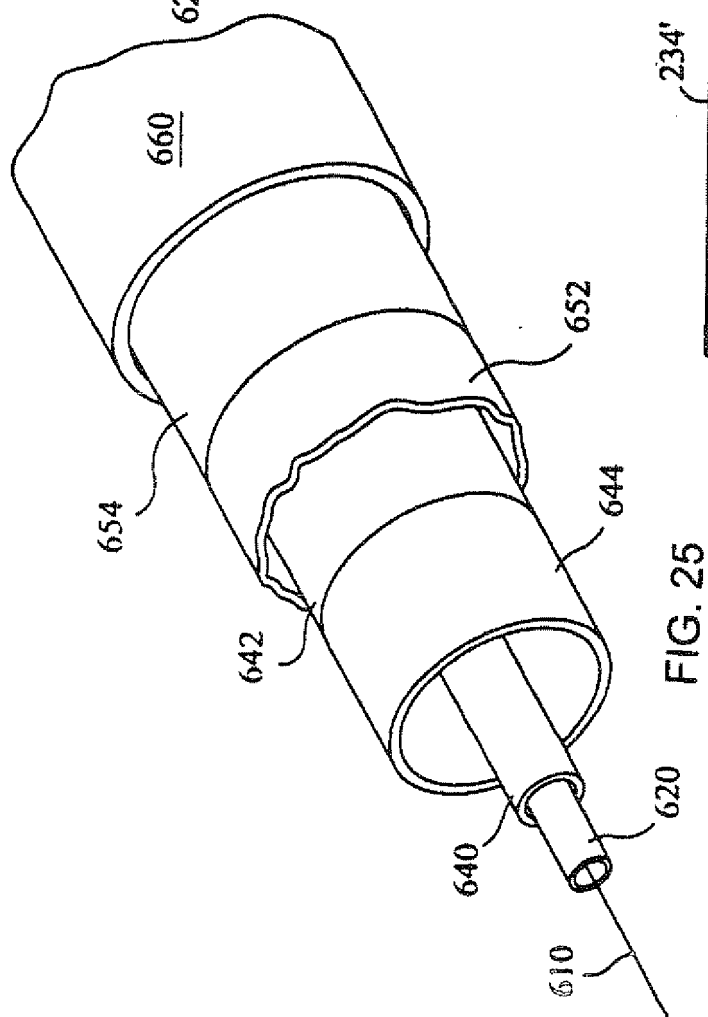


FIG. 25

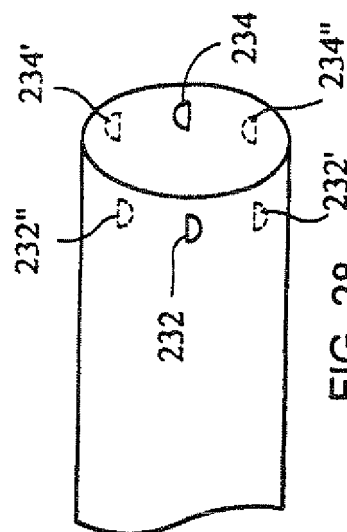


FIG. 28

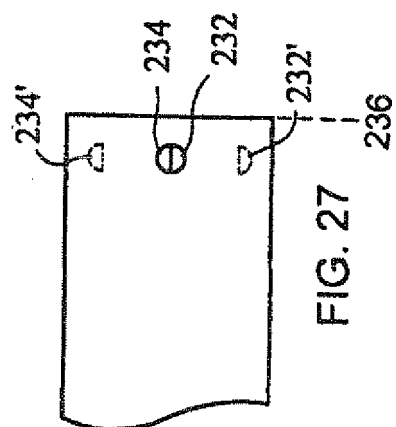
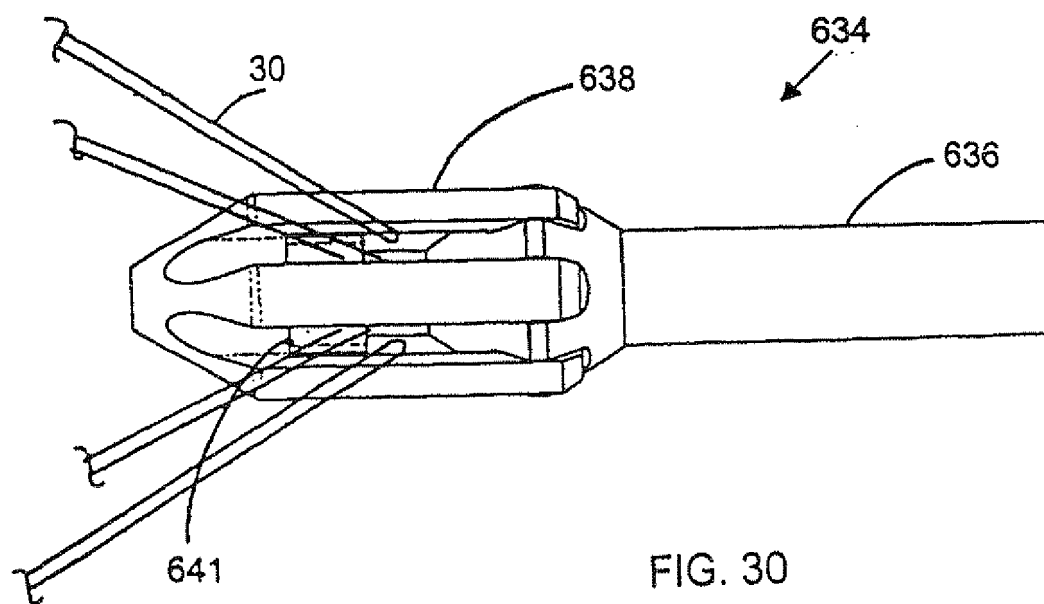
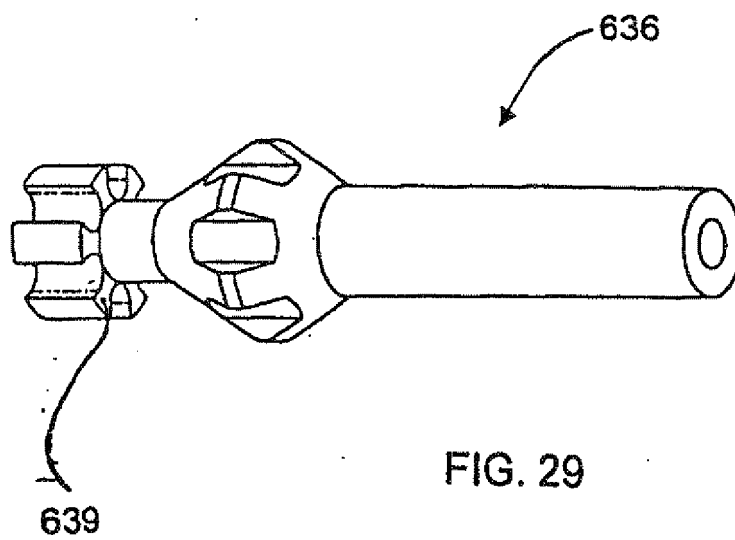
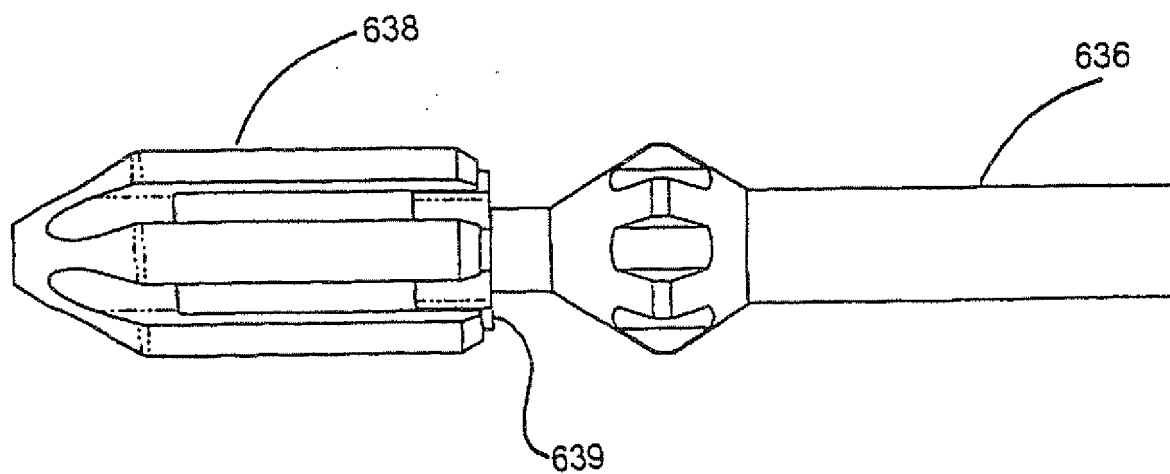
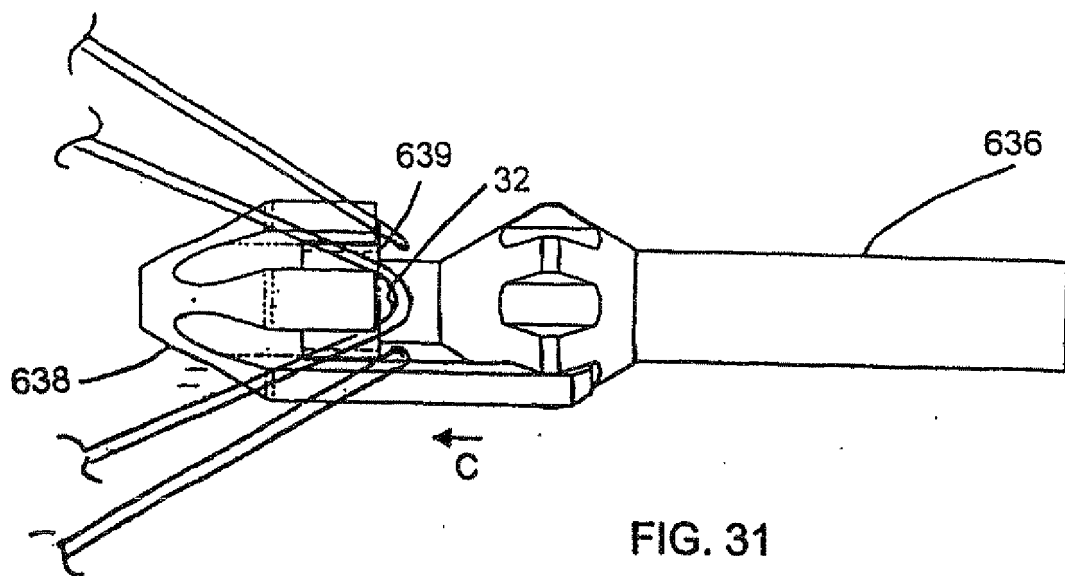


FIG. 27

9/24



10/24



11/24

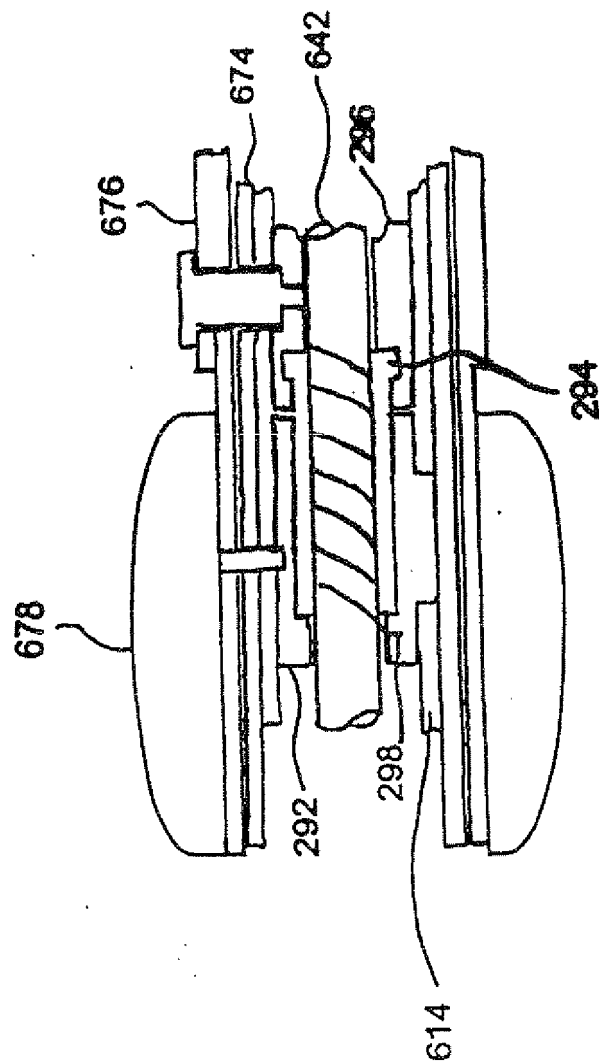


FIG. 33

12/24

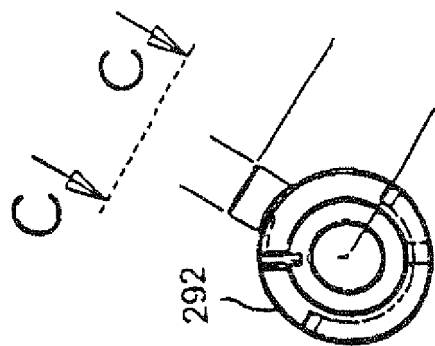


FIG. 34

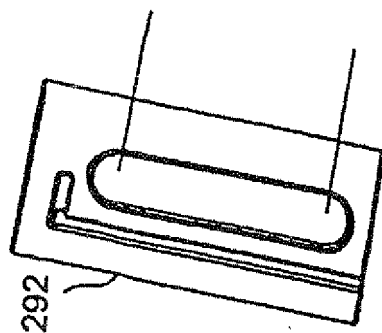


FIG. 35

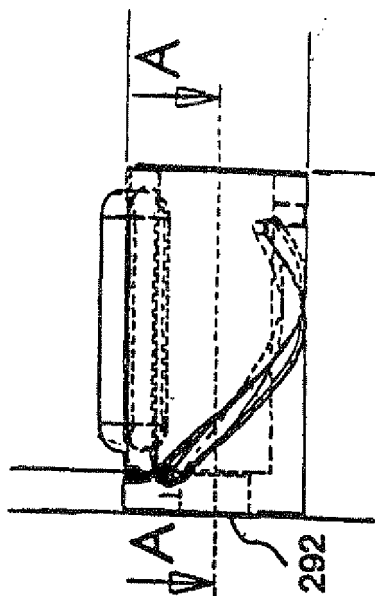


FIG. 36

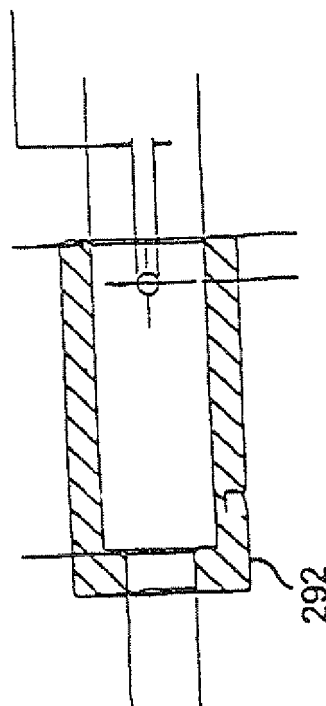


FIG. 37

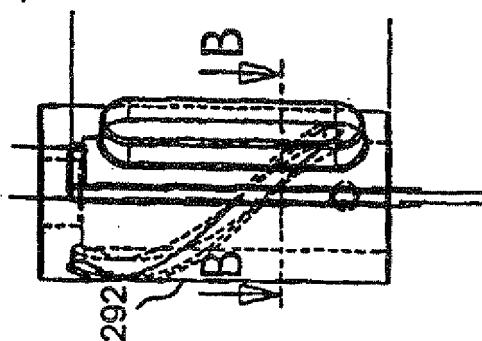


FIG. 38

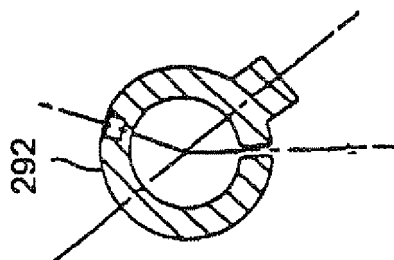


FIG. 39

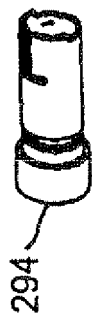


FIG. 40

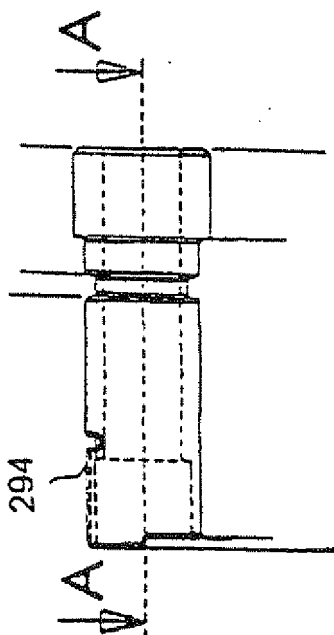


FIG. 41

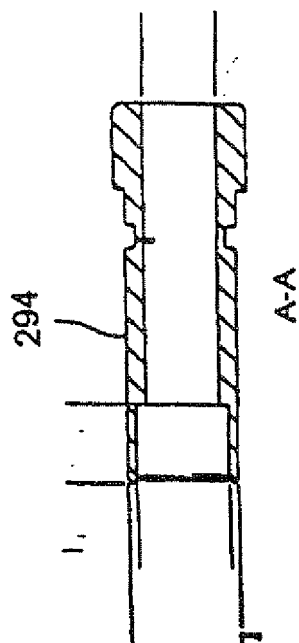


FIG. 42

13/24

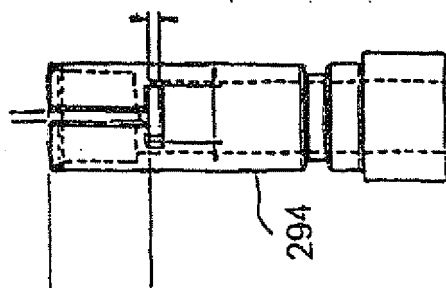


FIG. 43

14/24

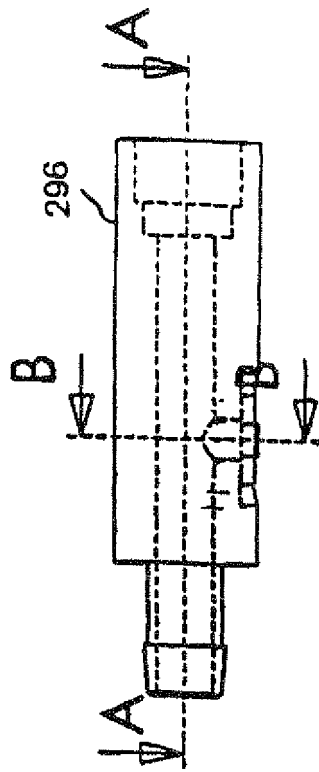


FIG. 44

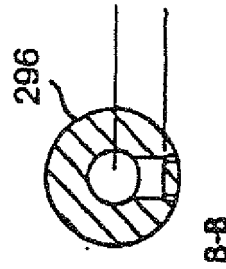
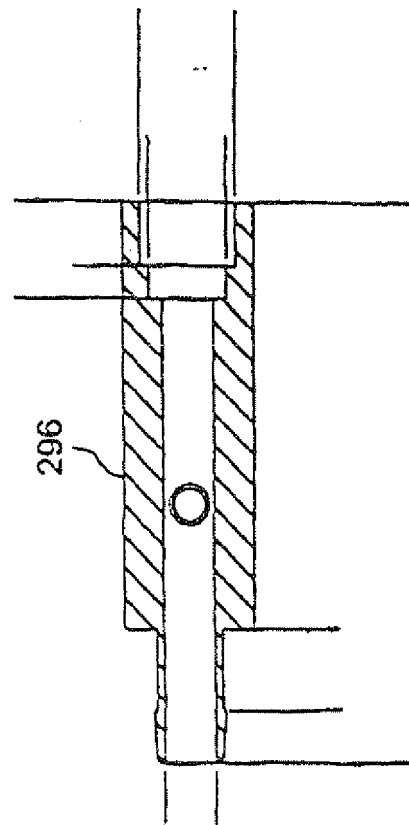


FIG. 46

FIG. 45



A-A

15/24

FIG. 47

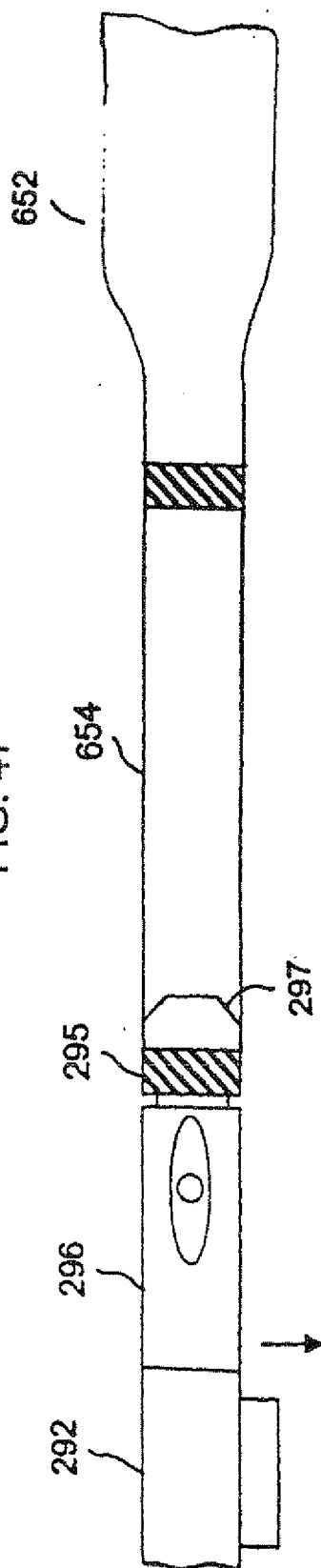
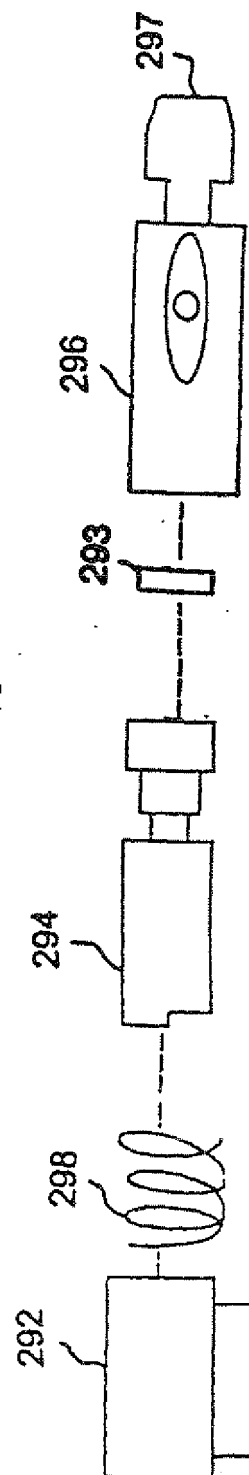


FIG. 48



16/24

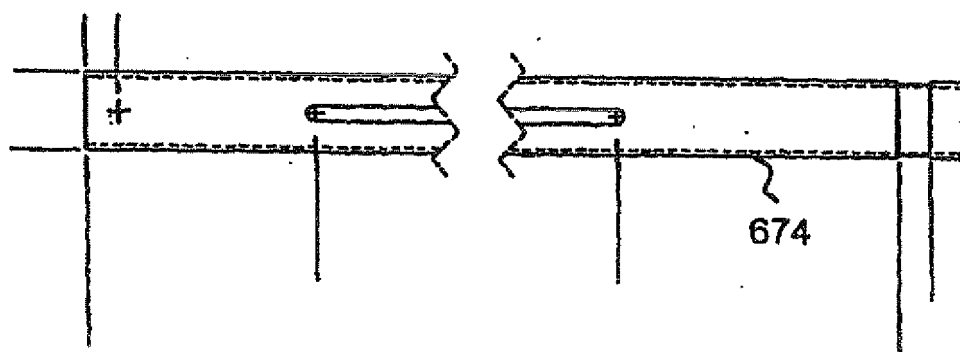


FIG. 49

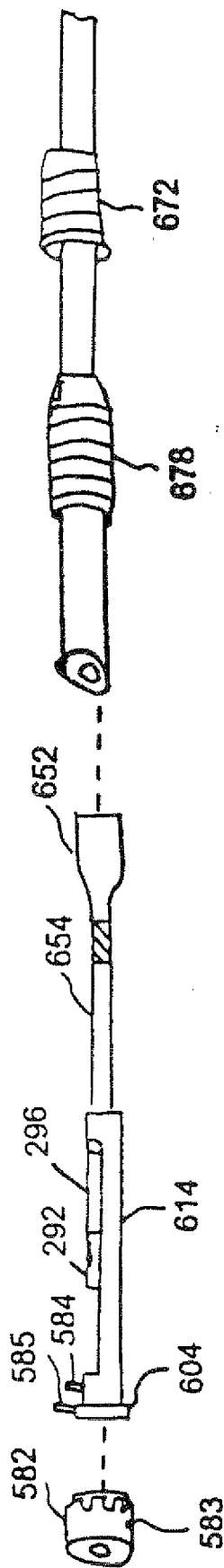


FIG. 50

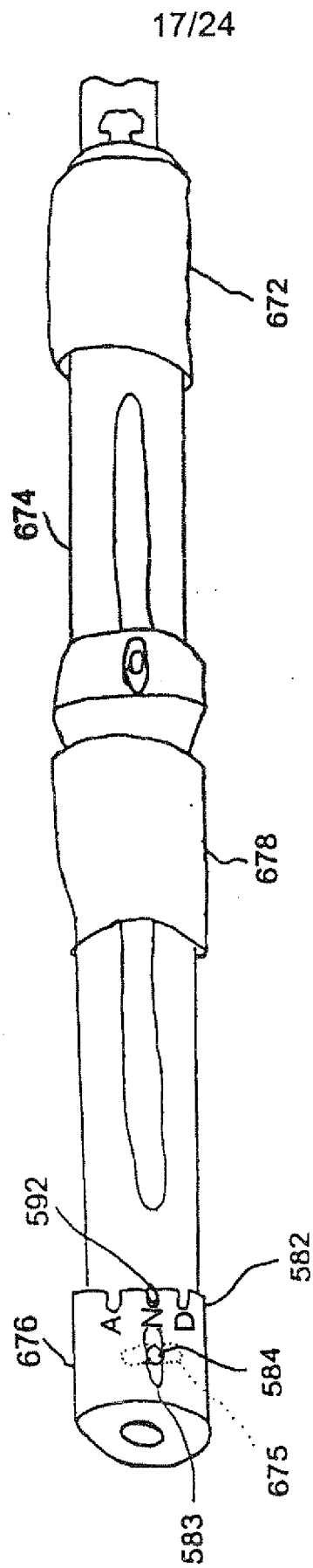


FIG. 51

18/24

FIG. 52

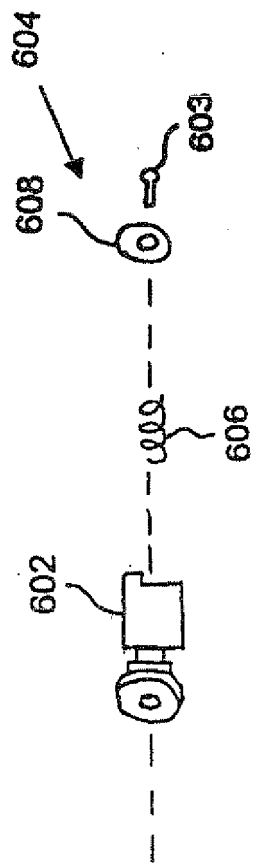
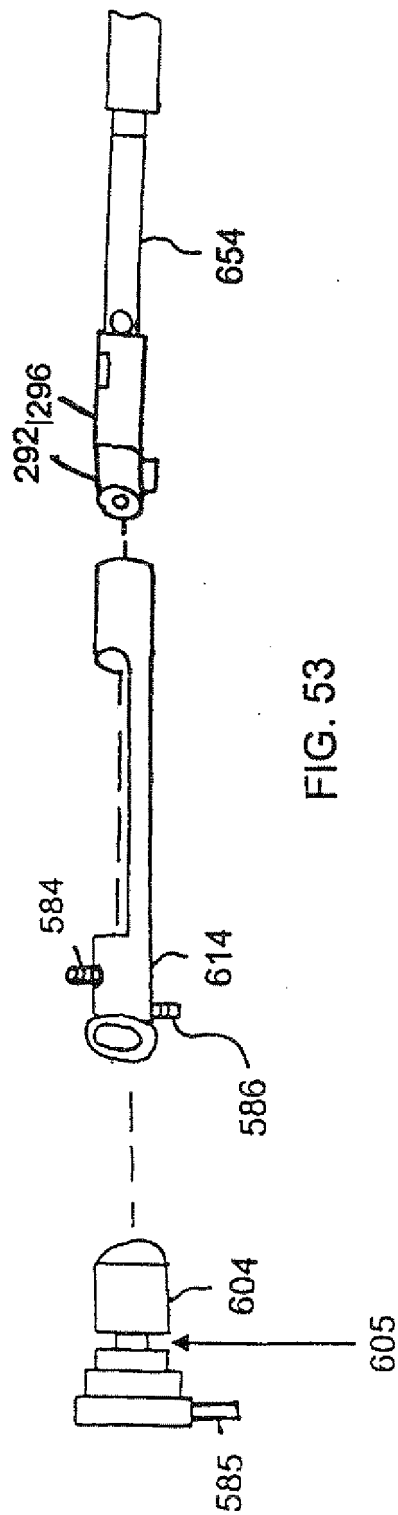


FIG. 53



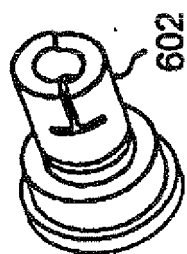


FIG. 54

FIG. 56

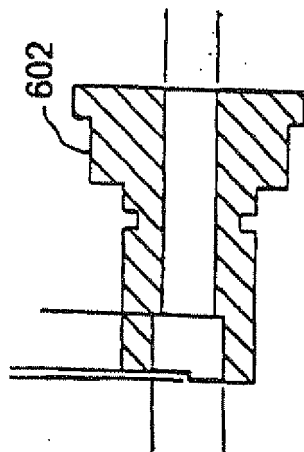


FIG. 55

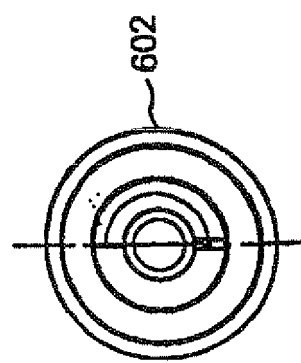
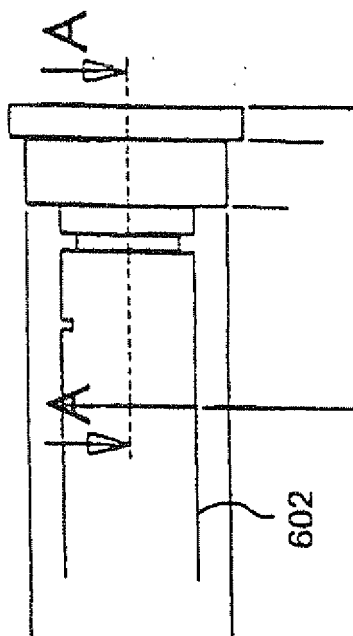


FIG. 58

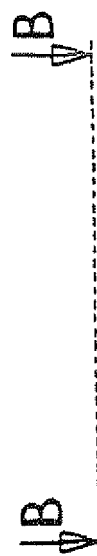


FIG. 57

20/24

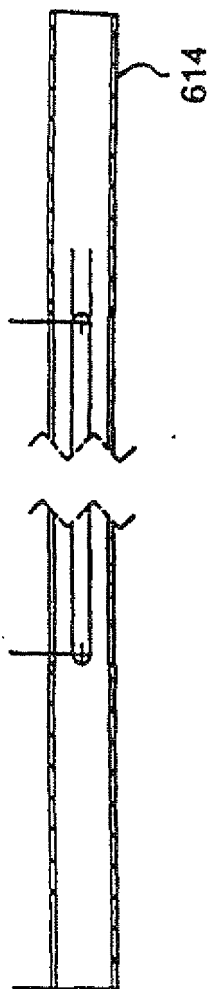
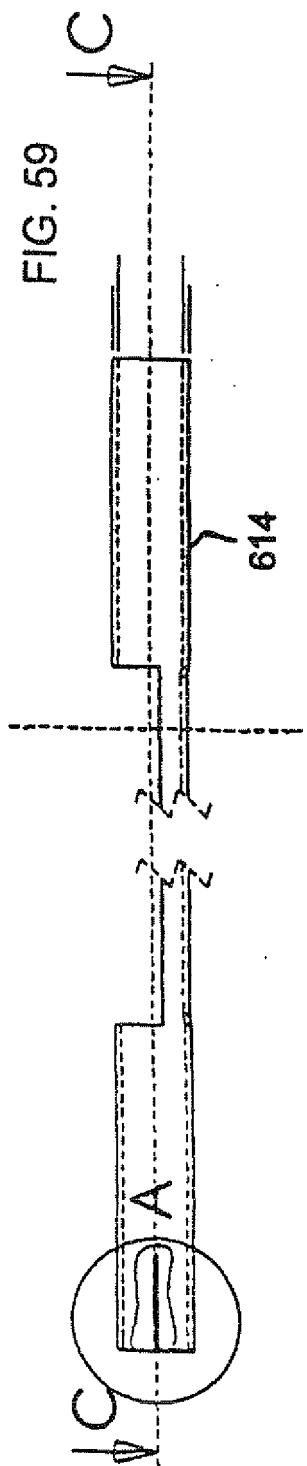


FIG. 60

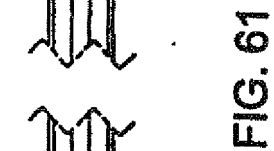


FIG. 61

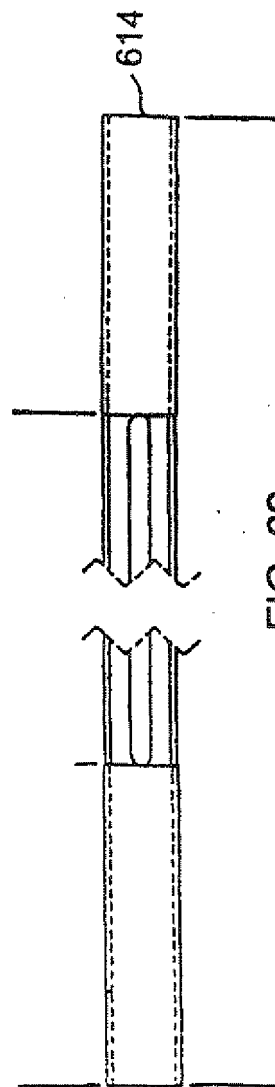


FIG. 62

21/24

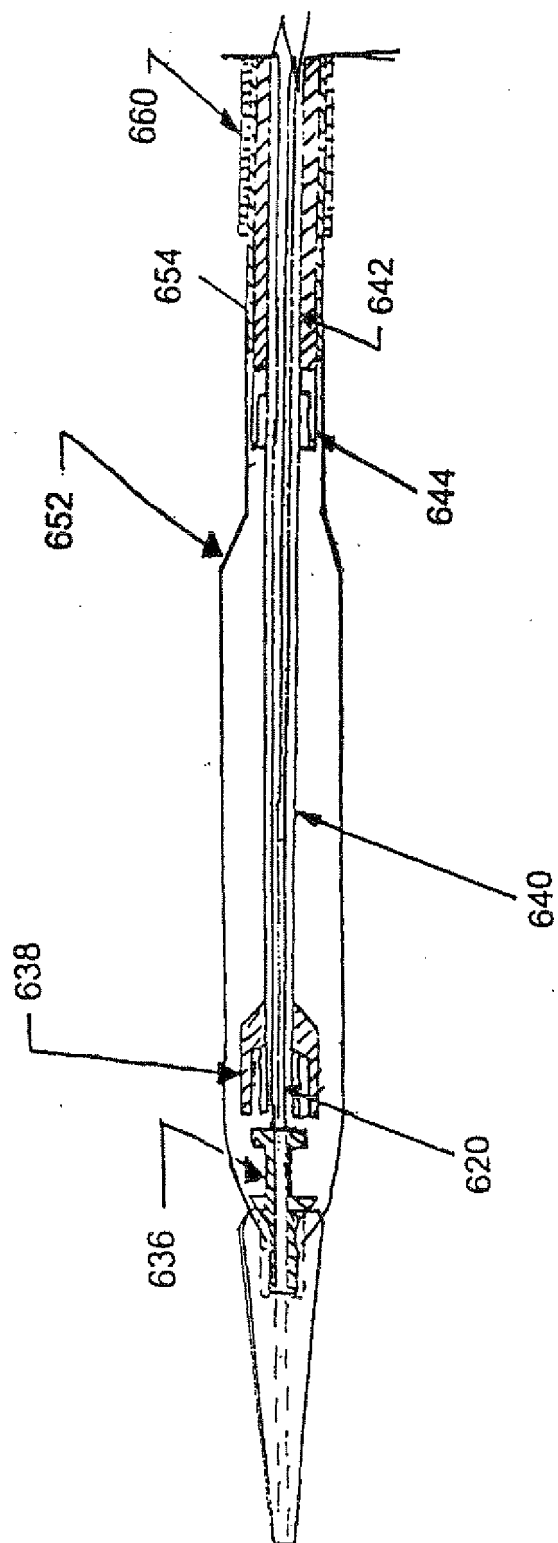


FIG. 63

22/24

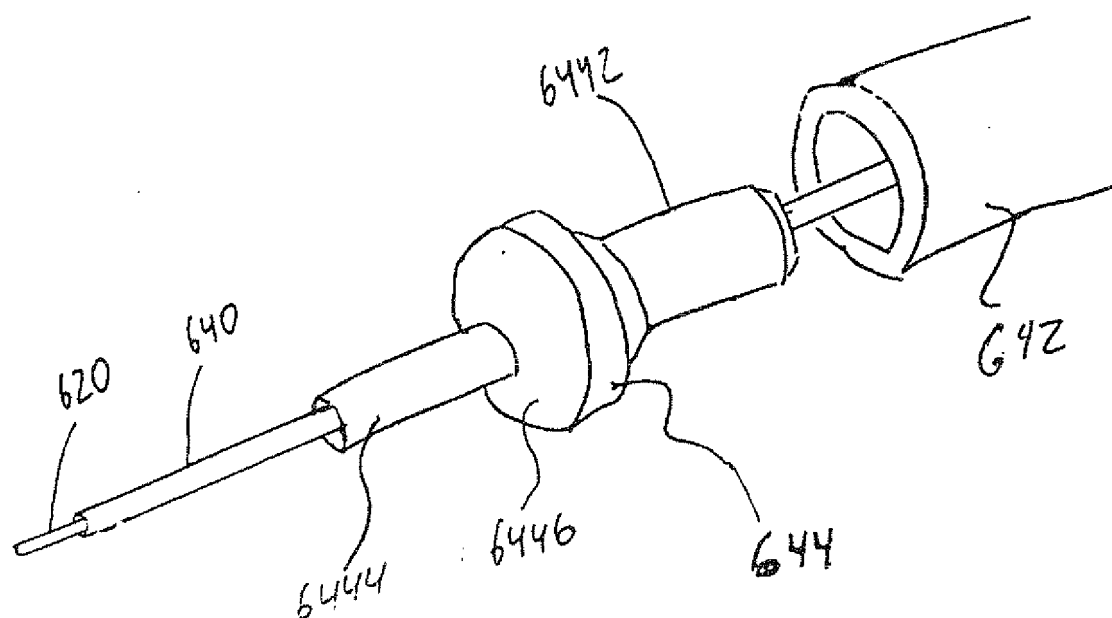
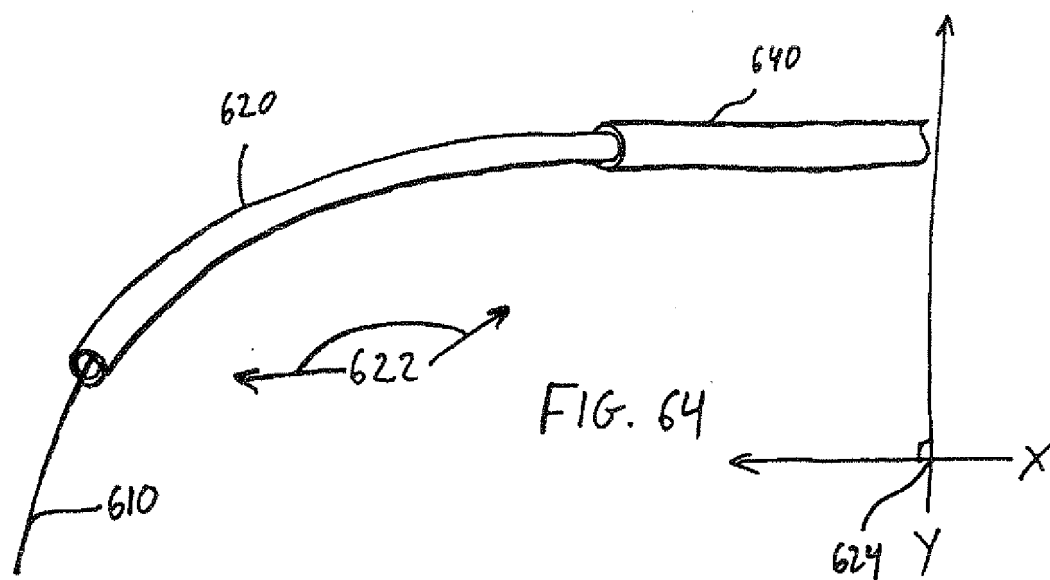


FIG. 68

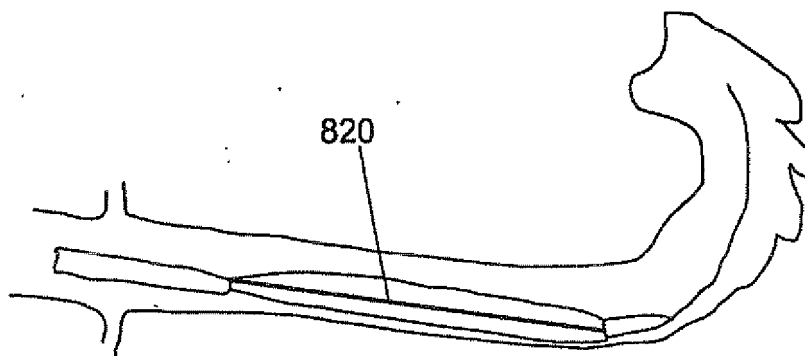
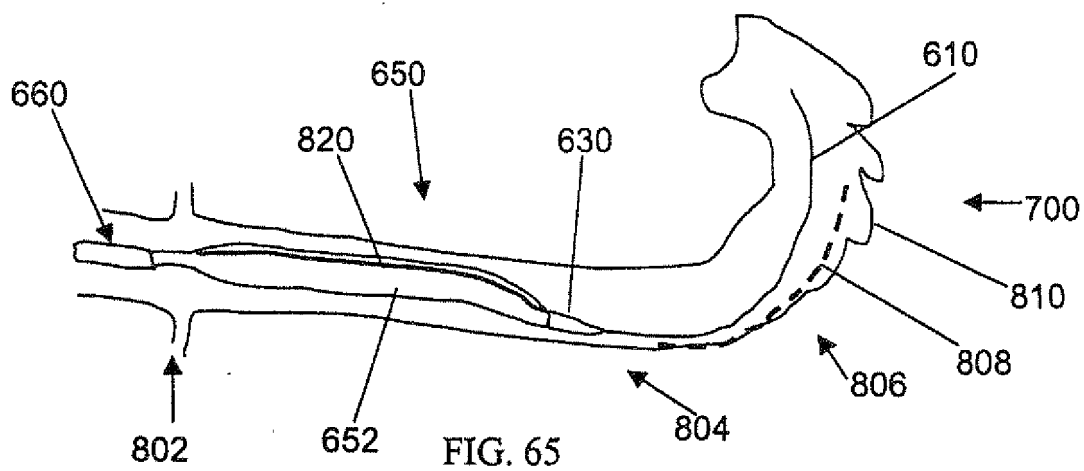


FIG. 66

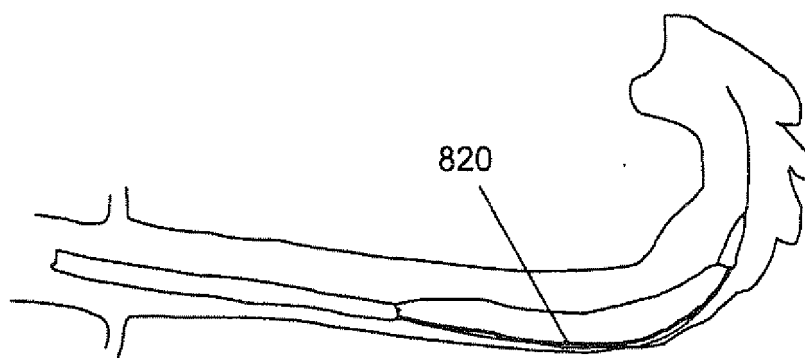


FIG. 67

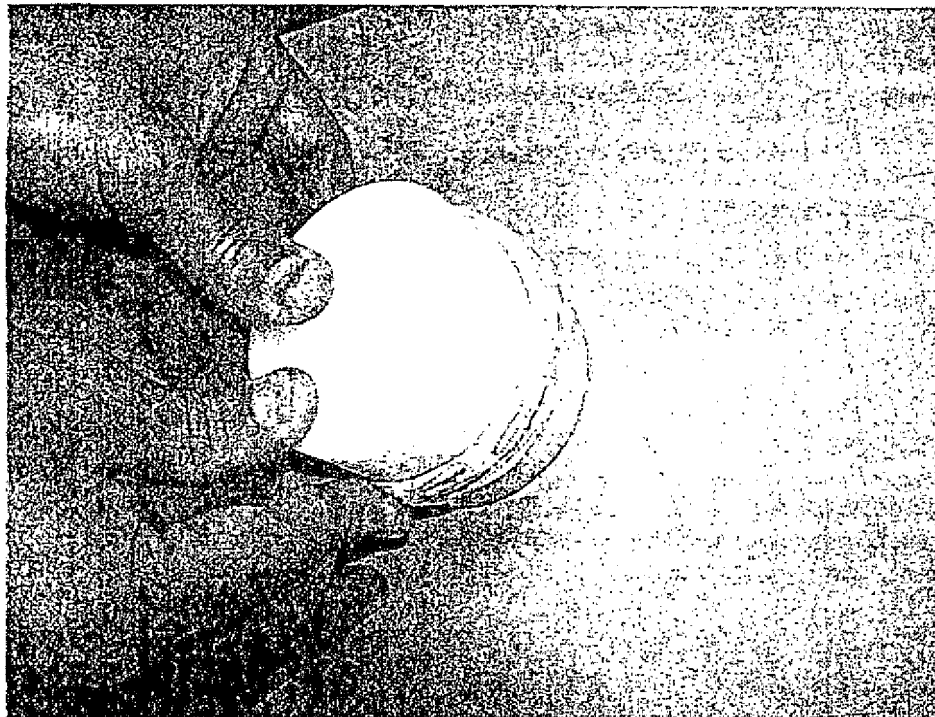


FIG. 69